

- Food Analysis (II year)
- Chemical Analysis of Foods and chemometrics (I year)

a.a. 2025/26

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Subjects

- Mass spectrometry, principles of instrumentation, integration of mass spectrometry with gas and liquid chromatography. Use of LC-MS-MS and GC-MS in food analysis.
- Confirmatory methods in food analysis, guidelines of Eu Legislation for food contaminants, maximum residue limits, artificial and natural contaminants, phytochemicals, control strategies, validation of methods.
- IR spectroscopy, basic theory, rotational and vibrational transitions. FT-IR instrumentation, samples and sampling signal in FT-IR, quality control, qualitative and quantitative application. FT-NIR in food analysis for quality and process control.

Previous knowledge required

- Spectroscopy:
electromagnetic waves, intensity, amplitude, wavelength,
Beer Law, UV-VIS classical spectrophotometer
- Sensors and Biosensors:
principles of potentiometry and voltammetry, enzyme
kinetic (Michaelis-Menten)
- Confirmatory methods and hyphenated techniques
Classical pretreatment of the samples, principles of
chromatography, gas and liquid chromatography

Examination

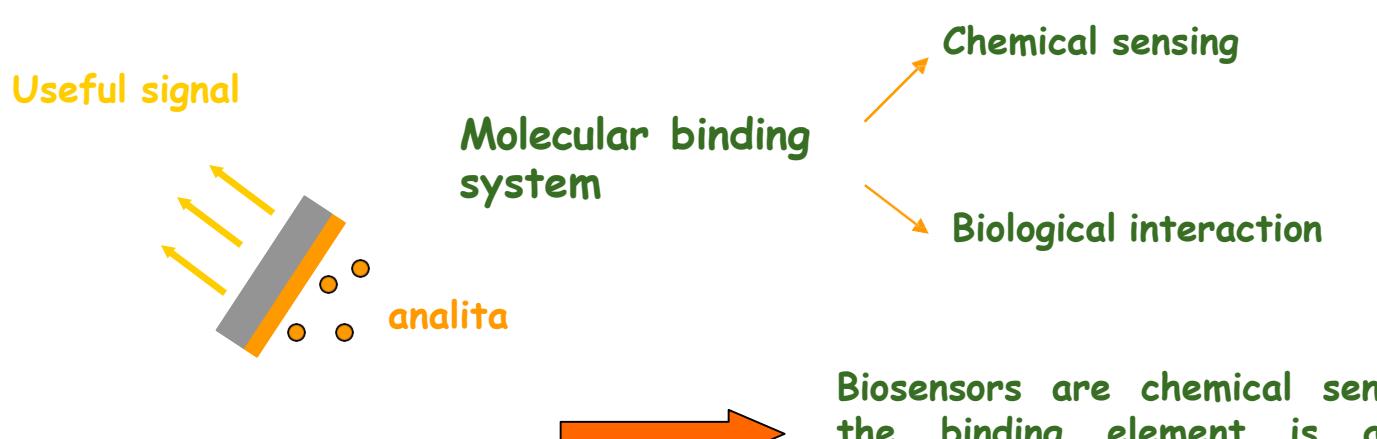
- Written examination (list of questions available)

What are sensors and biosensors?

“...a biosensor is a self-contained integrated device, which is capable of providing specific quantitative or semiquantitative analytical information using a biological recognition element (biochemical receptor) which is retained in direct spatial contact with a transduction element.”

Technical report “ Recommended definition and classification” IUPAC (Physical Chemistry and Analytical Chemistry Divisions) 2001

A **sensor** is a device able to transform a physical or chemical info (e.g. concentration of one or more compounds in a solution), into an analytical useful signal



Biosensors are chemical sensors in which the binding element is a biological molecule

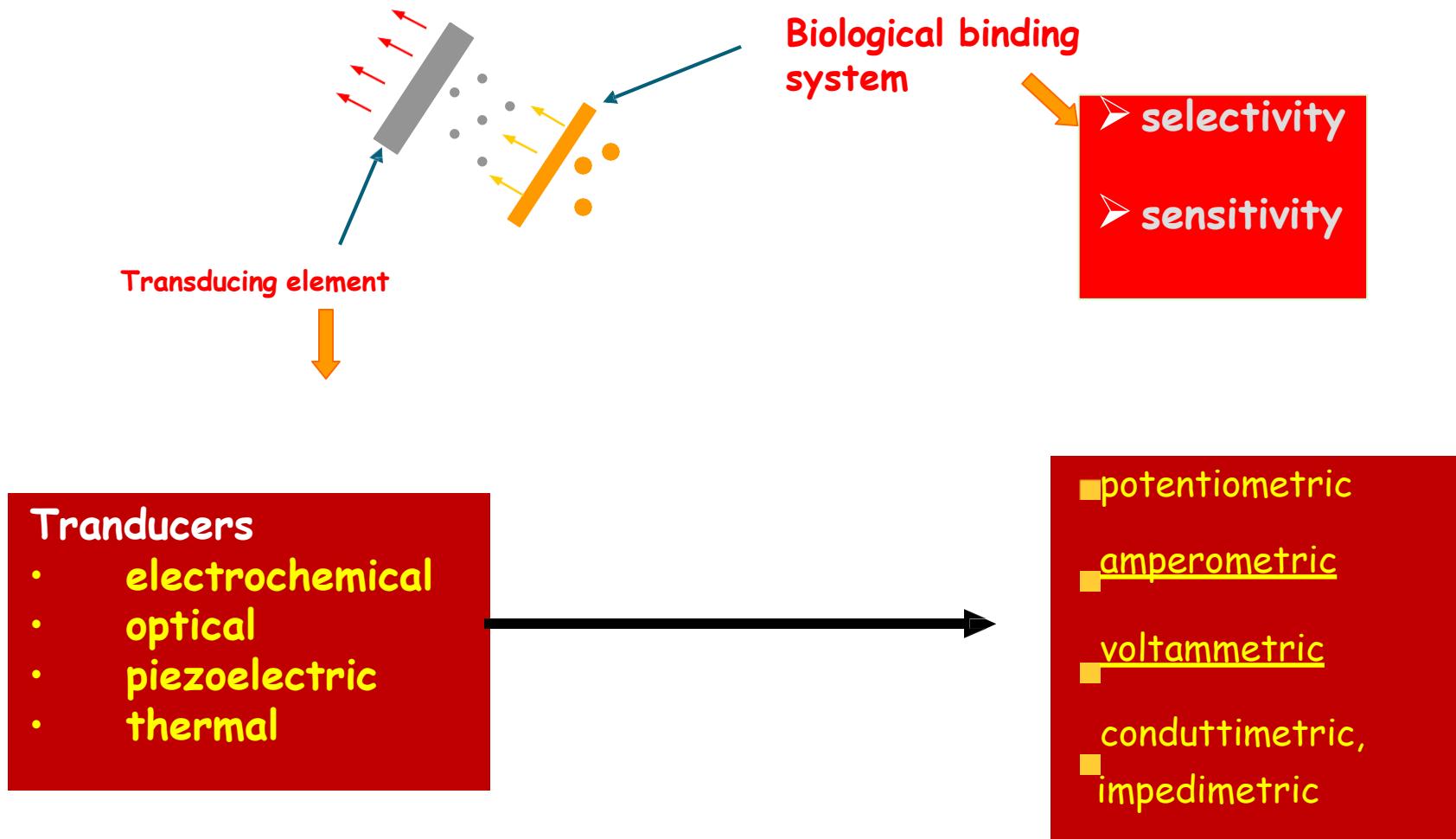
Self-testing



Numbers:

- 85% of the global market for biosensors
- 70 million tests per day worldwide
- 15 billion \$ in 2015
- 30 billion \$ in 2024 (exp.)

The biological element translates the info of the biochemical domain (e.g. concentration) into a chemical or physical signal with a certain selectivity



Classification of biosensors on the basis of the biological element

Catalytic biosensors

catalysis of a chemical reaction

ex: enzymes, cells, tissues

Affinity biosensors

formation of a stable complex with the ligand

ex: antibodies, DNA strands, proteic receptors

Biomimetic biosensors

affinity biosensors using a synthetic receptor

ex: peptides, aptamers, molecularly imprinted polymers

Ion selective electrodes for biosensors

The most used ISEs for the development of biosensors have been CO_2 and NH_3 probes.

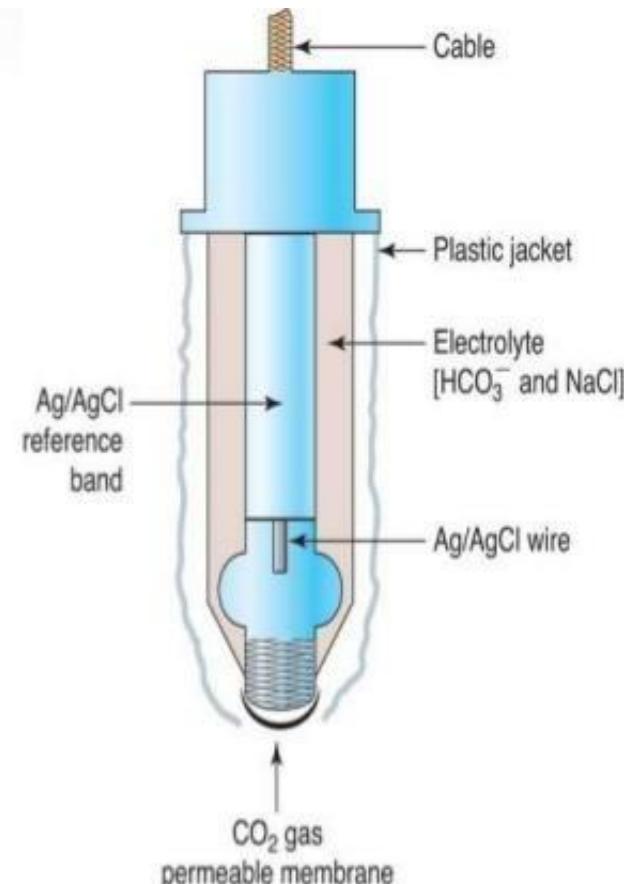
This potentiometric gas-sensors are realised using a pH glass electrode and a reference behind a gas permeable membrane (polytetrafluoroethylene, polypropylene, etc.). A very thin film of a suitable electrolyte is present between the gas permeable membrane and the surface of the pH electrode.

Hydrolysis of NH_3 or CO_2 (diffused from the sample) in the electrolyte causes a change in H^+ that is measured at the electrode.

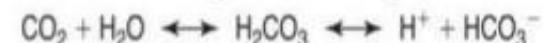
This is related to the partial pressure of the gas in the sample solution. Immobilisation of a suitable enzyme onto the surface leads to the detection of metabolites in the 10^{-5} – 10^{-2} mol/L range.

PCO₂ ELECTRODE

- Measurement of PCO₂ in routine blood gases
- A modified pH electrode with a CO₂ permeable membrane covering the glass membrane surface
- A bicarbonate buffer separates the membranes
- Change in pH is proportional to the concentration of dissolved CO₂ in the blood

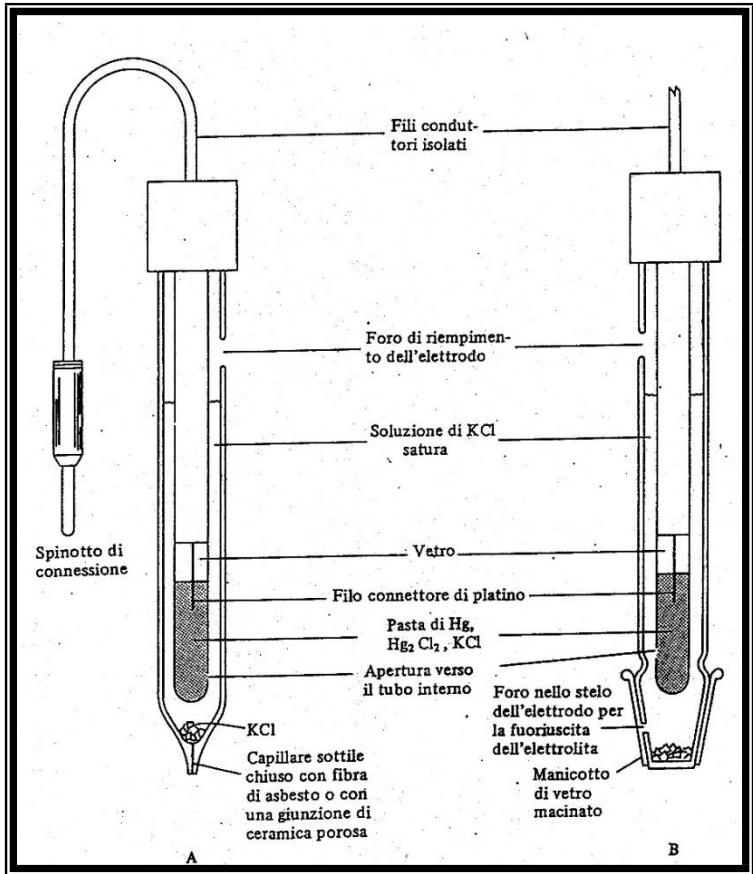


Reaction occurring in the electrolyte solution:

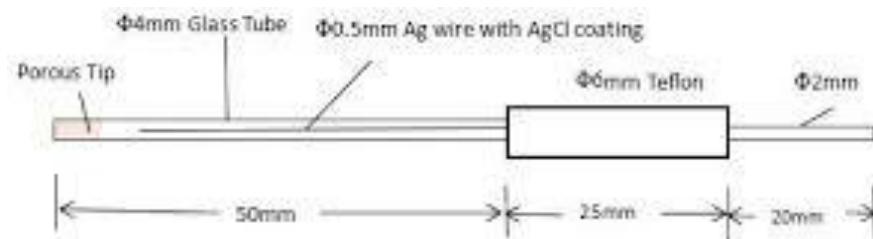


Reference electrodes

calomel



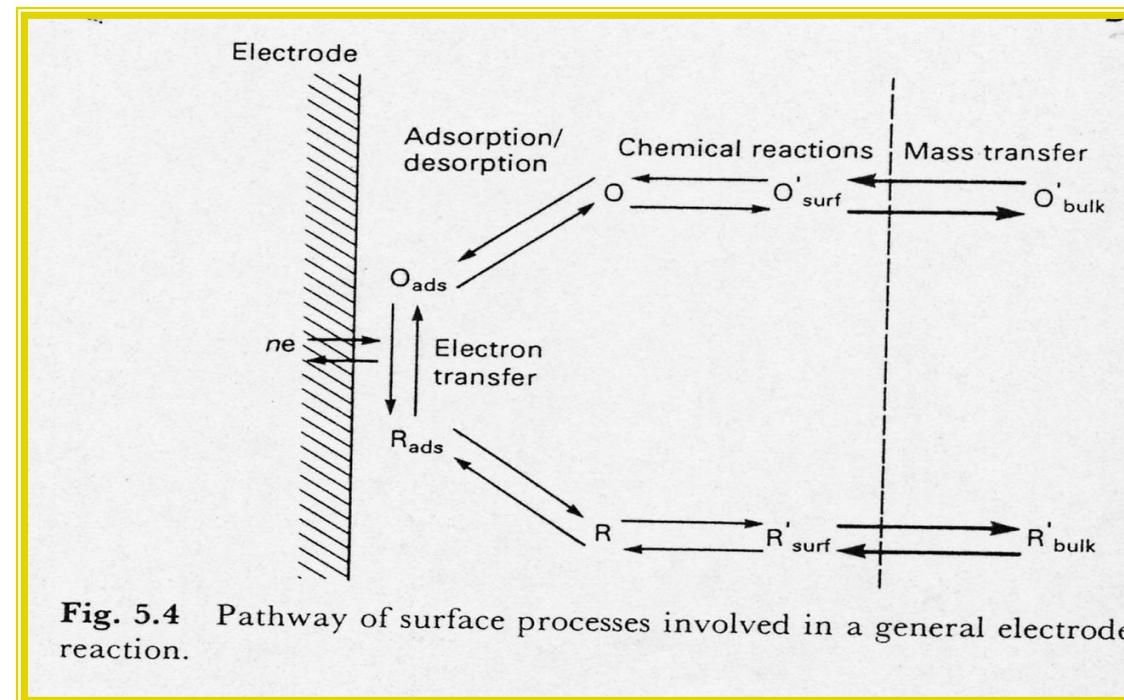
Ag/AgCl



CS901 Ag/AgCl Reference Electrode

Amperometric sensors monitor the current flow when a selected fixed potential is applied at a working electrode with respect to a reference electrode. The current generated by the oxidation (or reduction) of a compound is dependent by:

- heterogeneous rate constant k
- diffusion (mass transfer) of the electroactive species at the electrode surface
- preceding or following chemical reactions
- surface reactions (adsorption)



