


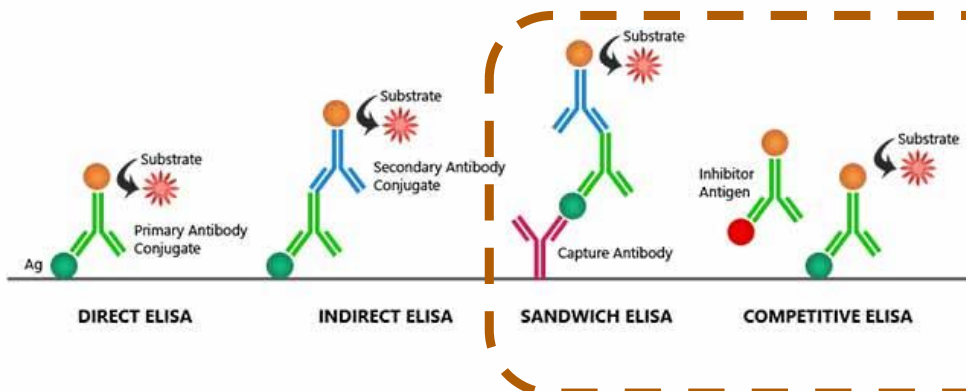
CONCENTRATION MOLES/LITER	<u>METABOLITES / IONS</u>	<u>THERAPEUTIC DRUGS</u>	<u>STEROID AND AMINO ACID HORMONES</u>	<u>PROTEIN/POLYPEPTIDE HORMONES</u>	<u>ANTIBODIES</u>
10 ⁻¹	SODIUM CHLORIDE				
10 ⁻²		ETHANOL			
(mM)	GLUCOSE				
10 ⁻³	UREA				
	CHOLESTEROL				
	CALCIUM	SALICYLATE			IgG (Total)
	TRIGLYCERIDES	ACETAMINOPHEN			
10 ⁻⁴	PHENYLANINE	THEOPHYLLINE			
10 ⁻⁵	AMMONIA	GENTAMICIN			
(μM)	IRON				
10 ⁻⁶	BILIRUBIN			THYROXINE BINDING GLOBULIN	IgM (Total)
10 ⁻⁷			T ₄ (Total)	PLACENTAL LACTOGEN	IgG (SPECIFIC)
10 ⁻⁸		DIGOXIN	CORTICOSTERONE		SYPHILIS
(nM)			T ₃ (Total)	ESTRADIOL PROGESTERONE	RUBELLA ETC.
10 ⁻⁹			T ₄ (Free)	INSULIN	
10 ⁻¹⁰			ALDOSTERONE	PARATHYROID HORMONE	IgE (Total)
10 ⁻¹¹			TSH (Thyroxine Stim. Hormone)	HGH (Growth Hormone)	
(pM)			ANGIOTENSIN	LH (Luteinizing Hormone)	
10 ⁻¹²			OXYTOCIN		
			VASOPRESSIN		

FIGURE 2. CLASSES OF CLINICALLY SIGNIFICANT ANALYTES AS A FUNCTION OF CONCENTRATION IN THE SAMPLE.

Enzyme Linked Immuno-Sorbent Assay (ELISA)

	ELISA	HPLC	LC-MS/MS
			
Price	Low	Medium	High
No. analytes per run	1 target	Multiple target	Up to 650
Accuracy	Screening	Reference method, highly sensitive and precise	Reference method (accredited results), highly sensitive and precise

Types of ELISA



Used for food and clinical analysis

Introduction to Antibodies - Enzyme-Linked Immunosorbent Assay (ELISA)

An assay for quantitating either antibody or antigen by use of an enzyme linked antibody and a substrate that forms a colored reaction product.

Enzyme-linked Immunosorbent Assays (ELISAs) combine the specificity of antibodies with the sensitivity of simple enzyme assays, by using antibodies or antigens coupled to an easily assayed enzyme that possesses a high turnover number. ELISAs can provide a useful measurement of antigen or antibody concentration.