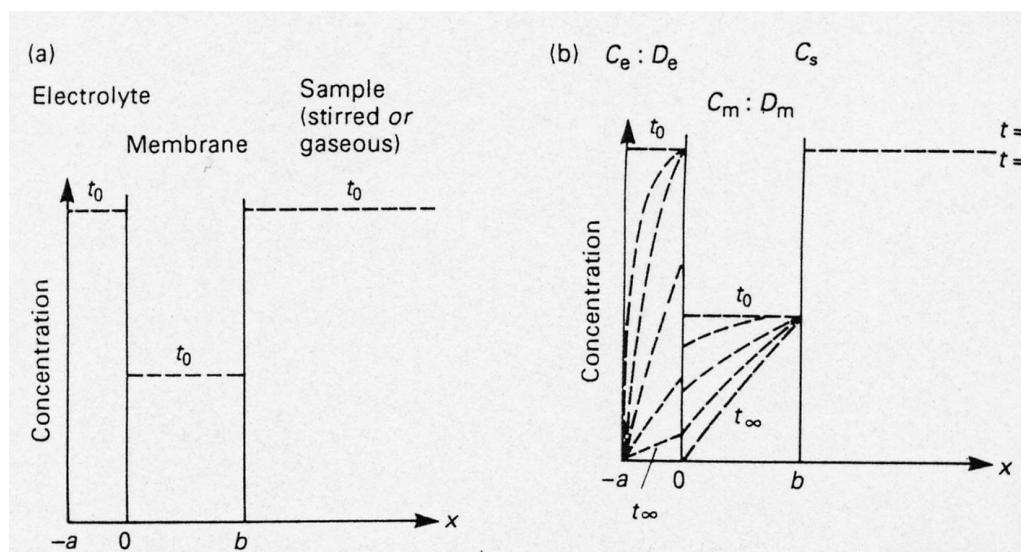
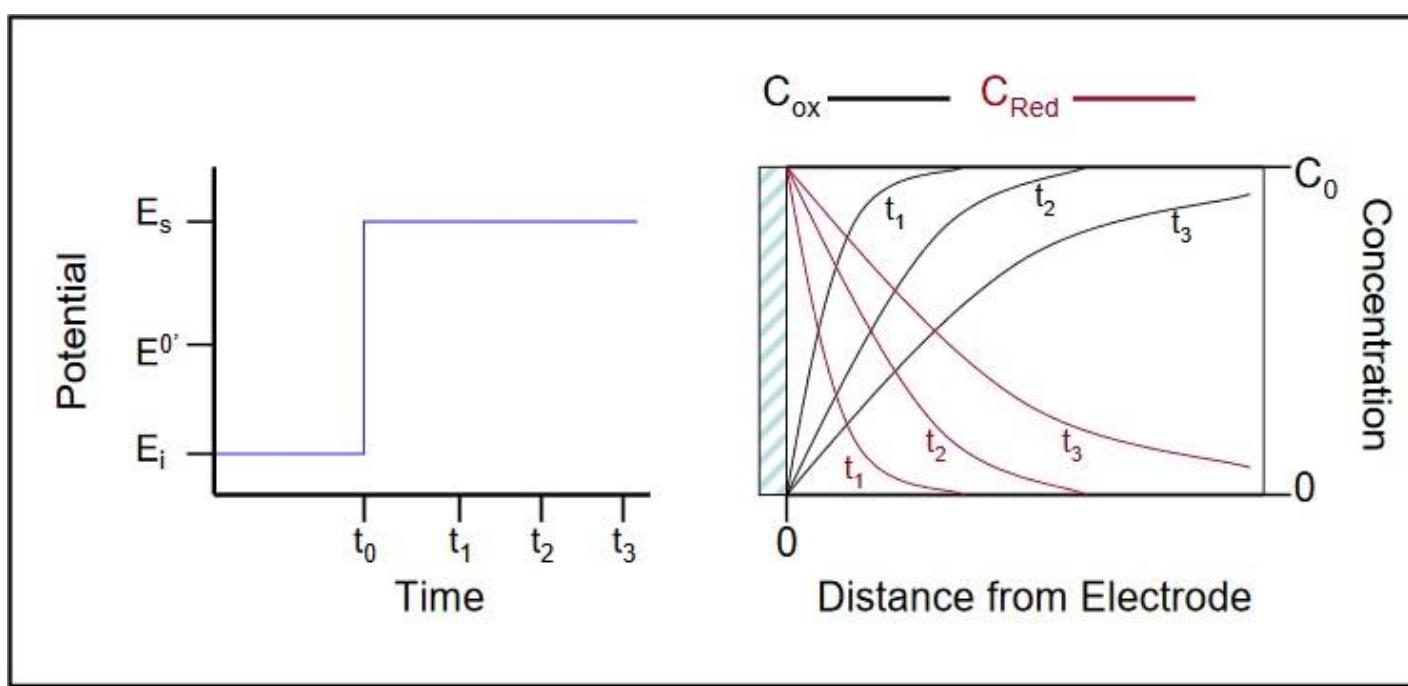
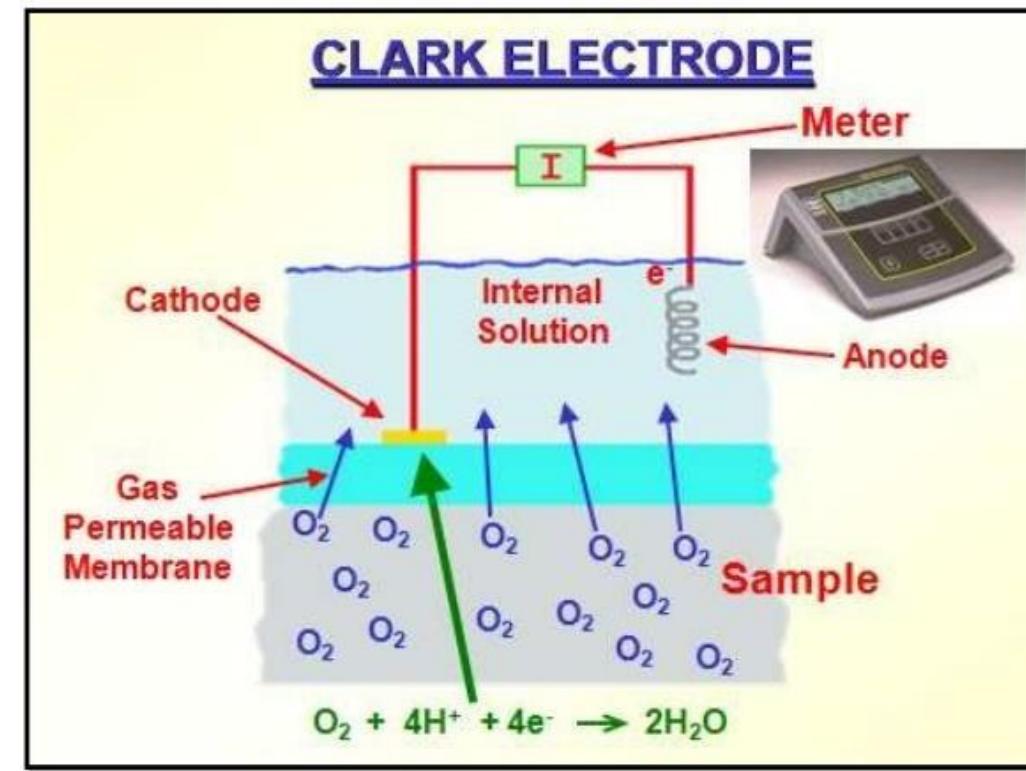
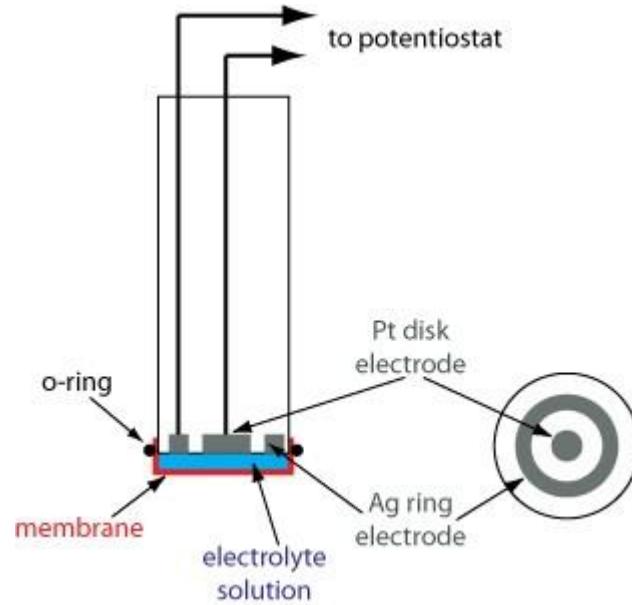


Fig. 5.8 Concentration profiles for a membrane-covered electrode. (a) The initial profile; (b) the development of concentration gradients through the different phases during attainment of steady state.



Applied potential
-0.7 V vs. Ag/AgCl



Dissolved Oxygen Electrode /Sensor
Industrial Type Model : MS DO 714

OXYGEN PROBE

The cathode should possess: high catalytic activity for the reduction of O_2 , (large exchange current) , sufficient electrical conductivity (low adsorption of organic impurities or O_2), it should be inert , it should exhibit a large overvoltage for the decomposition of water (no hydrogen liberation), it should permit the required construction operation (e.g. sealing into glass)

Pt and Au are the most used materials

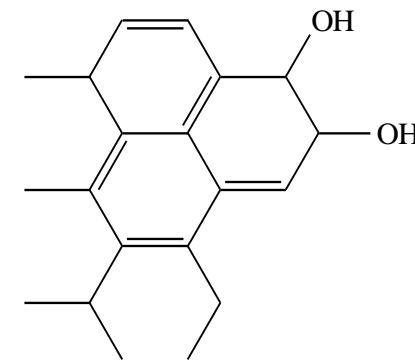
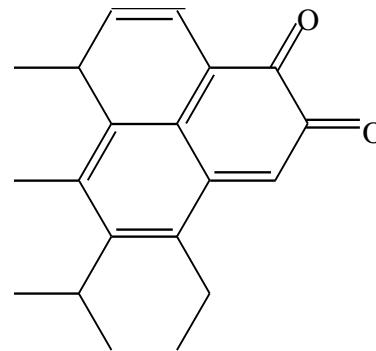
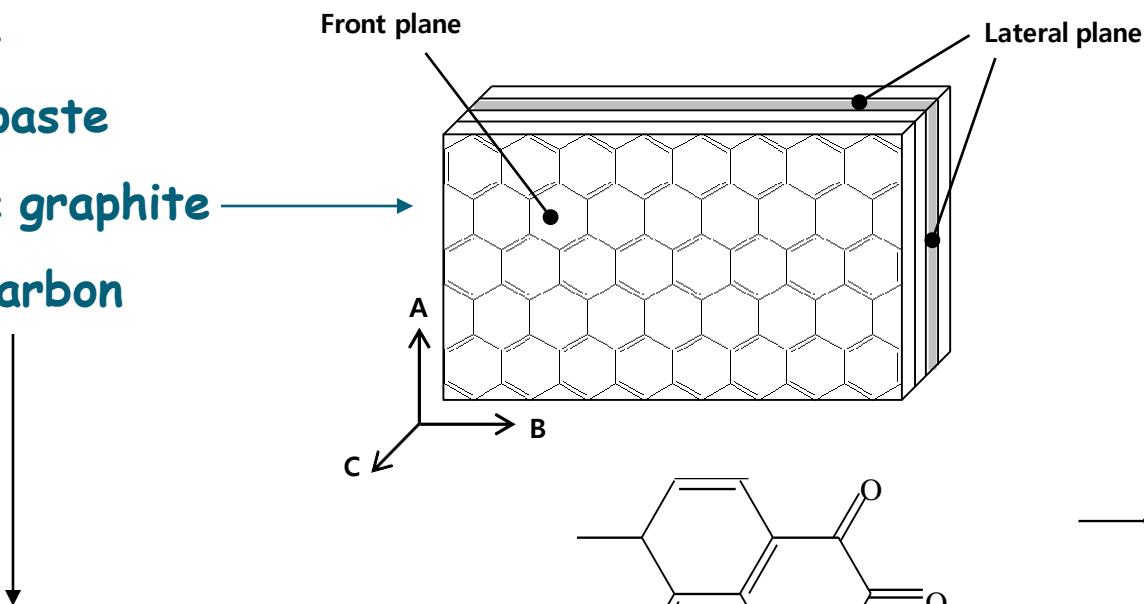
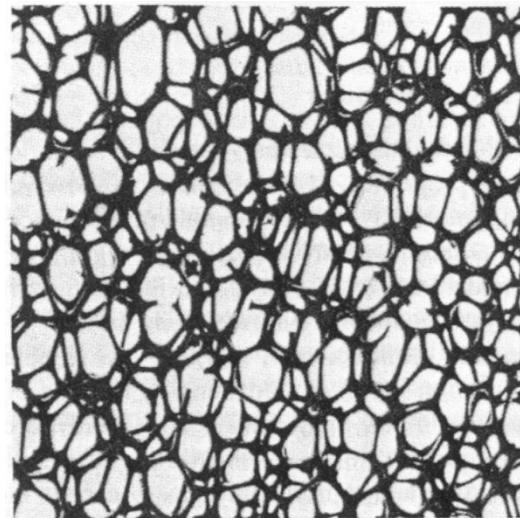
The gas permeable membrane protects the electrodes from contamination, provides for reproducible conditions of oxygen tranport and minimize undesirable changes in electrolyte composition. Ideally, it shoud be with low permeability and high diffusivity for oxygen.

Non-hydratable polymers as polytetrafluoroethylene (PTFE), polypropylene (PP) and polyethylene (PE) are generally used. Alternatively elastic rubber or silicone are useful, even though less stable in alkaline medium.

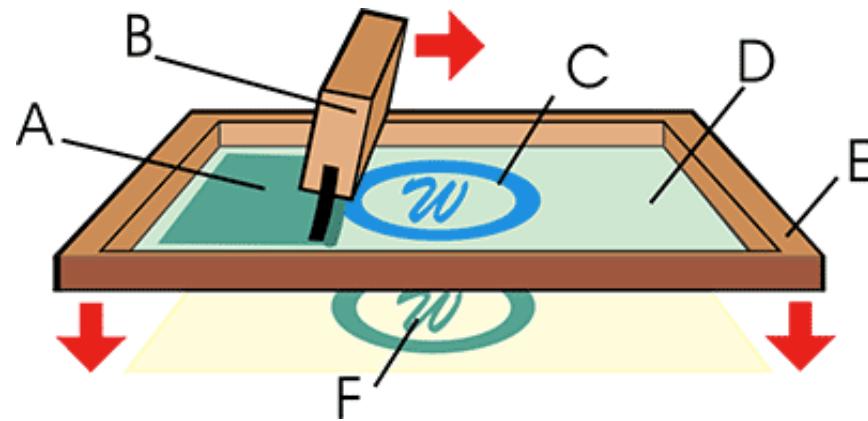
The anode is $Ag/AgCl$ and a neutral or alkaline electrolyte is used in the final assembling.

Conventional carbon based probes:

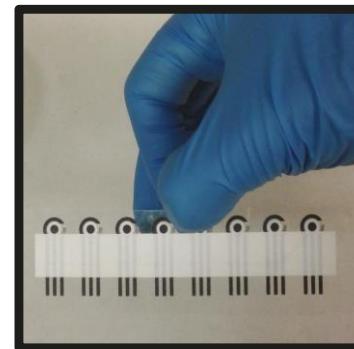
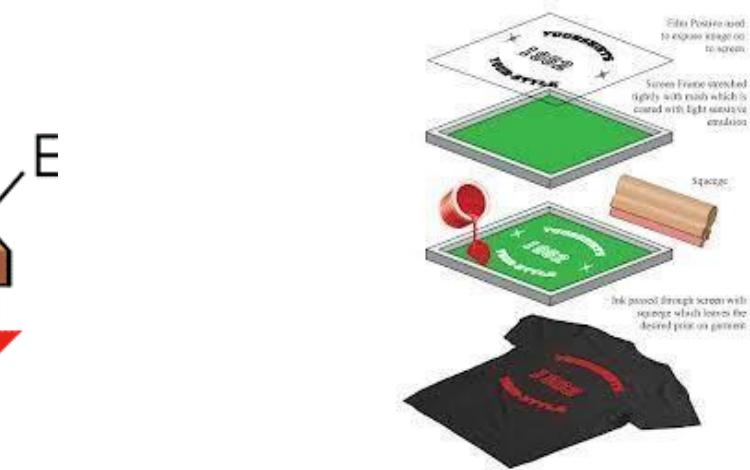
- graphite
- carbon paste
- pyrolytic graphite
- glassy carbon



Printing electrodes: serigraphy



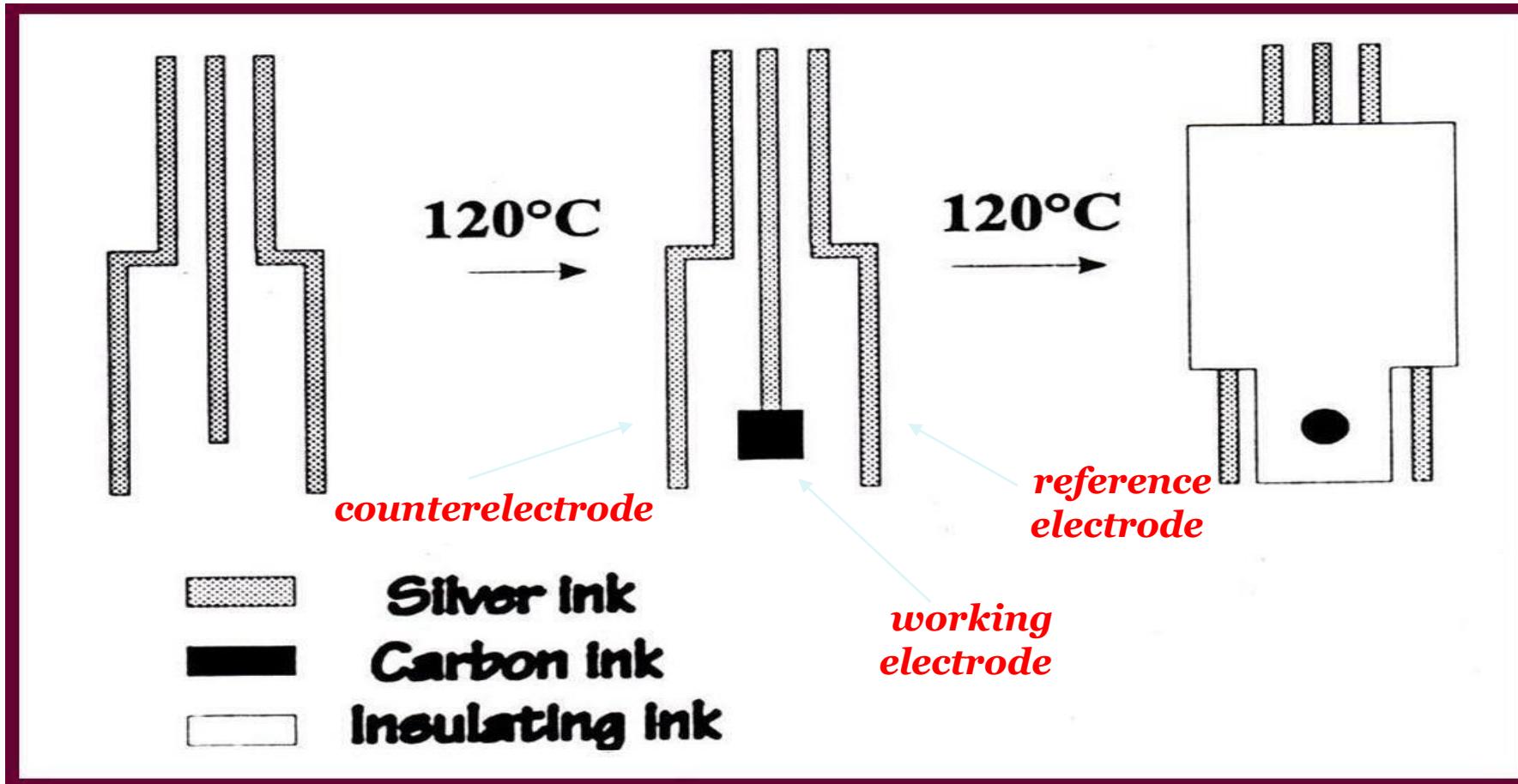
- A. ink;
- B. squeegee;
- C. printing mask;
- D. printing mesh;
- E. frame;
- F. printed ink