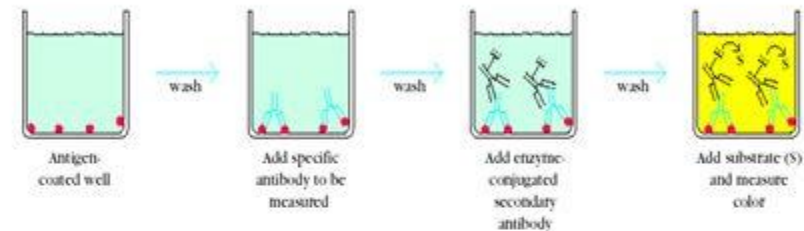
Sandwich ELISA Assays

To utilize this assay, one antibody (the “**capture**” antibody) is purified and bound to a solid phase typically attached to the bottom of a plate well. Antigen is then added and allowed to complex with the bound antibody. Unbound products are then removed with a wash, and a labeled second antibody (the “**detection**” antibody) is allowed to bind to the antigen, thus completing the “sandwich”. The assay is then quantitated by measuring the amount of labeled second antibody bound to the matrix, through the use of a colorimetric substrate. Major advantages of this technique are that the antigen does not need to be purified prior to use, and that these assays are very specific. However, one disadvantage is that not all antibodies can be used. Monoclonal antibody combinations must be qualified as “**matched pairs**”, meaning that they can recognize separate epitopes on the antigen so they do not hinder each other’s binding

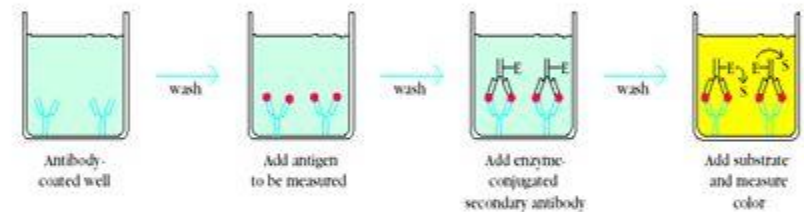
Competitive ELISA Assays

Briefly, an unlabeled purified primary antibody is coated onto the wells of a 96 well microtiter plate. This primary antibody is then incubated with unlabeled standards and unknowns. After this reaction is allowed to go to equilibrium, conjugated immunogen is added. This conjugate will bind to the primary antibody wherever its binding sites are not already occupied by unlabeled immunogen. Thus, the more immunogen in the sample or standard, the lower the amount of conjugated immunogen bound. The plate is then developed with substrate and color change is measured.

(a) Indirect ELISA



(b) Sandwich ELISA



(c) Competitive ELISA

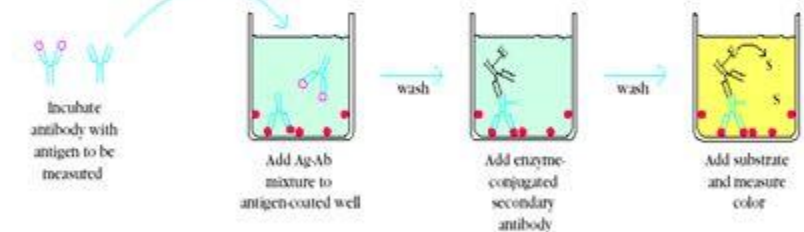
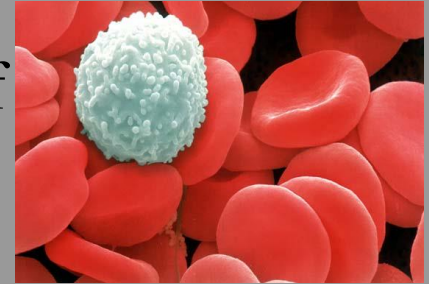


FIGURE 1.10 Variations in the enzyme-linked immunosorbent assay (ELISA) technique allow determination of antibody or antigen. Each assay can be used qualitatively, or quantitatively by comparison with standard curves prepared with known concentrations of antibody or antigen. Antibody can be determined with an indirect ELISA

(a), whereas antigen can be determined with a sandwich ELISA (b) or competitive ELISA (c). In the competitive ELISA, which is an inhibition-type assay, the concentration of antigen is inversely proportional to the color produced.

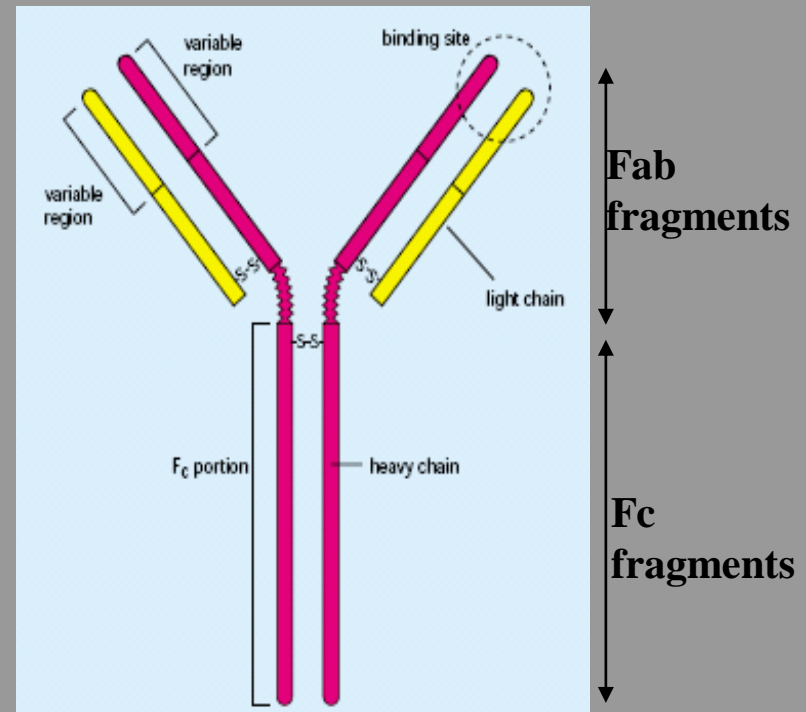
Antibodies

- Proteins secreted by B-lymphocytes (type of white blood cell), in vertebrates.



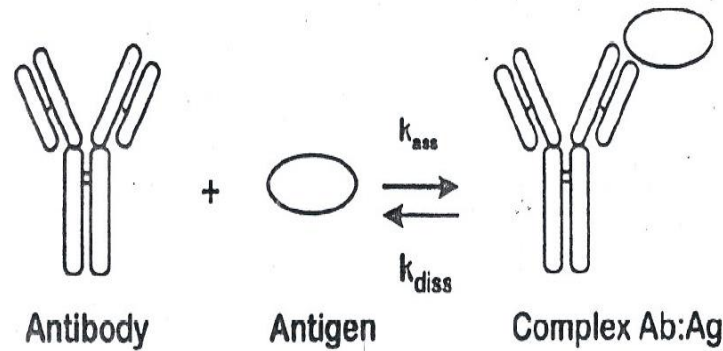
- Recognise and bind to molecules (**antigens**) on foreign particles, marking them for destruction by T-lymphocytes.

- Each antigen may generate several antibodies for different sites (**epitopes**) on antigen.