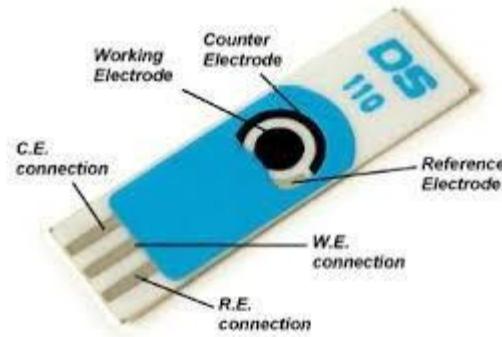


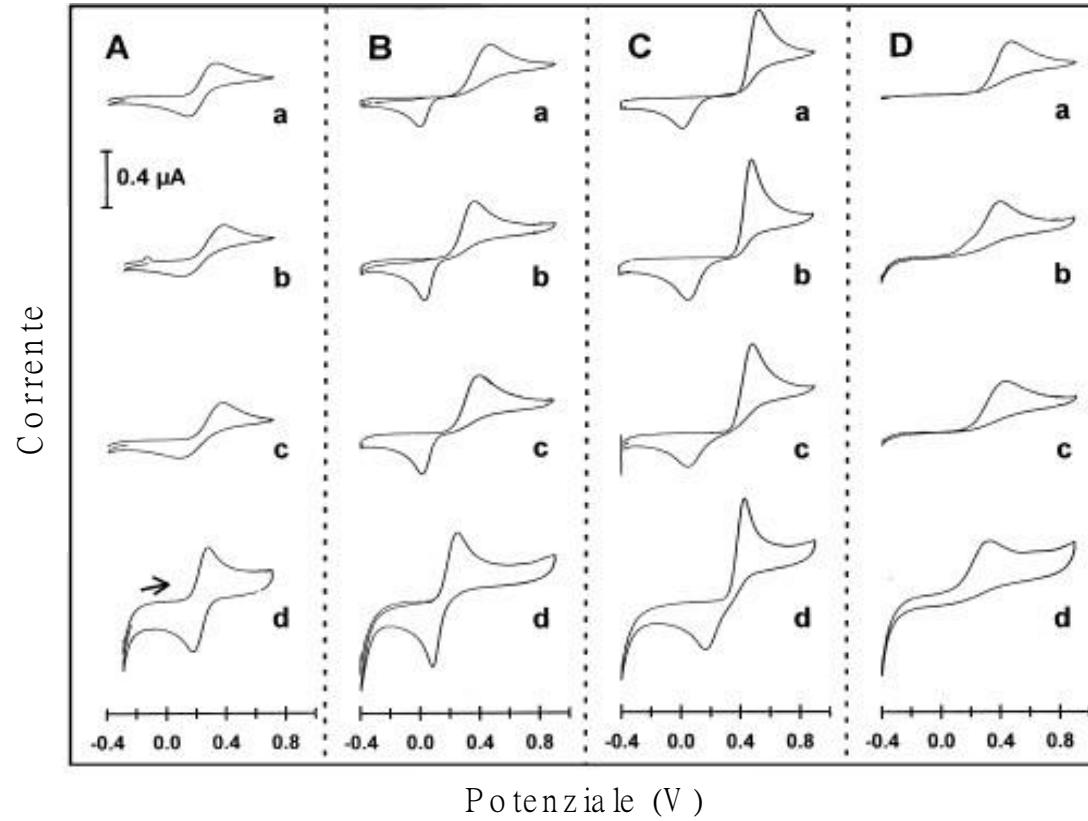
Advantages:

- Dimension
- Disposable
- Low-Cost

DISPOSABLE SCREEN-PRINTED CARBON ELECTRODES

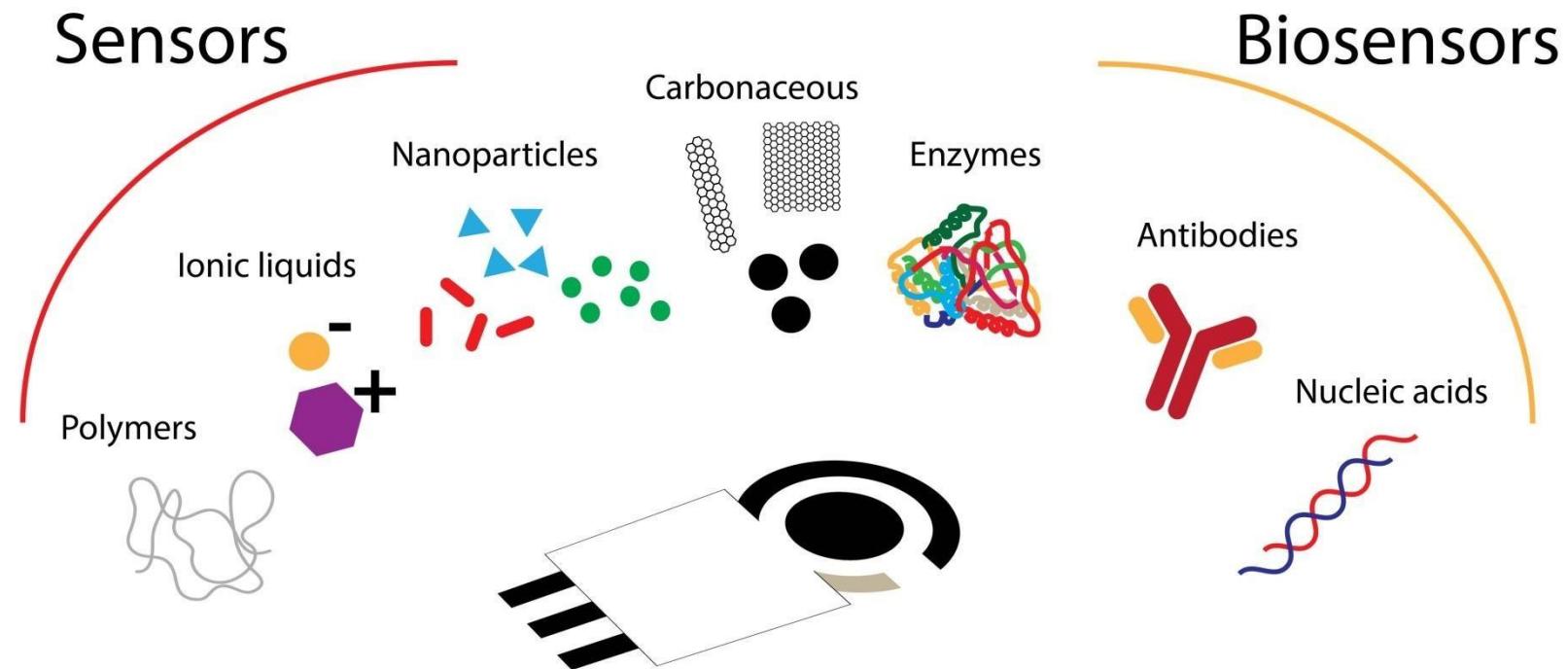






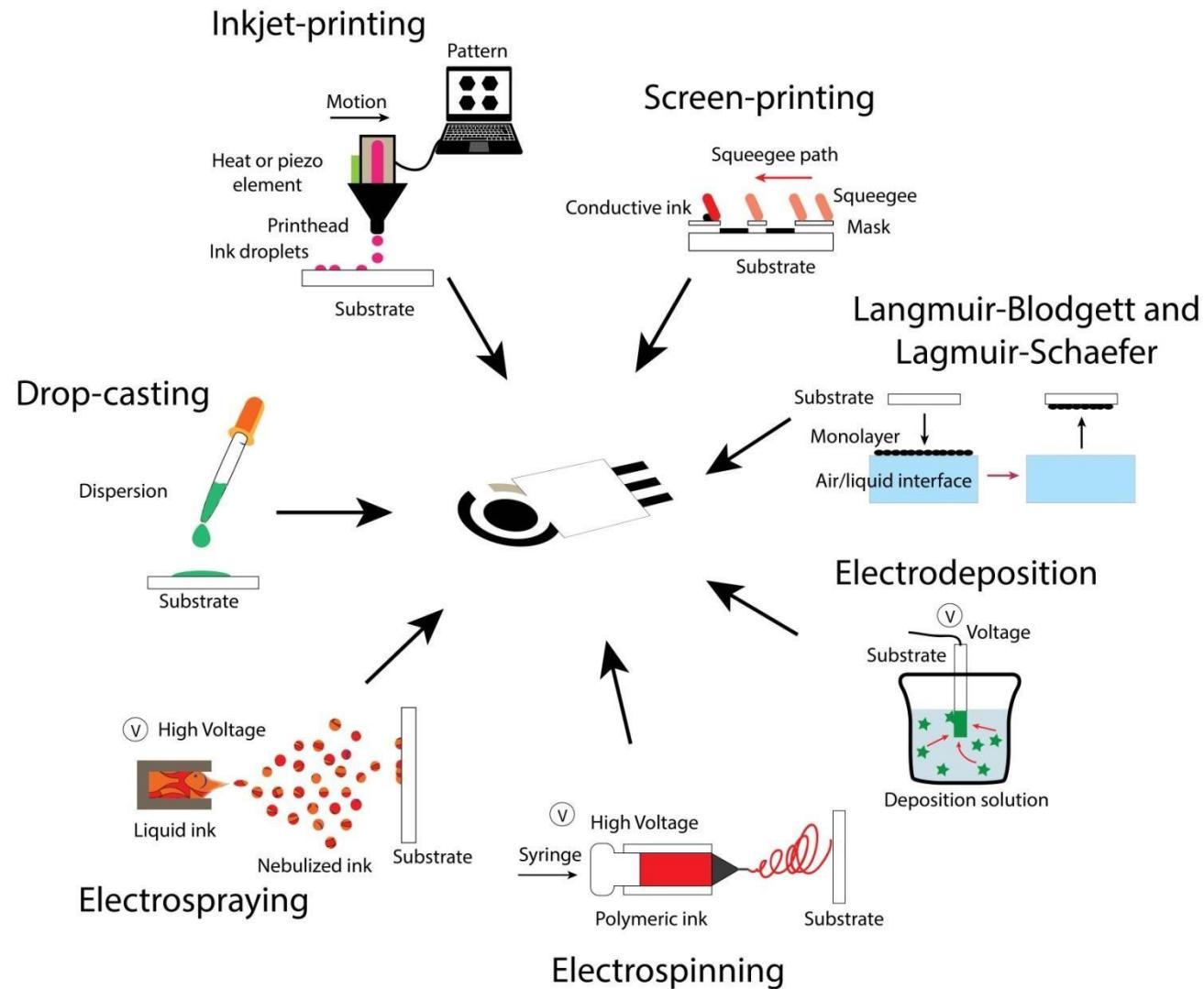
Cyclic voltammetries of ferricyanide (A), cathecol (B), acetaminophene (C), ascorbic acid (D) carried with different screen-printed electrodes: Dupont (a), Ercon (b), Acheson (c) Gwent (d). Supporting electrolyte; KCl 0.1M (A), scan rate 20 mV/s.

Screen-Printed Electrodes



Screen-printed electrochemical (bio)sensors

How do we tune them?

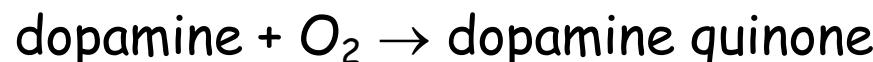


TISSUE BASED BIOSENSORS

bovine liver (rich in catalase)



banana (rich in polyphenol oxidase)



CELL BASED BIOSENSORS

measurement of ethanol using *acetobacter xylinum* (O_2 electrode)

Determination of the BOD (biological oxygen demand).

The BOD values indicate the amount of biochemically degradable organic material (carbonaceous demand) and the oxygen used to oxidise sulphides and ferrous ion.

Conventional methods include BOD_5 and BOD_7 which need 5 and 7 days.

BOD biosensors have been developed using *Trichosporon cutaneum*, *Bacillus subtilis*, *Hansenula anomala*, etc.

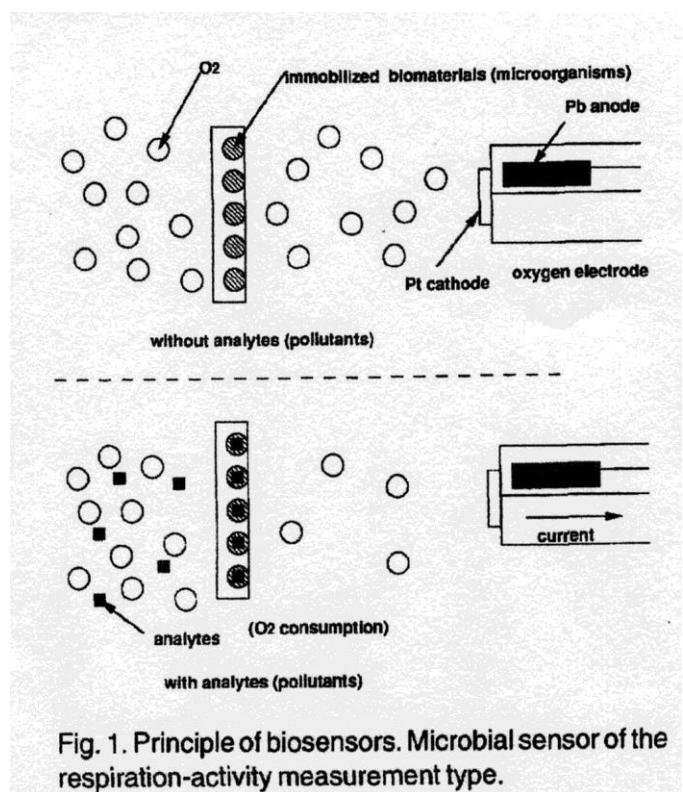
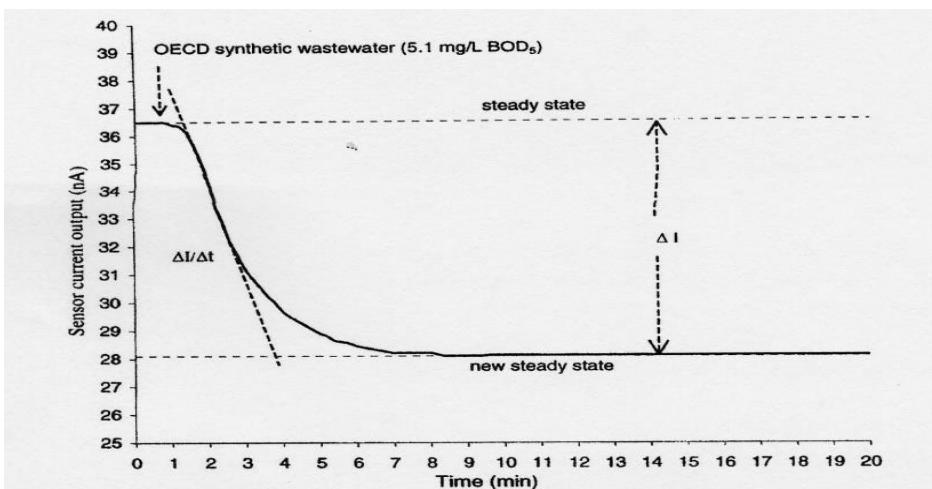
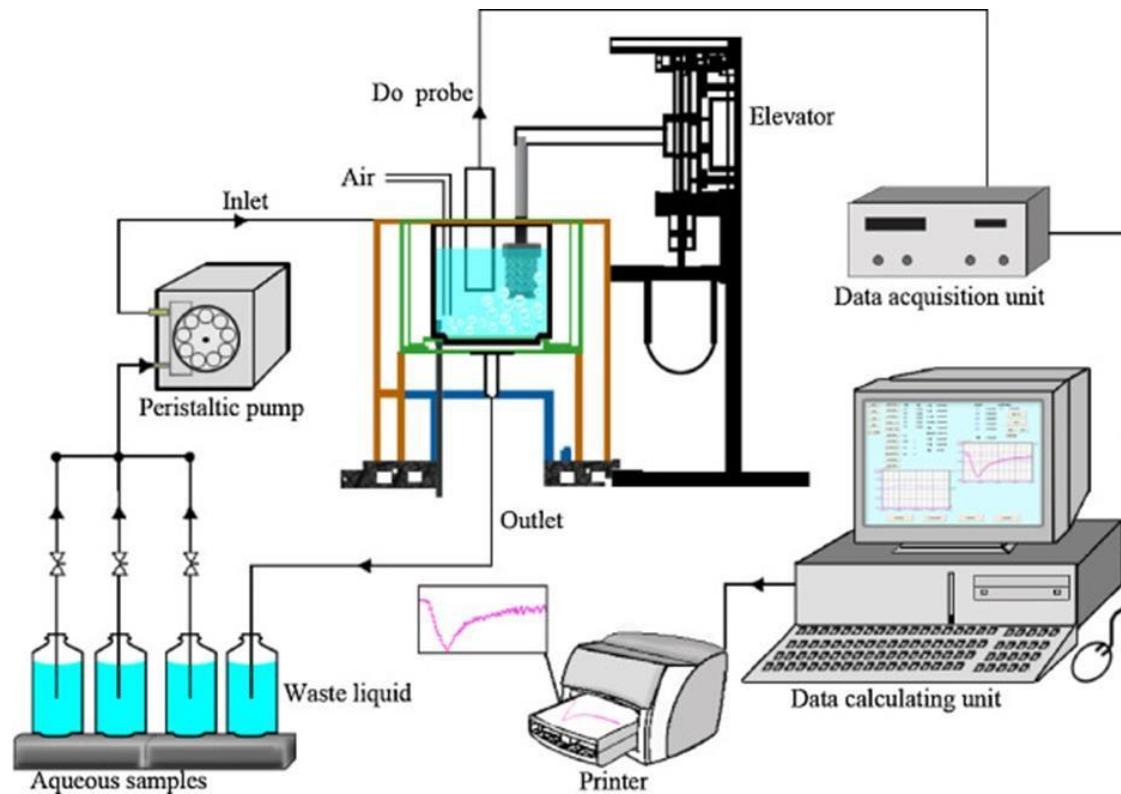
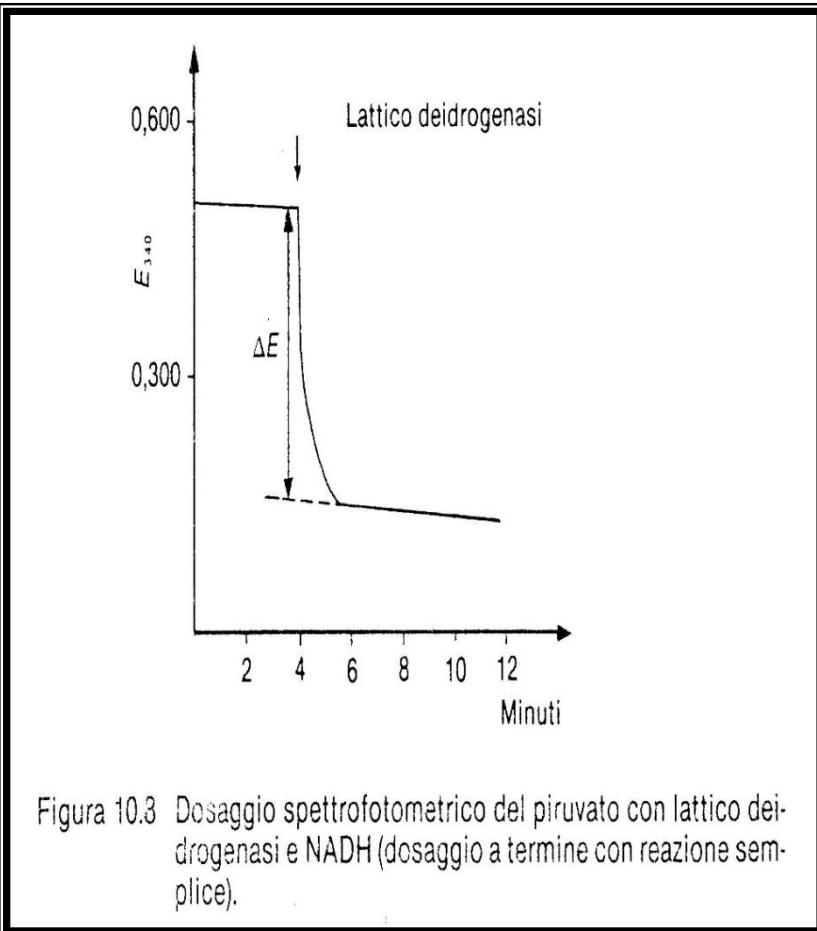