IgG molecule

Antibody - Antigen interaction

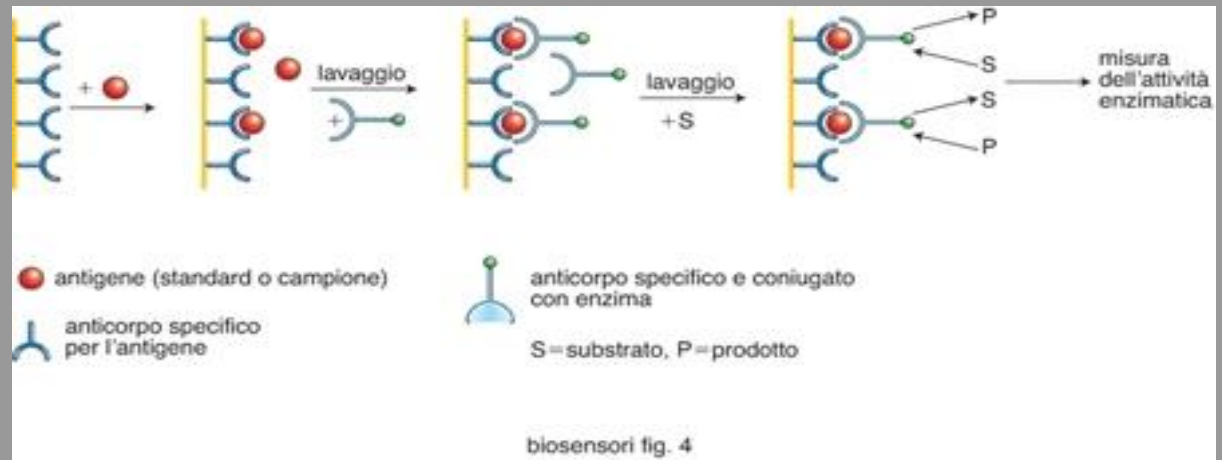


$$v = \frac{d[Ab:Ag]}{dt} = k_{ass} [Ab][Ag] - k_{diss} [Ab:Ag]$$

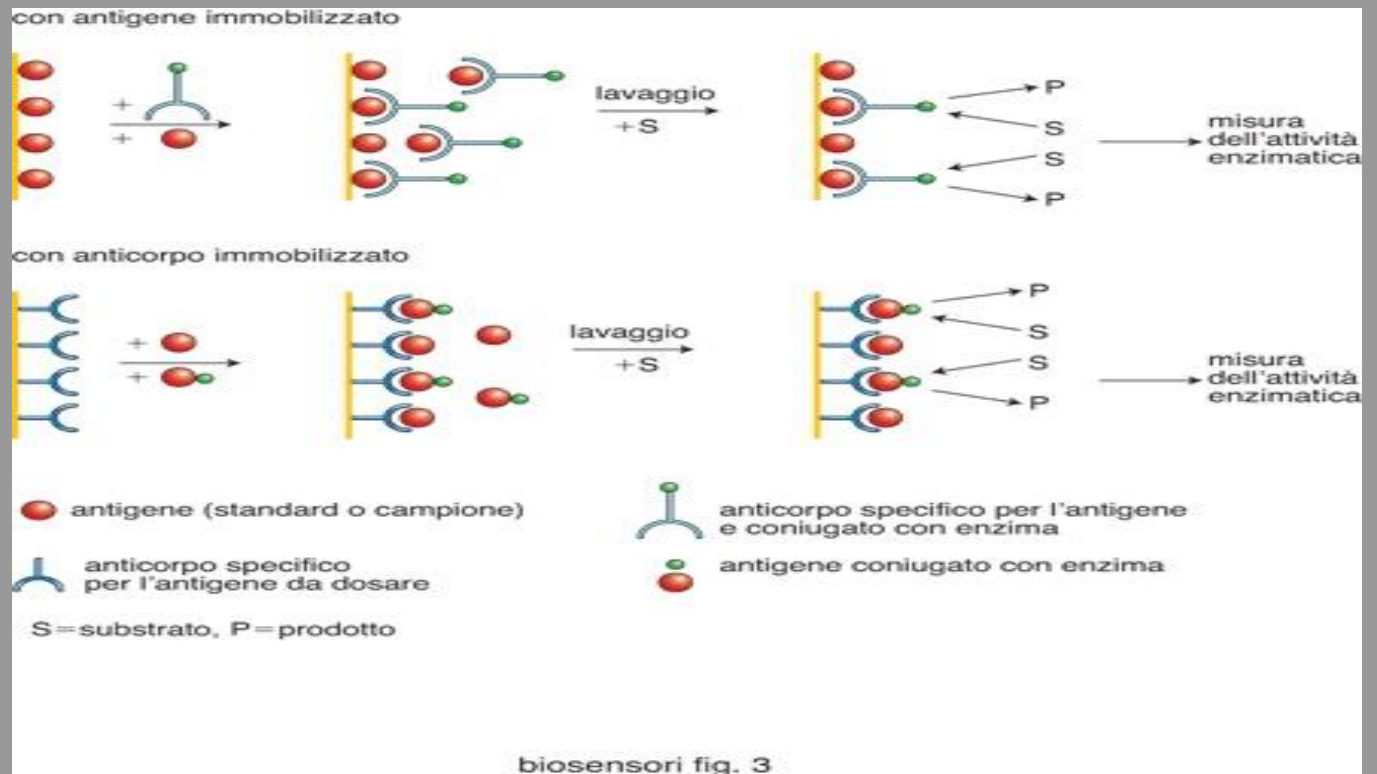
Equilibrium: $\frac{d[Ab:Ag]}{dt} = 0$ and $K_{aff} = \frac{k_{ass}}{k_{diss}} = \frac{[Ab:Ag]}{[Ab][Ag]}$

- Non - covalent
- Highly specific
- $k_{ass} \approx 10^6 - 10^8 \text{ M}^{-1}\text{s}^{-1}$
- $k_{diss} \approx 10^{-1} - 10^{-4} \text{ s}^{-1}$
- $K_{aff} \approx 10^6 - 10^{12} \text{ M}^{-1}$

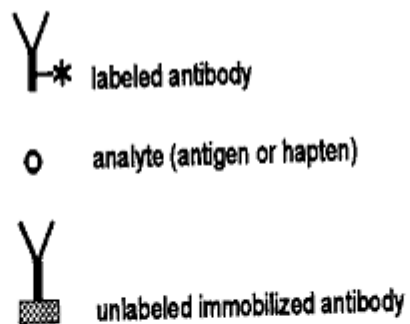
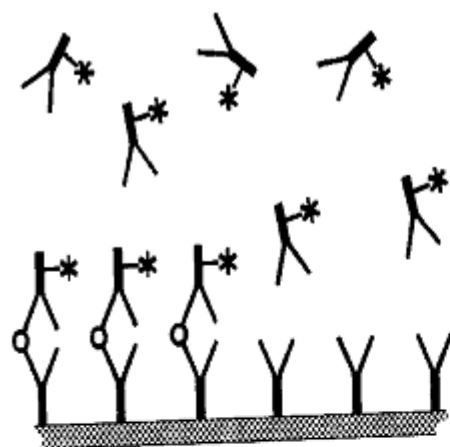
Dosaggi Non competitivi (sandwich)



Dosaggi competitivi



a) Non-competitive assays (antibody excess)



b)

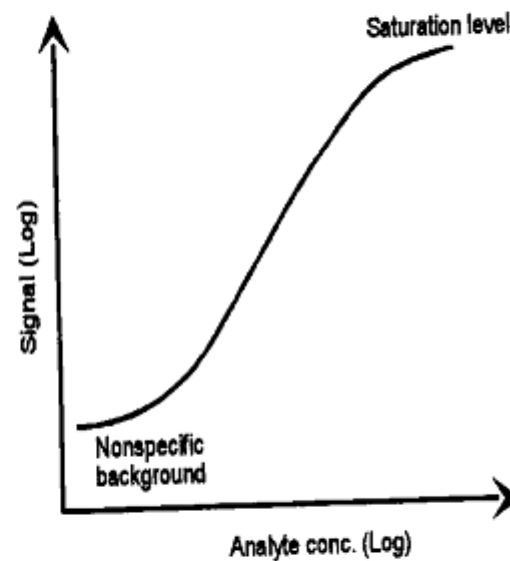


FIGURE 17.3 Schematic drawing of a sandwich immunoassay with typical calibration curve.