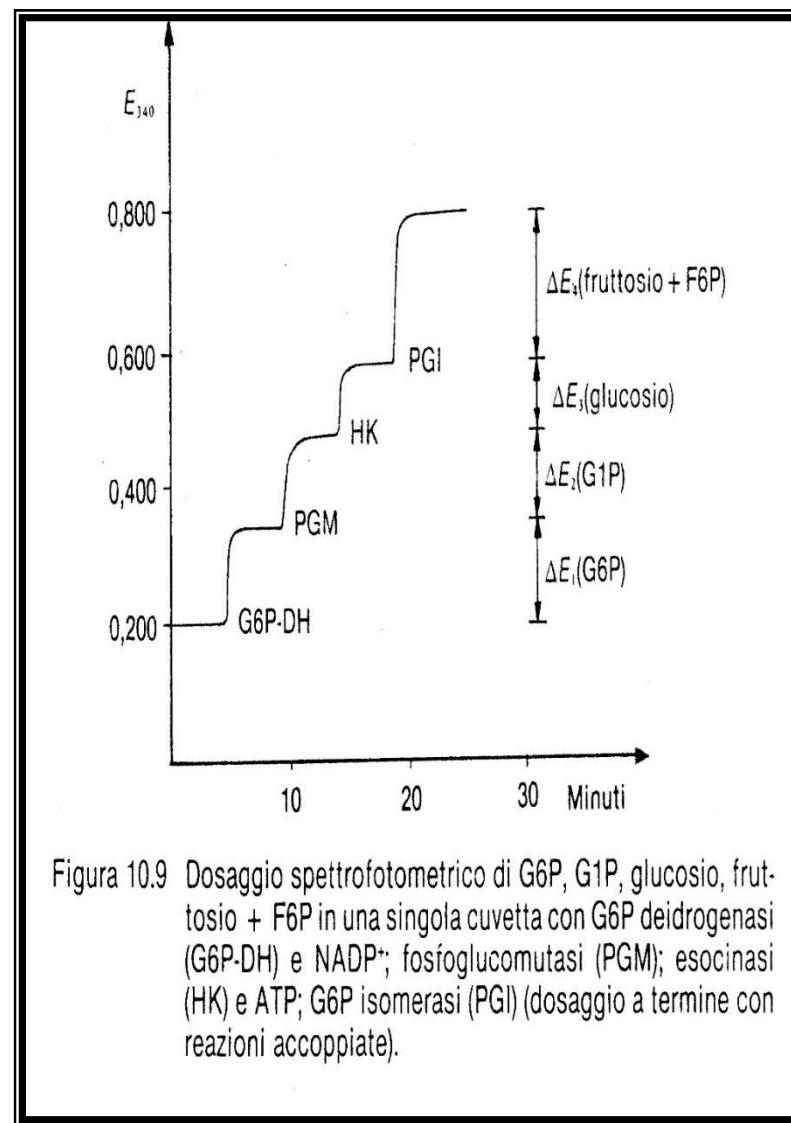
Fig. 1. Principle of biosensors. Microbial sensor of the respiration-activity measurement type.



Spectrophotometric enzymatic kits work as end-point reaction using enzymes in solution



<http://www.sigmaldrich.com/life-science/metabolomics/enzymatic-kits.html>





Food Industry

Beer and Spirits

Milk and Dairy Products

Fruits, Vegetables and Nuts

Meat, Poultry, Pork and Fish (Animal Protein)

Wine

Drinking Water



Molecular Target

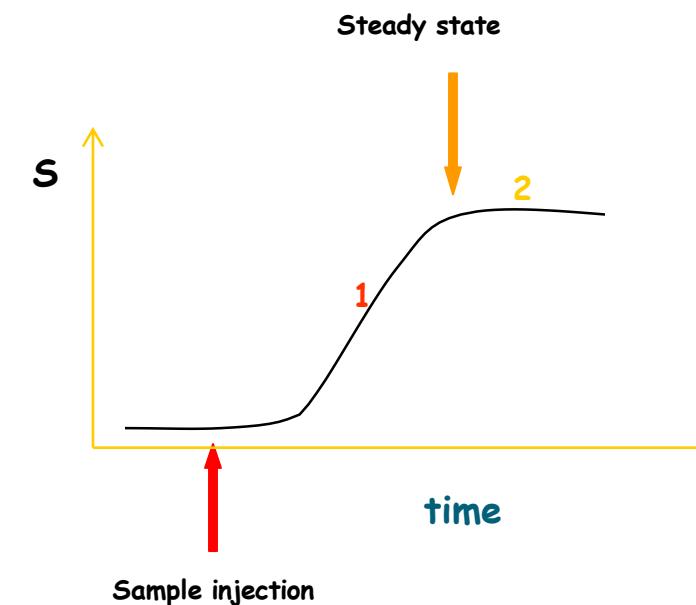
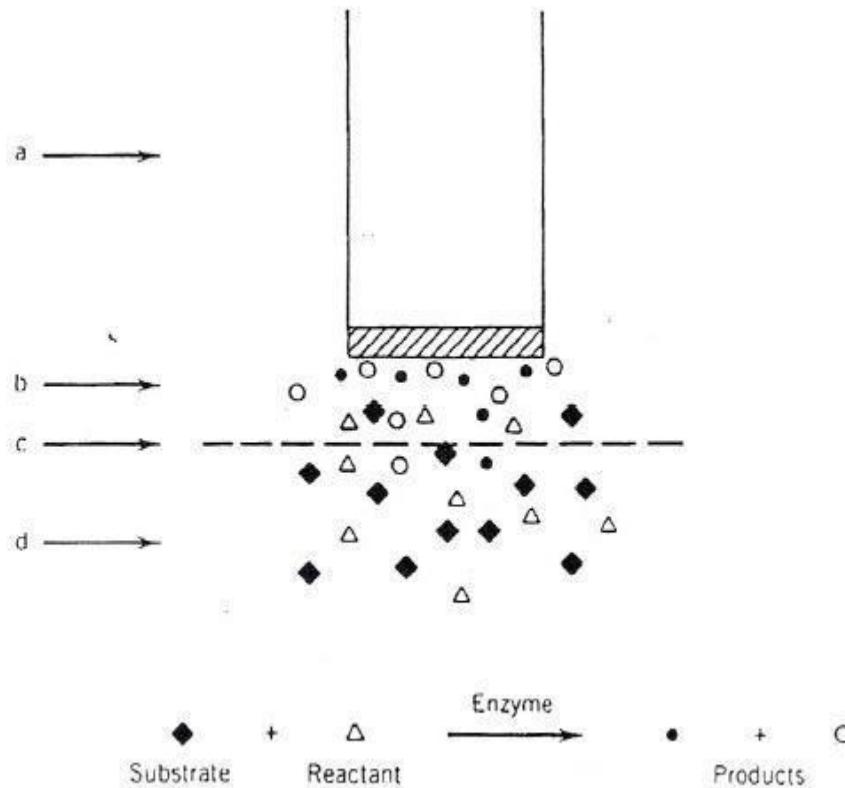
Carbohydrates and Sugars

Inorganic Ions

Lipids (Fats)

Amino Acids and Proteins

Enzyme electrode



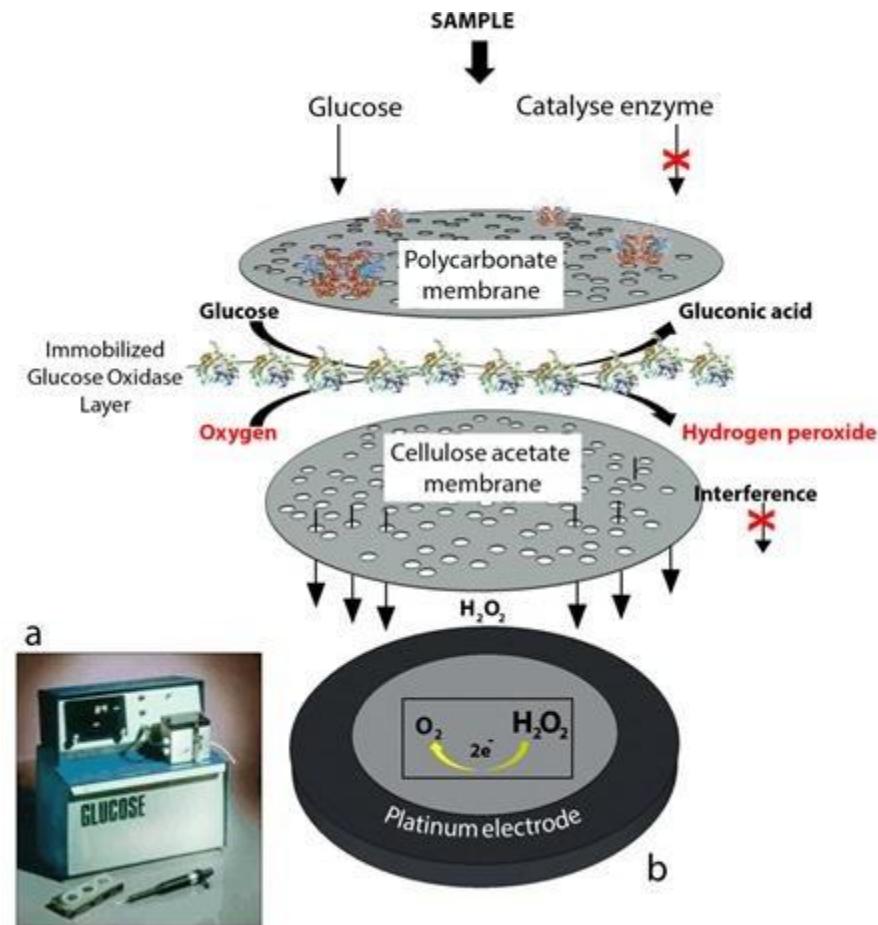
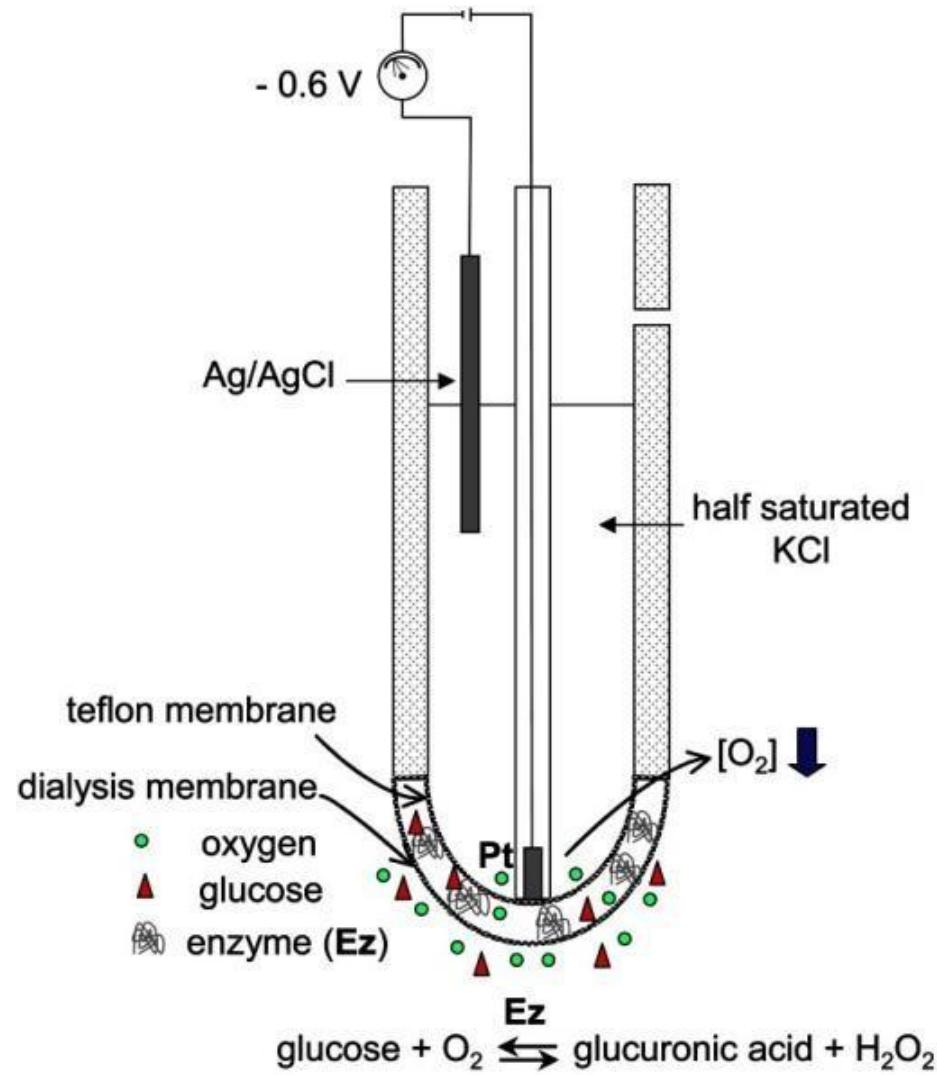
THE BIOLOGICAL ELEMENT SHOULD HAVE:

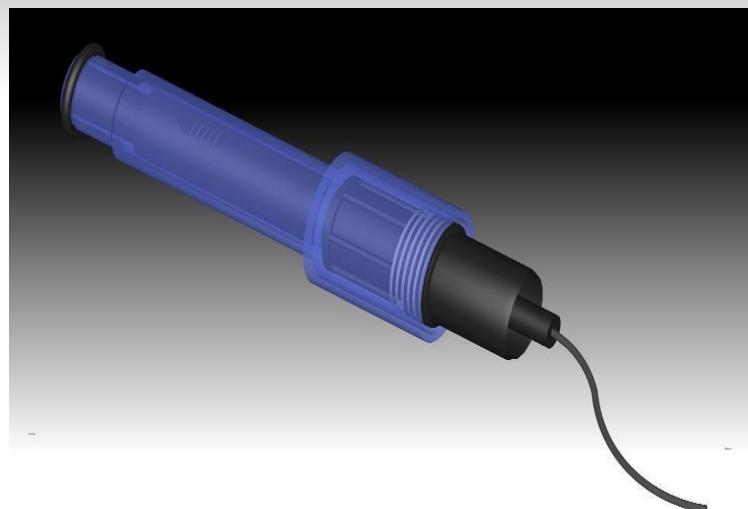
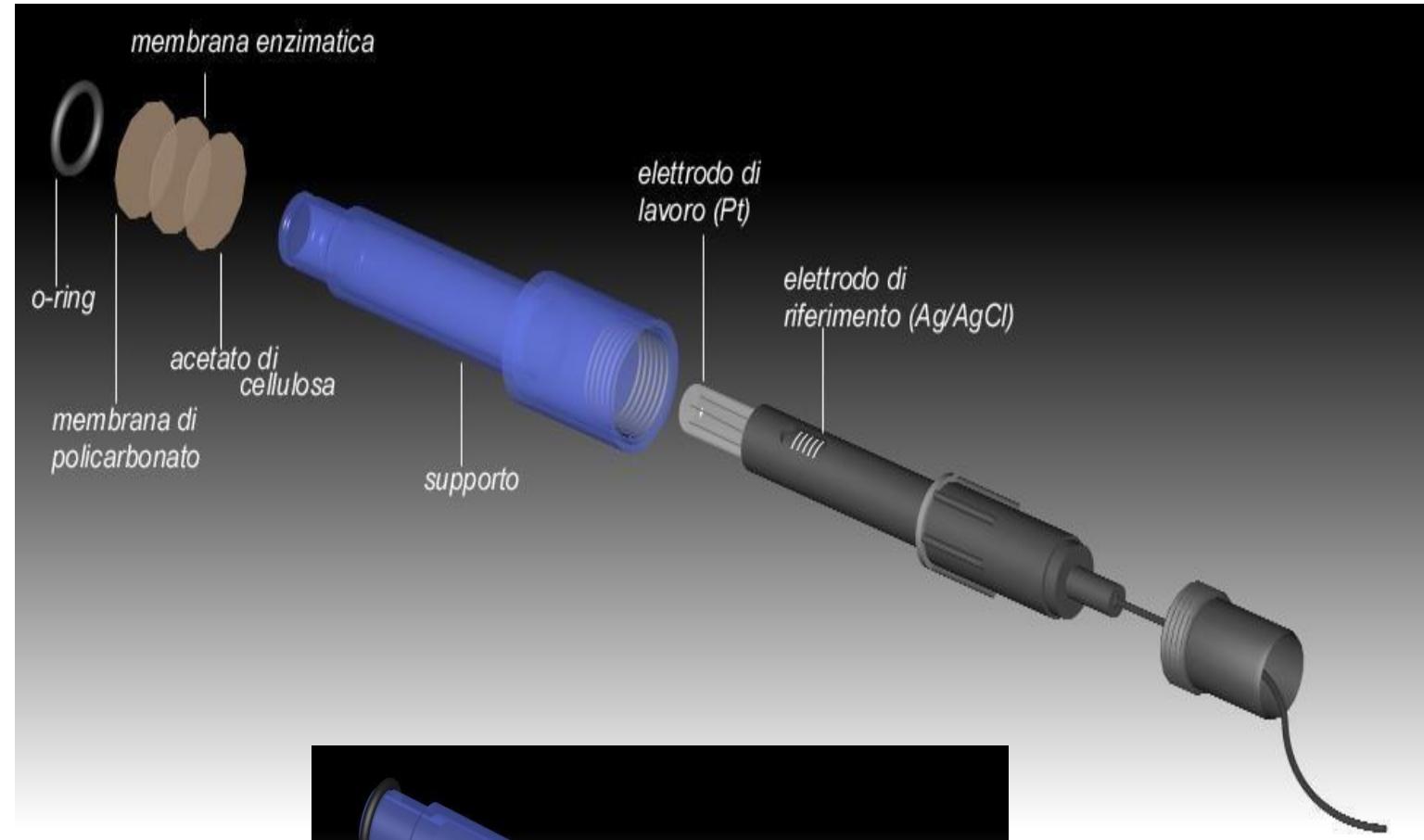
SPECIFICITY (HIGH SELECTIVITY) FOR THE ANALYTE(S)

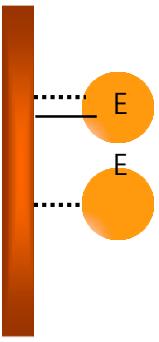
GOOD STABILITY IN OPERATING CONDITIONS (t, pH, μ)

RETENTION OF SUFFICIENT BIOLOGICAL ACTIVITY WHEN
IMMOBILISED

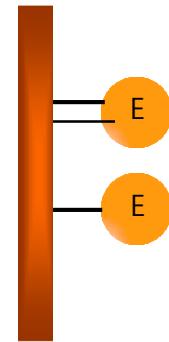
NO (VERY LOW) INHIBITION BY THE SAMPLE



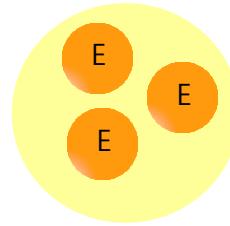




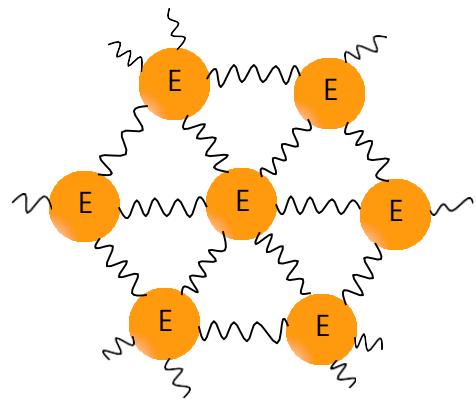
adsorption



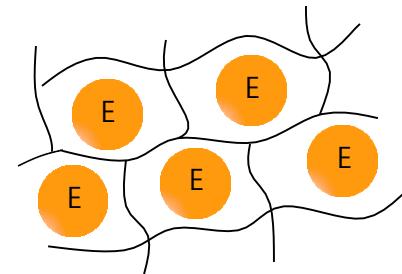
covalent
binding

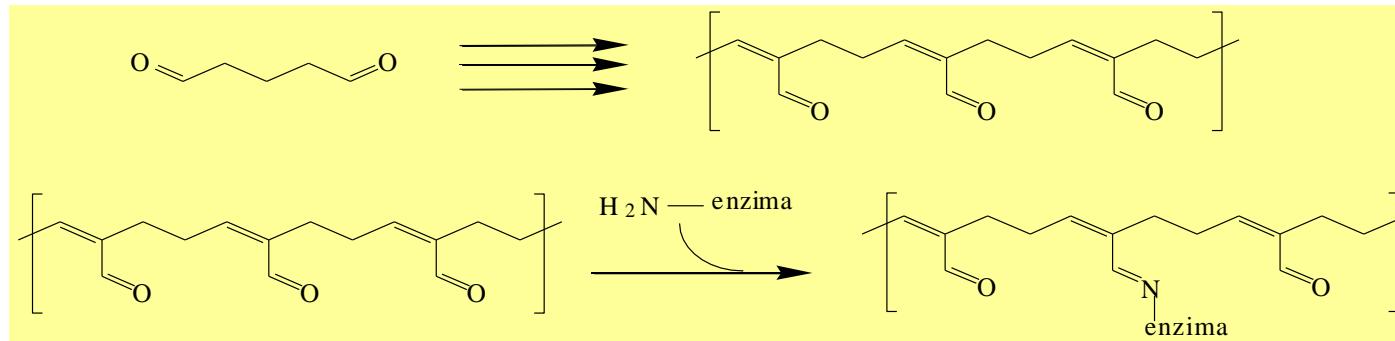


entrapment

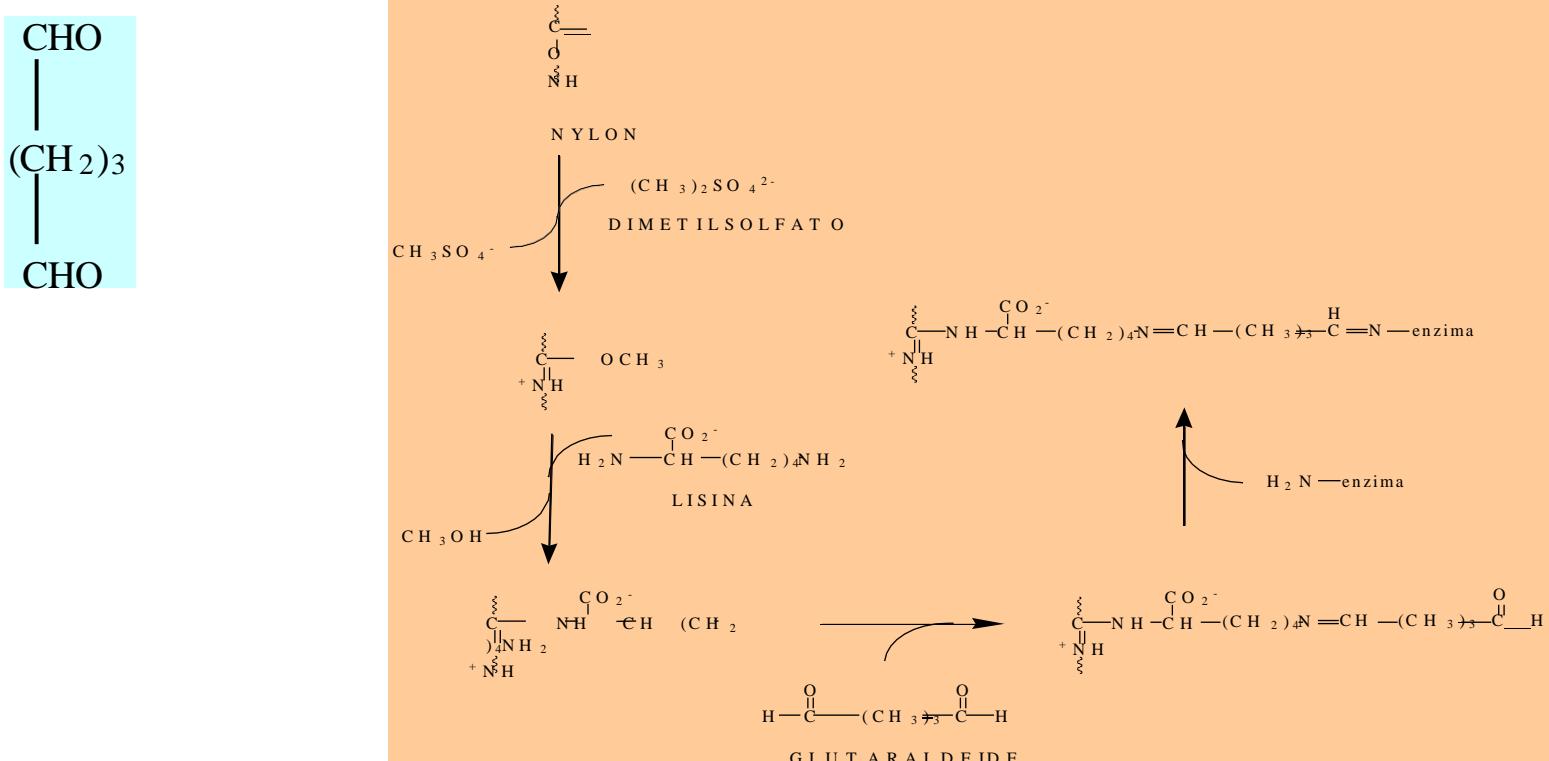


cross-linking

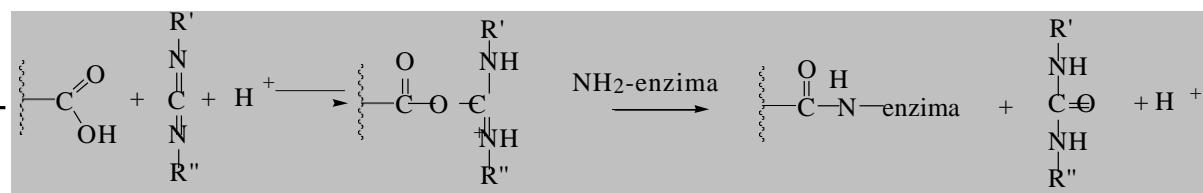


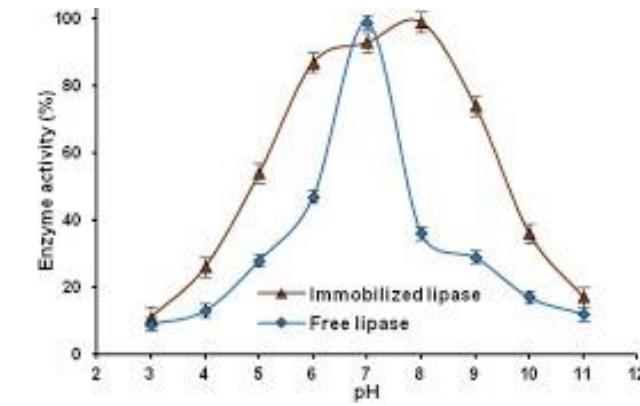
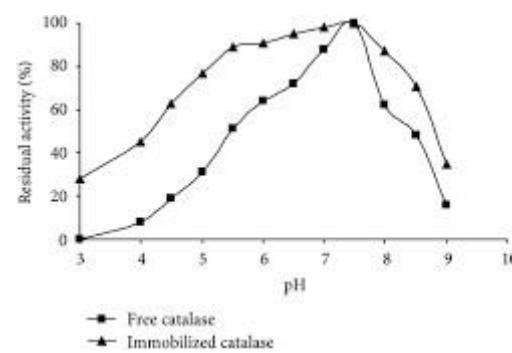
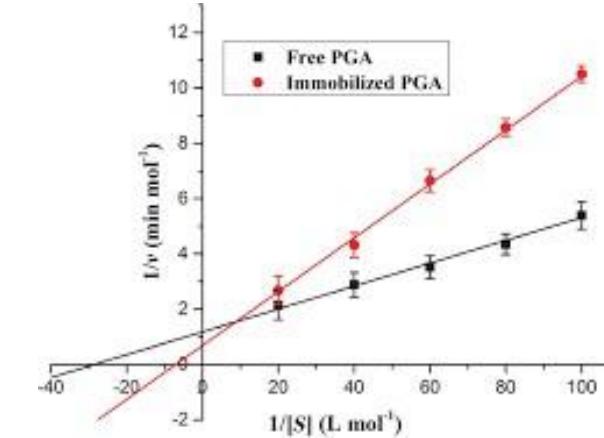
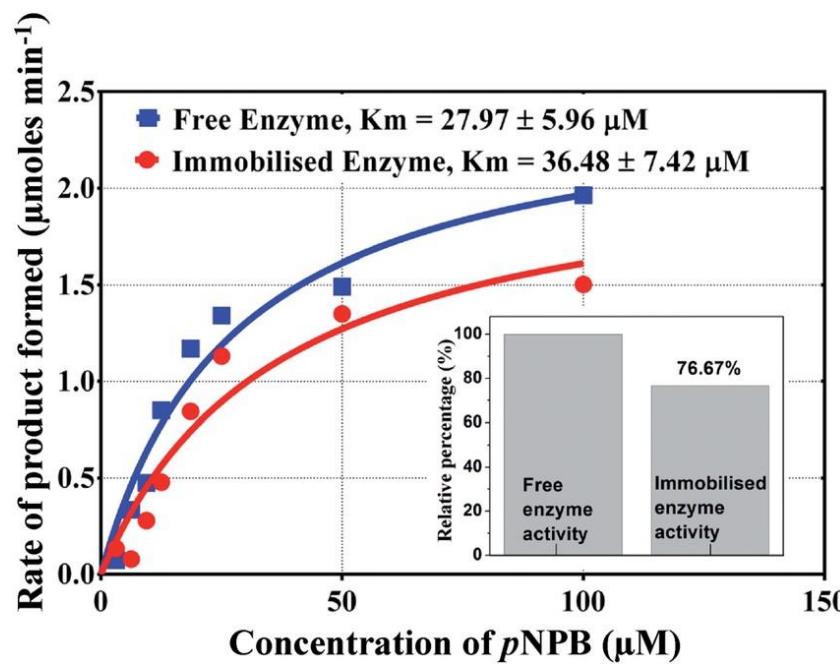


glutaraldehyde reactions: polymerization and lysine amino group



Immobilisation via carbodiimide

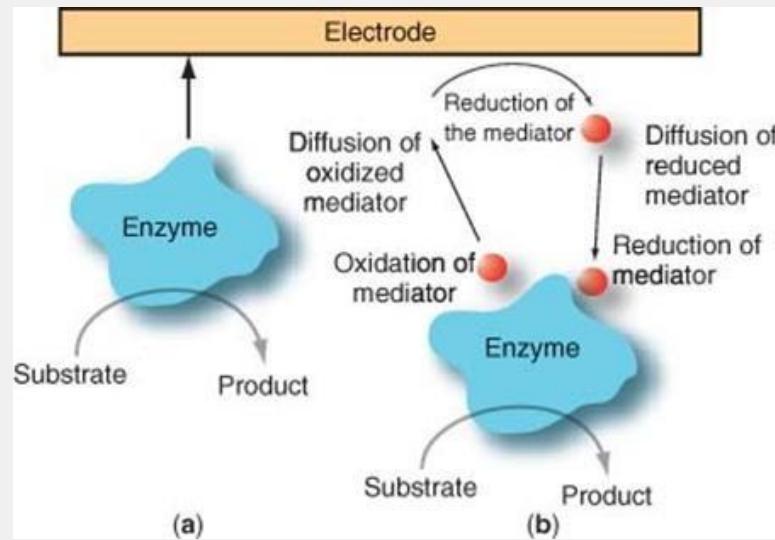




The immobilised enzyme has always a higher (apparent) K_m , a shifted and larger optimum pH and lower enzymatic activity compared to the enzyme in solution

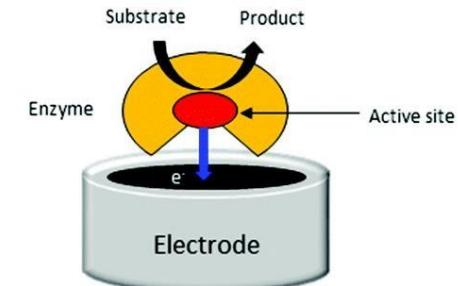
Enzyme electrodes are generally classified according to the mechanism of the electron transfer:

1. First generation: the enzyme is immobilised using a membrane that is in contact with the electrode surface. Usually there are other membranes to protect and regulate diffusion. Response time at the steady state is on the order of minutes
2. Second generation: electron transfer occurs via an electrochemical mediator in solution. The mediator shuttles electrons between the enzyme and the electrode.
3. Third generation: direct exchange of electrons between the electrode and the enzyme

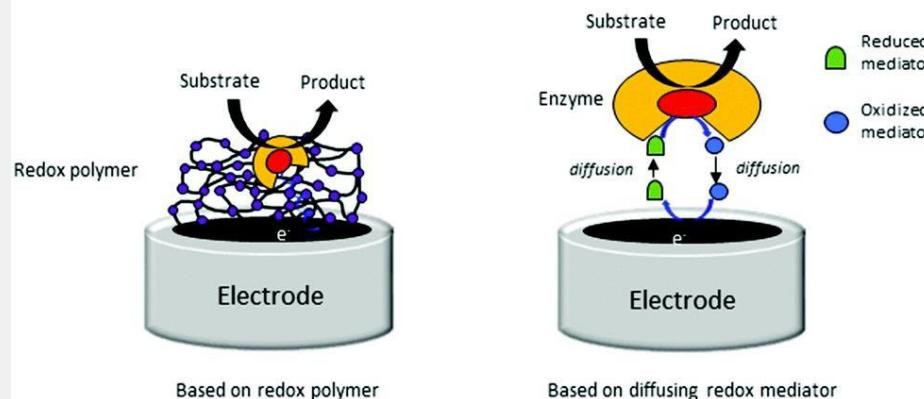


Second and third generation

Direct Electron Transfer

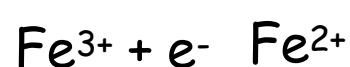


Mediated electron transfer



A good electrochemical mediator characteristics :

- rapid reaction with the enzyme
- rapid and reversible electron transfer rate
- low overpotential for the redox reaction
- pH independent
- stability in the reaction medium in both redox forms
- Should not react with the dissolved oxygen in solution
- no toxicity



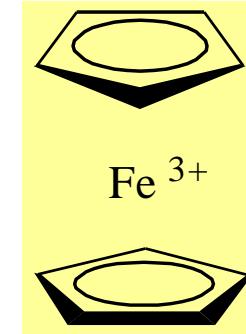
$$E^\circ = +0,53 \text{ V}$$



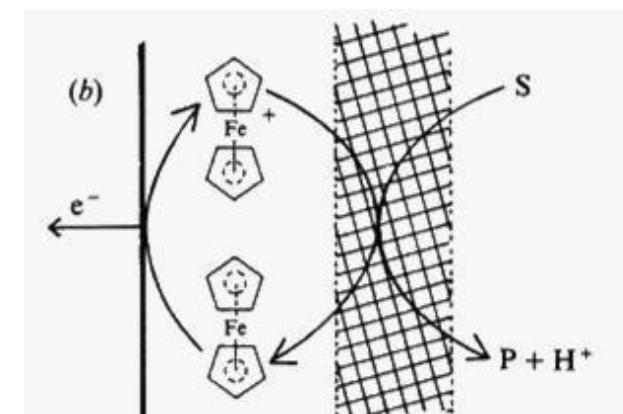
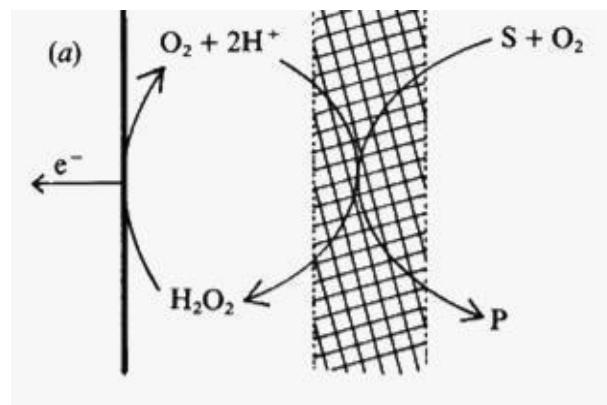
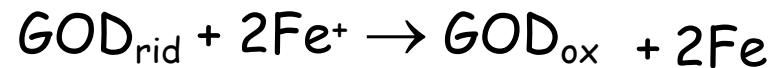
$$E^\circ = +0,45 \text{ V}$$