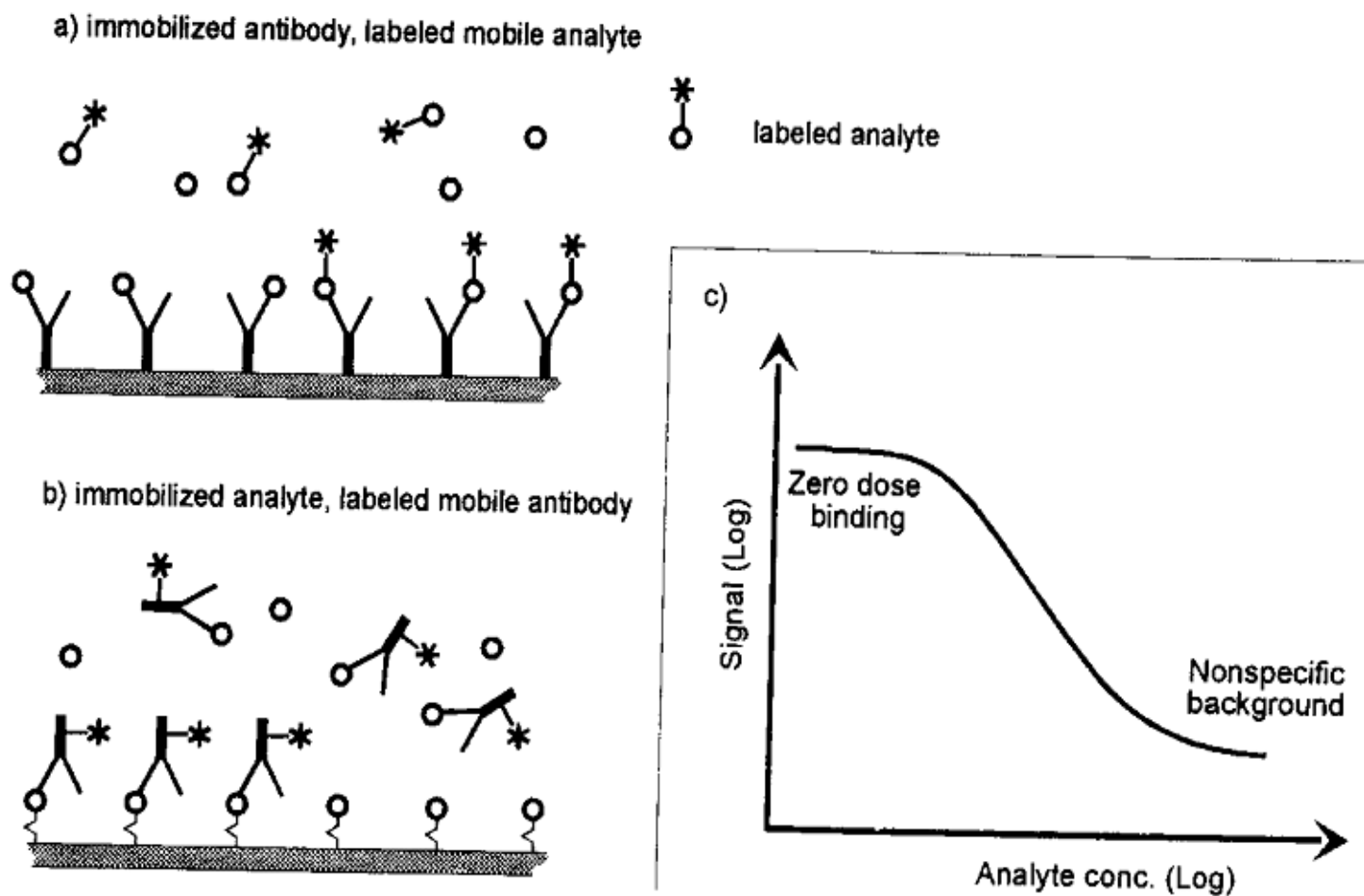


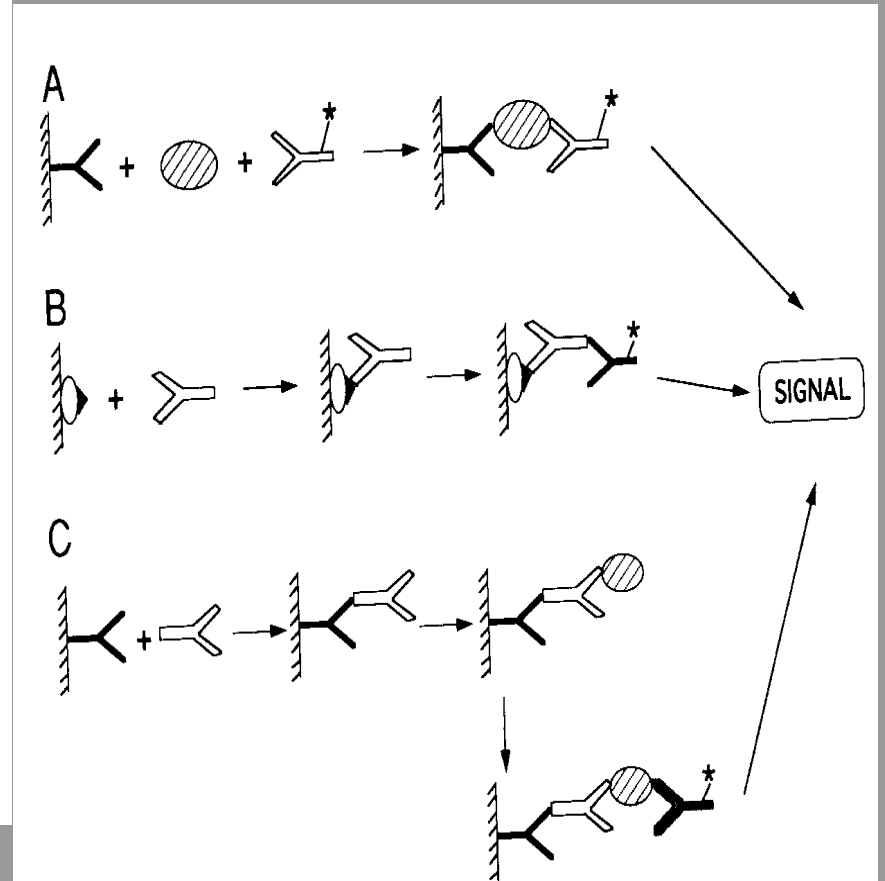
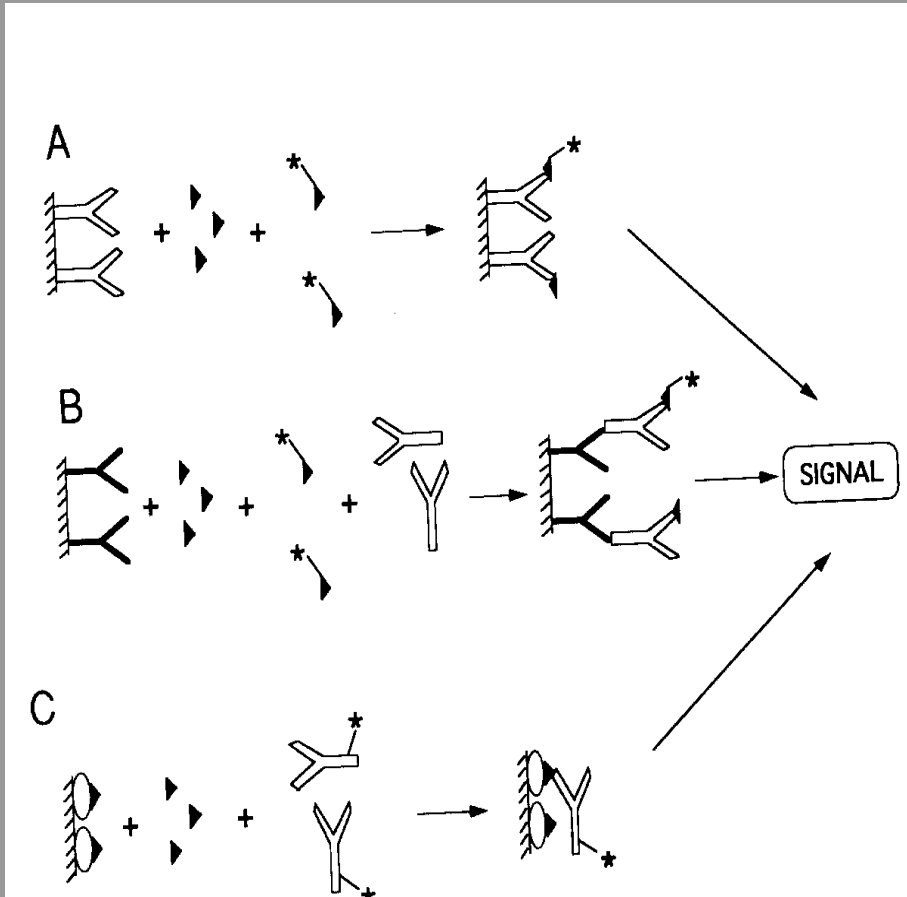
FIGURE 17.4 Competitive immunoassay: (a) competitive binding of analyte and labeled analyte to a limited number of antibody binding sites, (b) immobilized antigen competes with free antigens in solution for binding sites of the labeled antibody, (c) calibration curve obtained with either approach of the competitive assay type.