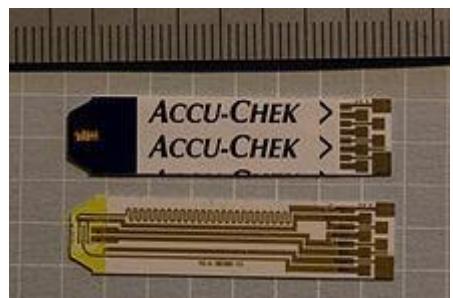
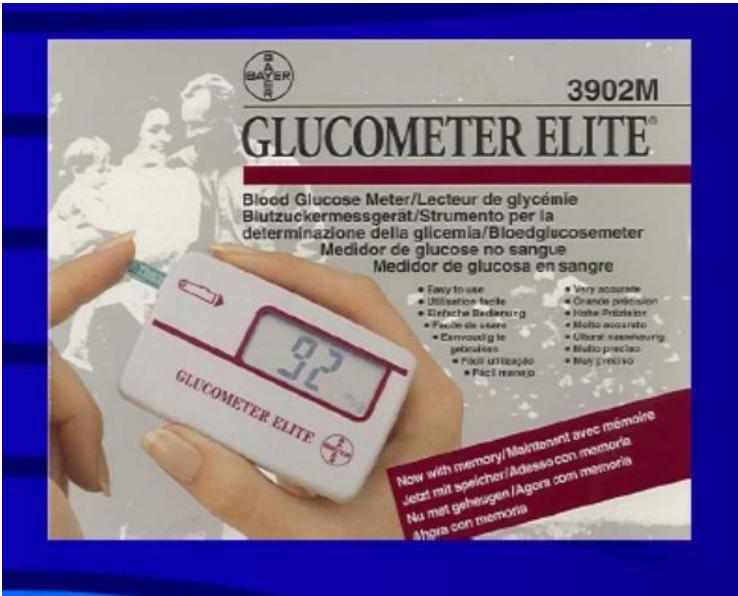


$$E^\circ = +0,165 \text{ V}$$



ferrocene is an excellent mediator for the oxidation of glucose catalysed by glucose oxidase





SIMPLE STEP BY STEP FUNCTION



1. Insert the ExacTech test strip in the meter and then place a blood sample on the target area.



2. Press the button immediately. **0 SECS**
The meter is now analysing the sample.



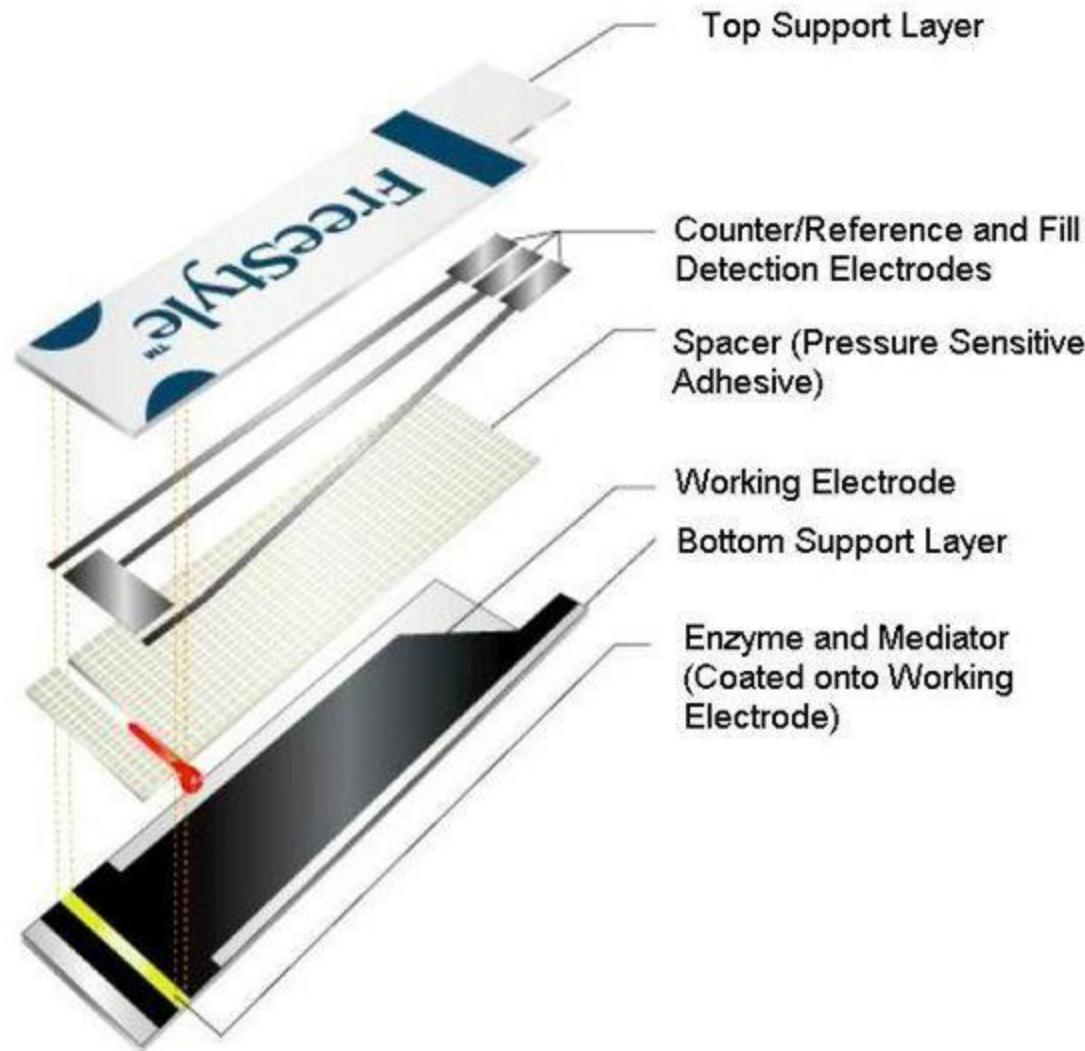
3. After a 30 second countdown, the result is displayed. **30 SECS**



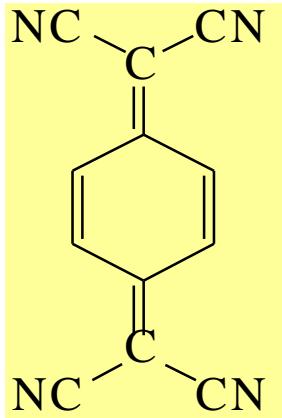
The ExacTech Blood Glucose Meter is shown Actual Size

Test Strips

- When blood added, glucose is oxidized by enzyme coated on working electrode
- Voltage applied between working and reference electrode
- Measure current between working and reference electrode

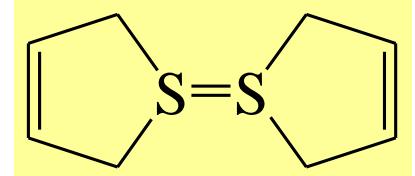


NATURAL	E(V) vs. SHC	SYNTHETIC	E (V) vs. SHC
Cytochrome a ₃	+0,29	Esacyanoferrate(III)	+0,45
Cytochrome c ₃	+0,24	2,6-dichlorophenol	+0,24
Ubiquinone	+0,10	Indophenolo	+0,24
Cytochrome b	+0,08	Ferrocene	+0,17
Vitamin K ₂	-0,03	N-metilfenazium sulphate	+0,07
Rubredoxin	-0,05	Metilene blue	+0,4
Flavoproteins	da -0,4 a +0,2	Ftalocyanin	-0,02
FAD/FADH ₂	-0,23	Fenosafranin	-0,23
FMN/FMNH ₂	-0,23	Benzyl viologen	-0,36
NAD ⁺ /NADH	-0,32	Methyl viologen	-0,46
NADP ⁺ /NADPH	-0,32		
ferredossina	-0,43		



Tetracyanochinodimethane
(TCNQ)

Third generation Conducting salts



Tetra tiafulvalene(TTF)

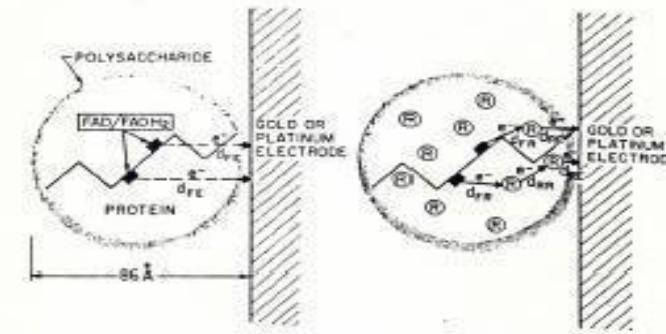
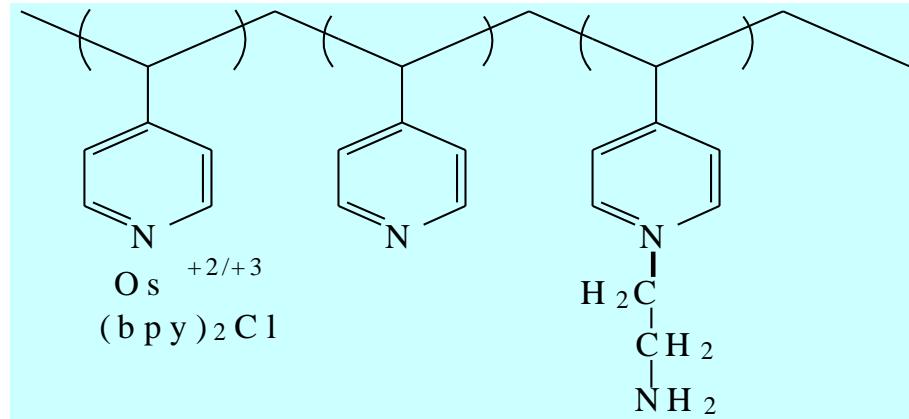


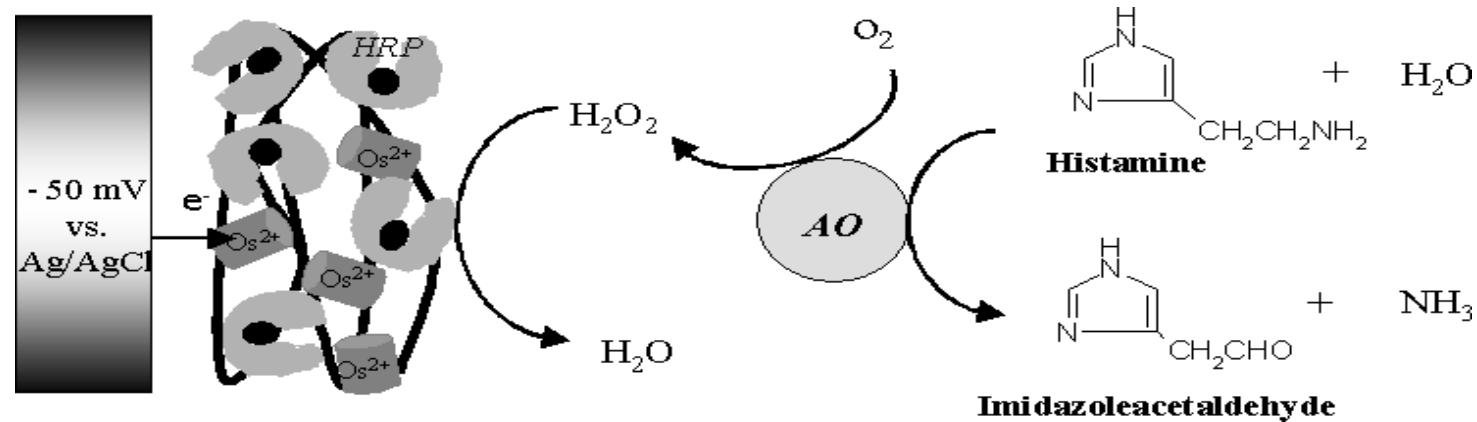
Figure 1. Schematic drawing of the glucose oxidase molecule, showing the electron-transfer distances involved in the various steps of moving an electron from its two FAD/FADH₂ centers to a metal electrode. Left: the enzyme before modification. Right: the modified enzyme, after chemical attachment of an array of electron-transfer relays.

Redox gel

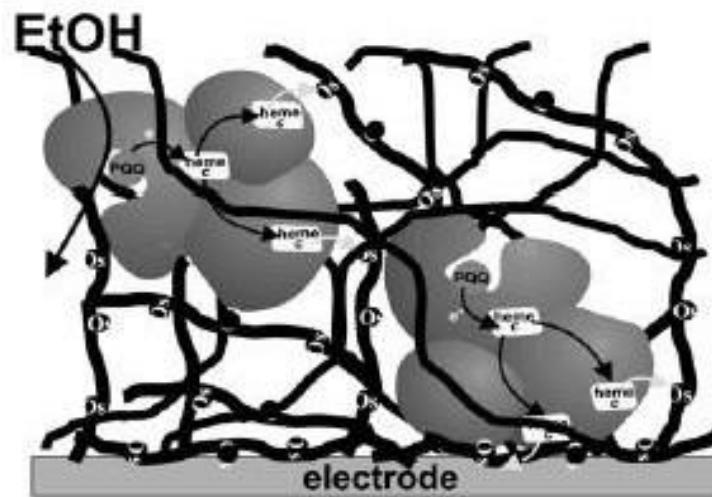


Struttura dell' osmio bipiridile legato a polivinilpiridina

Hystamine Biosensor



PQQ Alcohol Dehydrogenase
entrapped in a Os hydrogel



NAD(P)H electrodes

The largest class of redox enzymes known is dehydrogenases which use the NAD(P)H / NAD(P)⁺ couple as cofactor.

Oxidation of NADH at carbon and metal solid electrodes proceeds at high overvoltages (+400/ +700 mV vs. Ag/AgCl) via formation of the radical cation NADH^{·+}. This can give side reactions (dimerisation) and adsorb onto the electrode (carbon).

A soluble mediator can be used to lower the overpotential and increase the electron transfer rate



at the electrode surface polarised at the appropriate E :

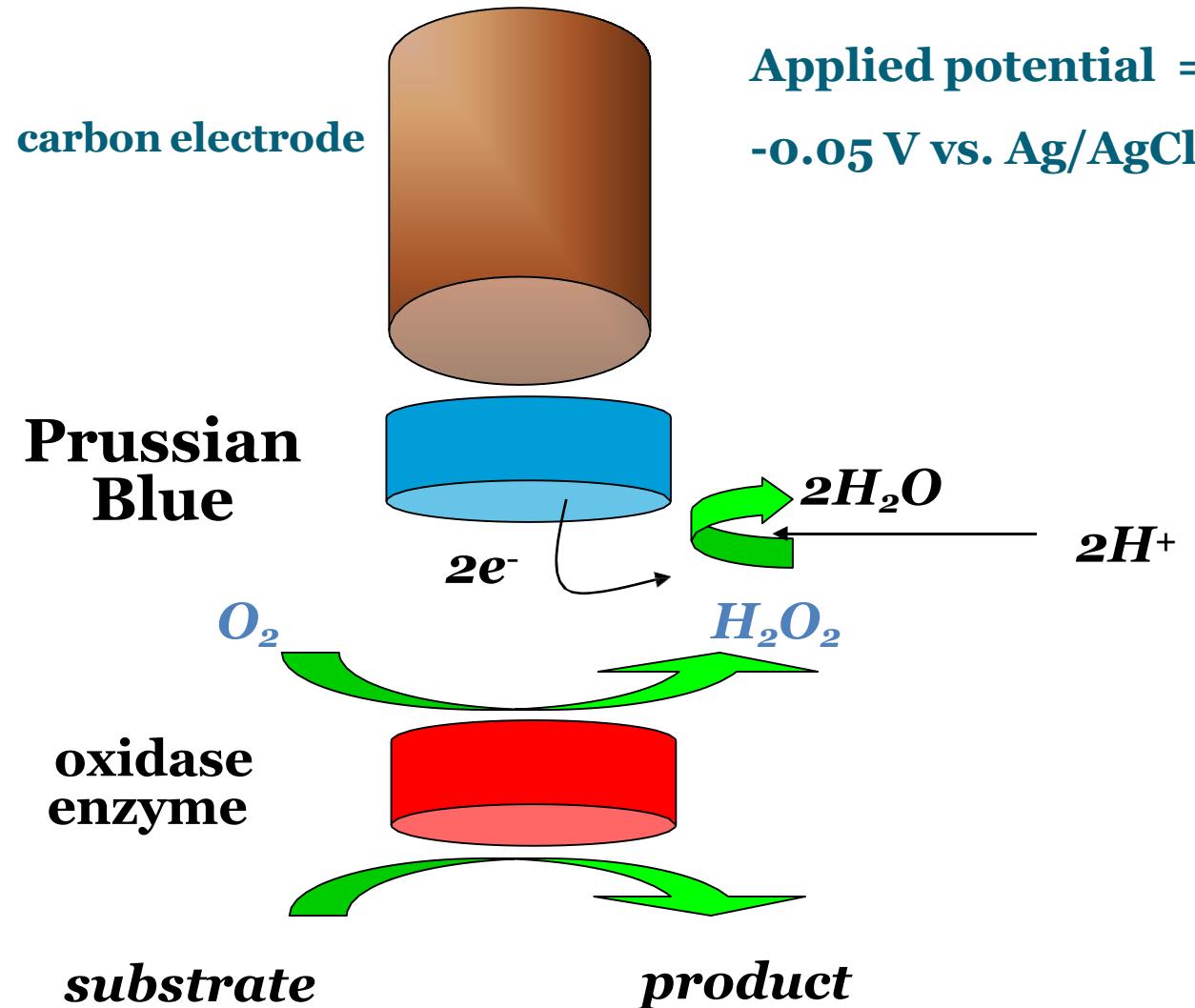


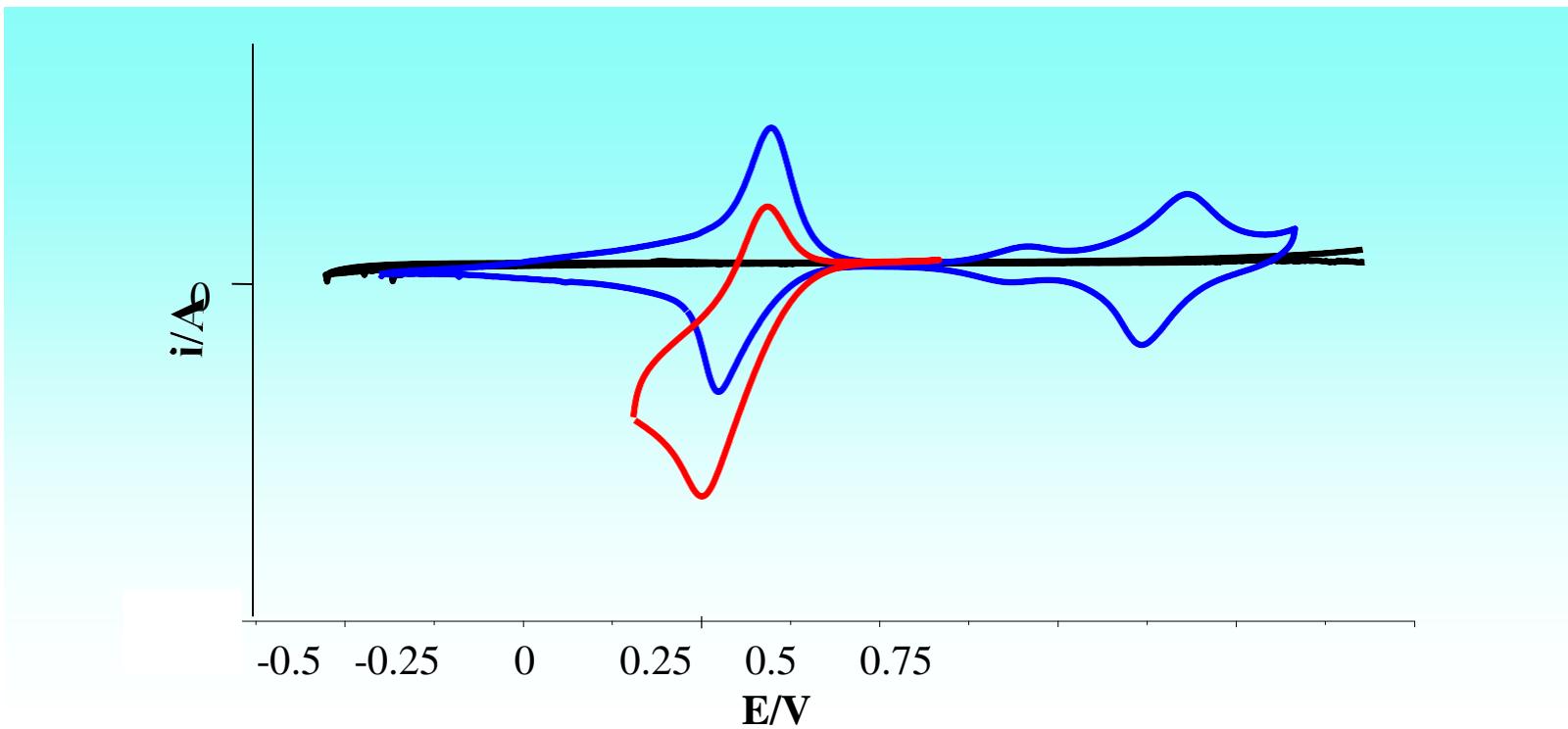
ortho- and para-quinones , quinone imines have been used and incorporated into larger molecules as indophenols, phenazines and phenoxazines

The mediator can be also immobilized at the electrode surface giving a **chemically modified electrode** for NADH

Sensitivity is excellent, major problems arise from selectivity and stability of the sensors

**Reduced Prussian Blue is a selective catalyst
for H_2O_2 reduction**



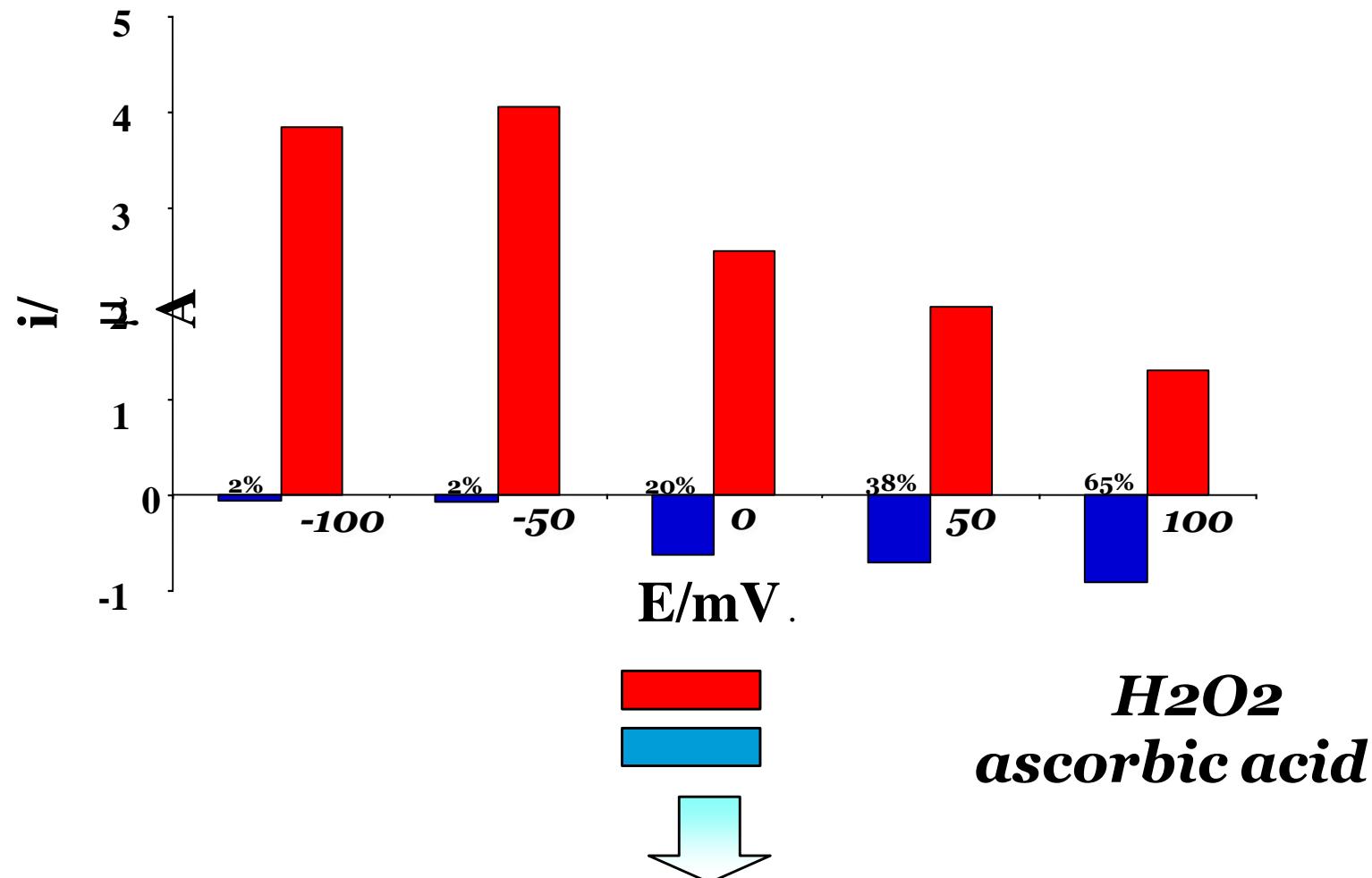


Bare electrode

Prussian Blue modified electrode

Prussian Blue modified electrode + H_2O_2

Selection of the applied potential



Potential selected - 50 mV vs. Ag/AgCl pseudo-ref.

Lysine biosensor, linear range and selectivity

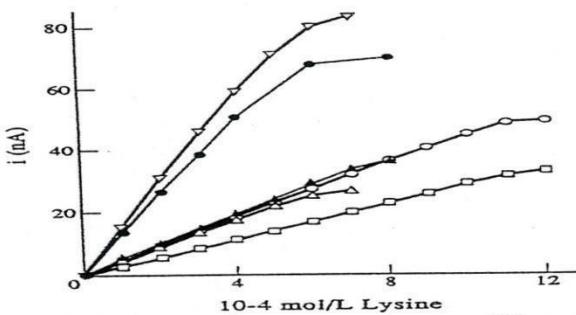


Fig. 1. Lysine calibration curves using two different immobilization procedures and protective polycarbonate membranes with different porosity. ∇ BSA/glutaraldehyde on Immobilon and 0.8- μ m polycarbonate; \bullet Immobilon only and 0.8- μ m polycarbonate; \circ BSA/glutaraldehyde on Immobilon and 0.03- μ m polycarbonate; \blacktriangle BSA/glutaraldehyde on Immobilon and 0.05- μ m polycarbonate; \triangle Immobilon only and 0.05- μ m polycarbonate; \square Immobilon only and 0.03- μ m polycarbonate. Buffer phosphate 0.1M pH 7.0 $T = 25^\circ$.

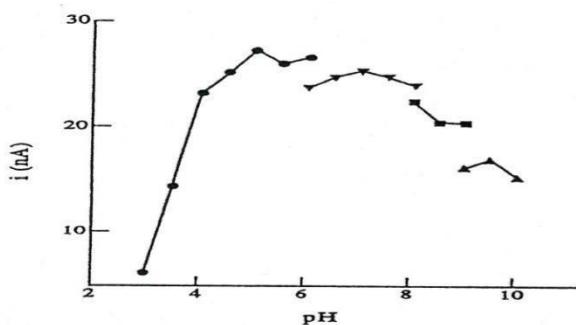


Fig. 2. Effect of pH on lysine oxidase activity. The enzyme activity was measured in the following buffers: \bullet citrate; ∇ phosphate; \blacksquare tris; \blacktriangle borax, $T = 25^\circ$.

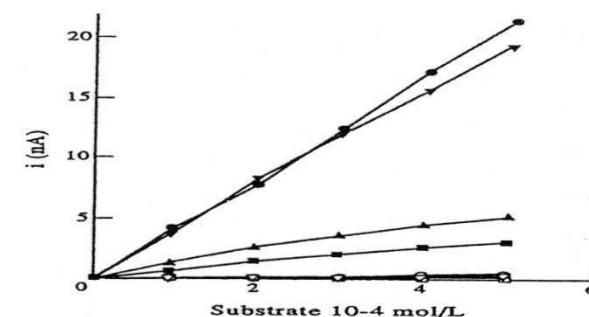
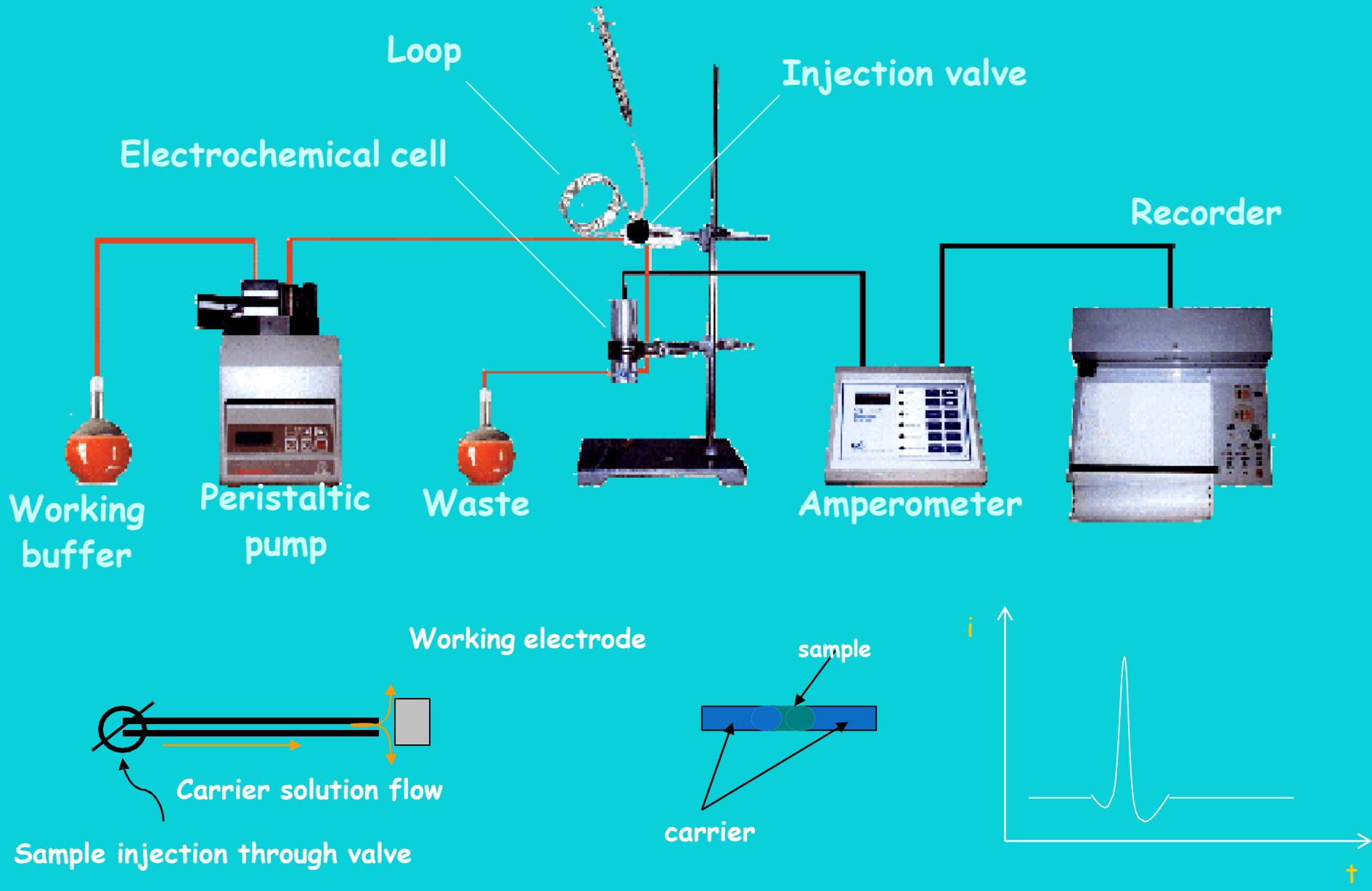


Fig. 4. Relative lysine oxidase activity toward some substrates pH 7.0 phosphate buffer $T = 25^\circ$. \bullet lysine; ∇ lysine after the analysis of other aminoacids. \blacktriangle ornithine; \blacksquare arginine; \circ tyrosine; \square phenylalanine; ∇ histidine.



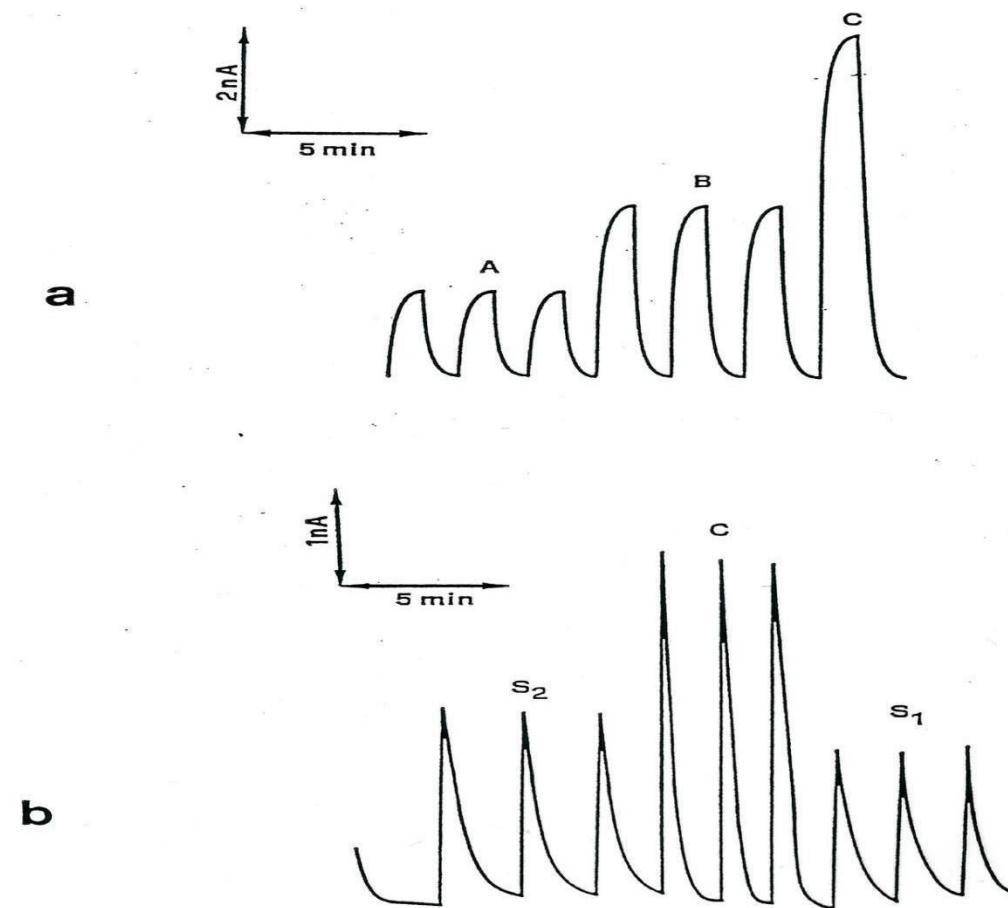


Figure 7 Reproducibility and response time of the bioprobe in flow through analysis and FIA.
a = flow through: Lysine concentration in standard solution.
A = $5 \cdot 10^{-5}$ mol/L; B = 10^{-4} mol/L; C = $2 \cdot 10^{-4}$ mol/L.
b = FIA; S₁ and S₂ foodstuff samples; C = Lysine standard $5 \cdot 10^{-4}$ mol/L.

Relative activity of 3 different purified lysine oxidase

compound	Yamasa	SIGMA	Univ. of Athens
Lysine	100	100	100
Phenylalanine	14	42	6
Arginine	2	17	0
Ornithine	3	14	0
Histidine	0	15	0
Furosine	0	0	0
Piridosine	0	0	0
Norleucine	3	17	3
AGPA*	0	0	0

Microwave hydrolysis + biosensor , analysis time 30 min

Sample	Amino-acid analysis (mM)	L-lysine biosensor (mM)	Recovery (%)
Milk	1.684	1.493 ± 0.014	88.66
pasta	0.299	0.308 ± 0.012	103.01

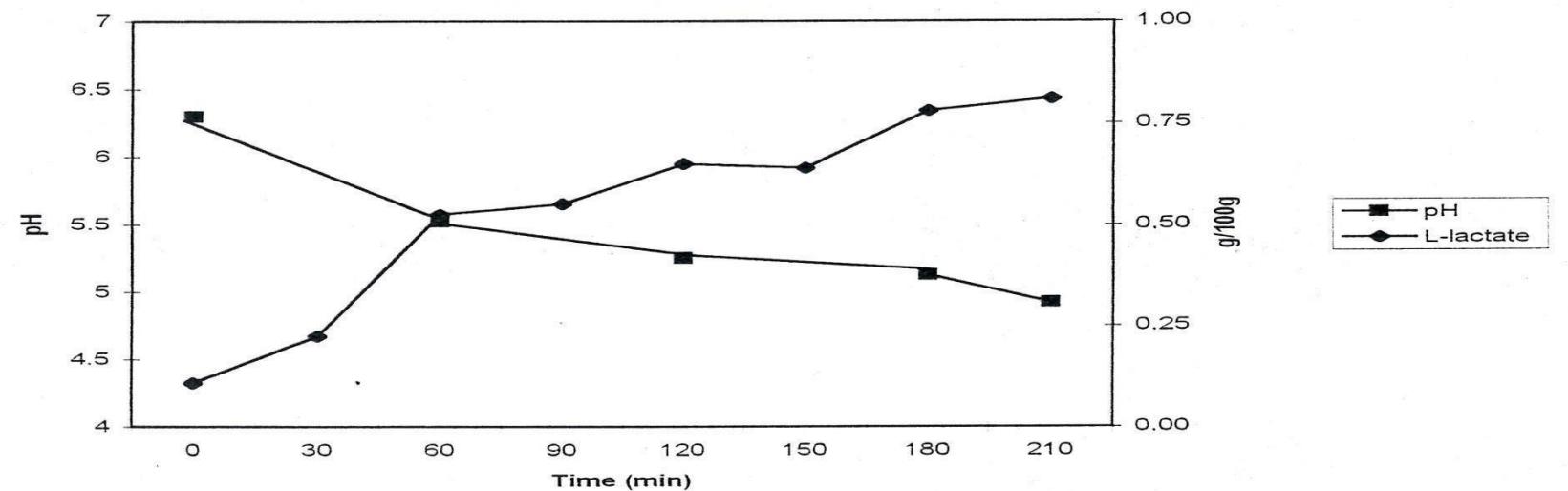
Lactic acid monitoring during mozzarella cheese manufacturing

In mozzarella cheese manufacture L-Lactic acid is the main product of lactose fermentation generated by selected cultures of lactic acid bacteria. A progressive acidification of the curd and the whey occurs and had to be carefully controlled.

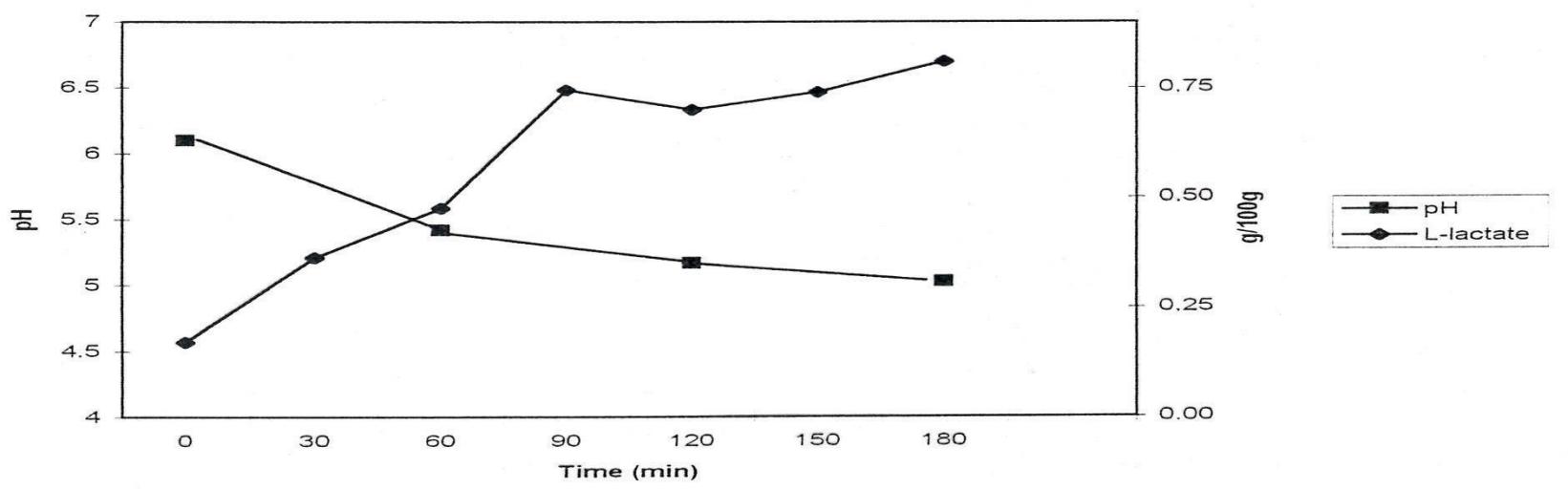
Particularly, the pH of the "stretching point" is important in order to avoid loss of fats, a decrease in yield and low reproducibility of the manufacturing.

Optimum pH is 4.9 for water-buffalo milk and 5.1 for cow milk. At these pH values there is a great increase in the buffer capacity due to casein (isoelectric point pH ~ 5) and low molecular weight acids

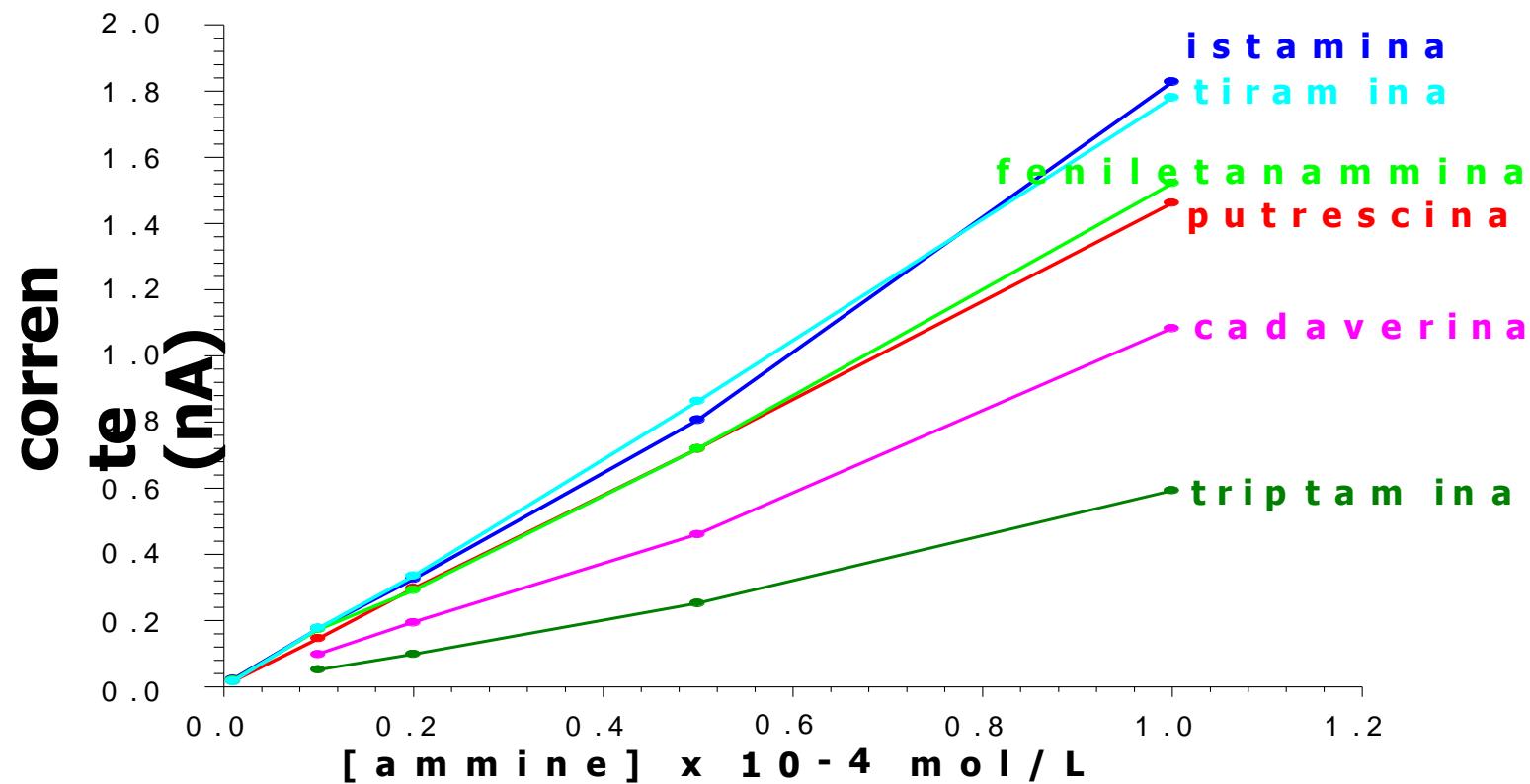
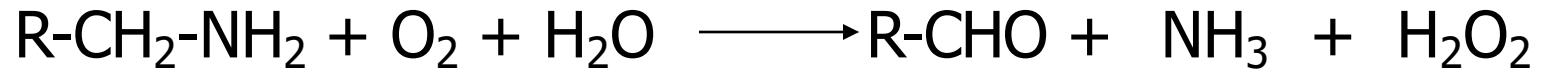
A sensitive measurement of lactic acid in real time can be useful in the optimization of the mozzarella cheese manufacture



B

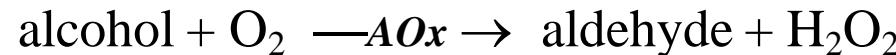


Biogenic amines



Total amines (mg/mL), expressed as equivalents of Put, measured in apricot samples using DAO biosensor^a.

		Storage time 20 days, temp. 0 ± 1°C		
variety	at harvest	LDPE	Super L	air
Pellecchiella				
ripening time I	5.6 ± 0.5	3.0 ± 0.2	2.9 ± 0.6	3.4 ± 0.6
ripening time II	5.5 ± 0.2	3.1 ± 0.4	3.0 ± 0.7	3.6 ± 0.0.2
Boccuccia				
ripening time I	5.2 ± 0.2	2.2 ± 0.1	3.7 ± 0.7	4.9 ± 0.2
ripening time II	5.1 ± 0.2	4.6 ± 0.8	4.6 ± 0.4	5.1 ± 0.1



Immobilization: PEI on Pall Immunodyne

Storage: 1% sucrose

Optimised operative conditions: 0.1 M phosphate buffer pH 7.0 + 0.02% Tween. Flow rate 1 mL/min; injection loop 500 μL .

Analytical performances:

detection limit 10^{-6} mol/L

linearity 2×10^{-6} / 10^{-3} mol/L

stability: 20% decrease after 200 samples



Immobilization: GK on aminopropyl glass beads (via glutaraldehyde), GPO on Immunodyne

Storage: DEAE-dextran/lactitol (1/5%)

Optimised operative conditions: 0.1 M borate buffer pH 8.5 + 3 mM ATP(Mg^{2+}) + 0.02% Tween. Flow rate 0.5 mL/min; injection loop 250 μL .

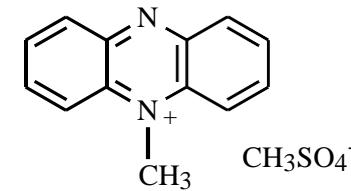
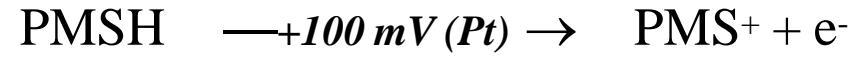
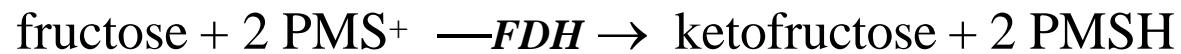
Analytical performances:

detection limit 10^{-6} mol/L

linearity 2.5×10^{-6} / 5×10^{-4} mol/L

stability: 40% decrease after 200 samples

Fructose



Immobilization: BSA-glutaraldehyde on Immobilon AV

Storage: DEAE-dextran/lactitol (1/5%)

Optimised operative conditions: 0.1 M citrate/phosphate buffer pH 4.5 + 0.02% Tween. Flow rate 0.5 mL/min; injection loop 100 µL.

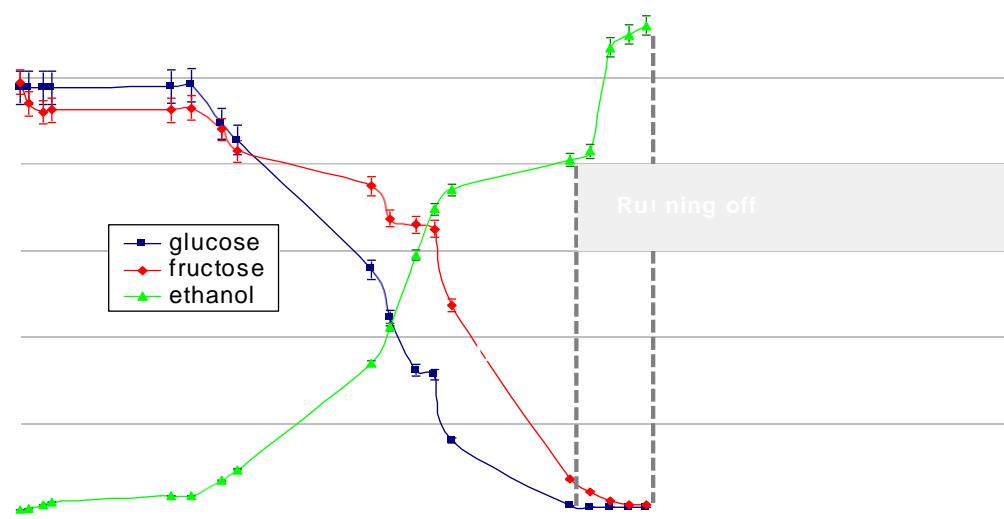
Analytical performances:

detection limit 5×10^{-7} mol/L

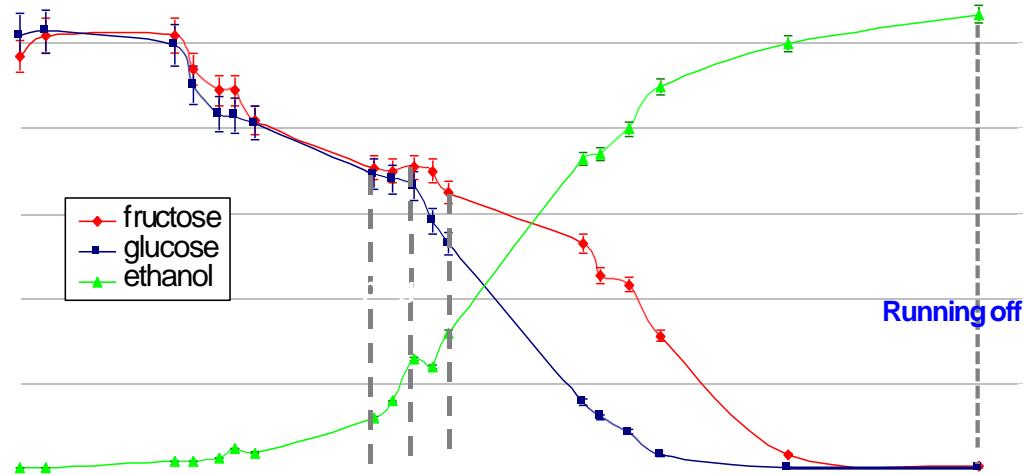
linearity 10^{-6} / 8×10^{-4} mol/L

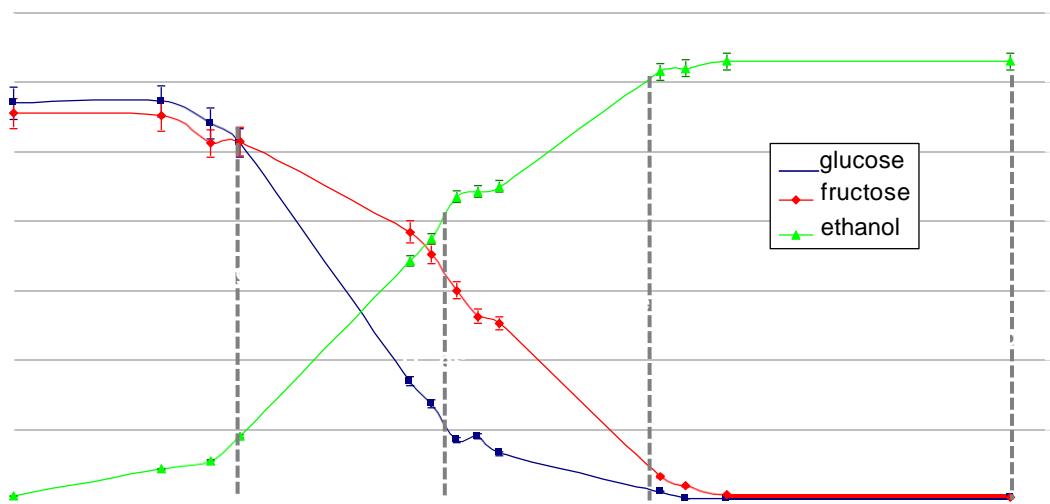
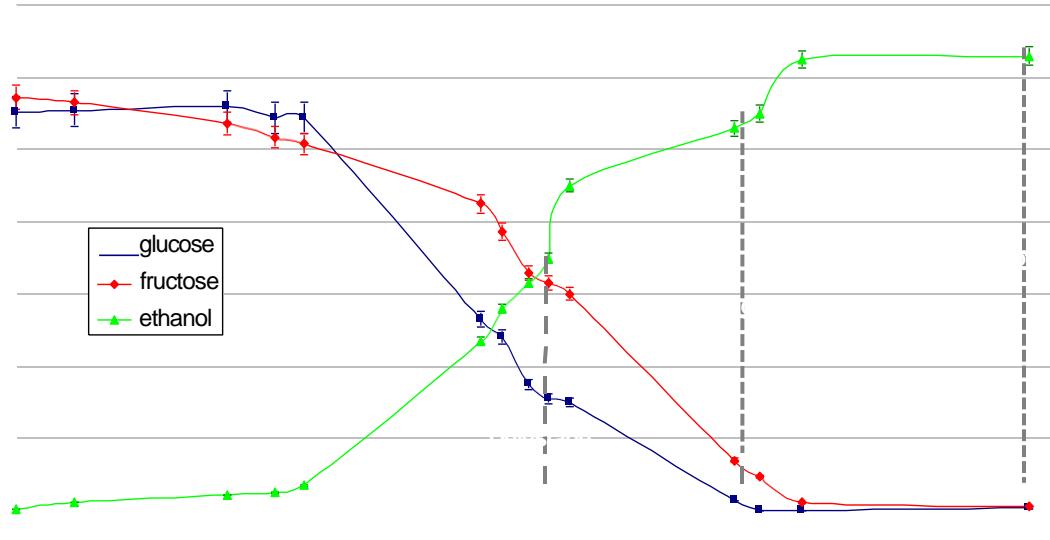
stability: 30% decrease after 200 samples

One delestage



Pumping-over





Fructose:Glucose ratio during alcoholic fermentation