TABLE 17.1**Overview of Immunoassay Techniques**

Assay method	Label	Detected	Detector	
RIA (radioimmunoassay)	^{125}I , ^3H , ^{14}C	Radiation	Scintillation counter	Sensitive unsafe, high cost
EIA (enzyme immunoassay)	HRP AP β -D-galactosidase HRP, AP, galactosidase	Color change (absorbance)	Photometer	
FrIA (fluoroimmunoassay)	HRP HRP, AP, GOD, catalase Fluorescein rhodamines, dansyl chloride, coumarins, phycoerythrin, also liposomes	Fluorescence Luminescence Current Fluorescence	Fluorimeter Luminometer Amperometric electrode Fluorimeter	Sensitive Low to medium cost
TR-FrIA (time-resolved FIA)	Lanthanoid cations: Eu^{3+} , Tb^{3+} , Sm^{3+}	Delayed fluorescence	Time-resolved fluorimeter	
LIA (luminescence immunoassay)	Acridinium esters Dioxetanes Peroxyoxalates Luminol Luciferase/luciferin Peroxidase Pyrene	Chemi- and bioluminescence	Luminometer	Very sensitive high cost
Electrochemical immunoassays	Metalloenes Metals GOD, catalase Urease Liposomes	Electroluminescence Current Ions (potential change)	Electrode luminometer DPP (differential pulse polarograph) DPASV (differential pulse anodic stripping voltammetry) Potentiometric electrode	

Note: AP: alkaline phosphatase, GOD: glucose oxidase, HRP: horseradish peroxidase.

schemi di immunodosaggi



$$y = \frac{a-d}{(1+(x/c)^b)} + d$$

a = (theoretical) response at low concentration/dilution
b = absolute value of the slope at the inflection point
c = value of x at inflection point
d = (theoretical) response at high concentration/dilution
x = concentration or dilution
y = response (OD)

Typical calibration curve for immunoassay

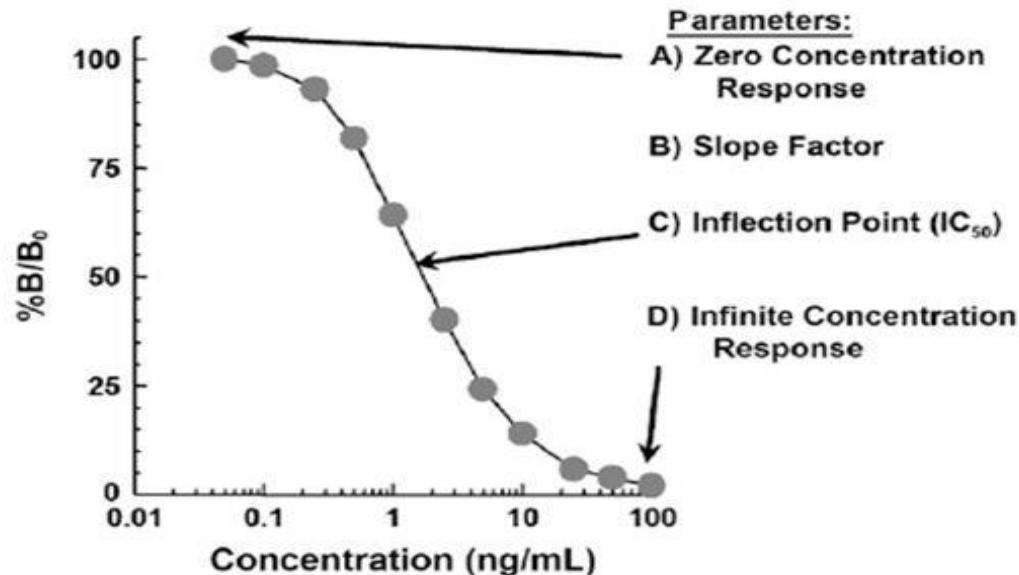


Figure 1. Typical 4-parameter logistic graph for a competitive-format immunoassay.

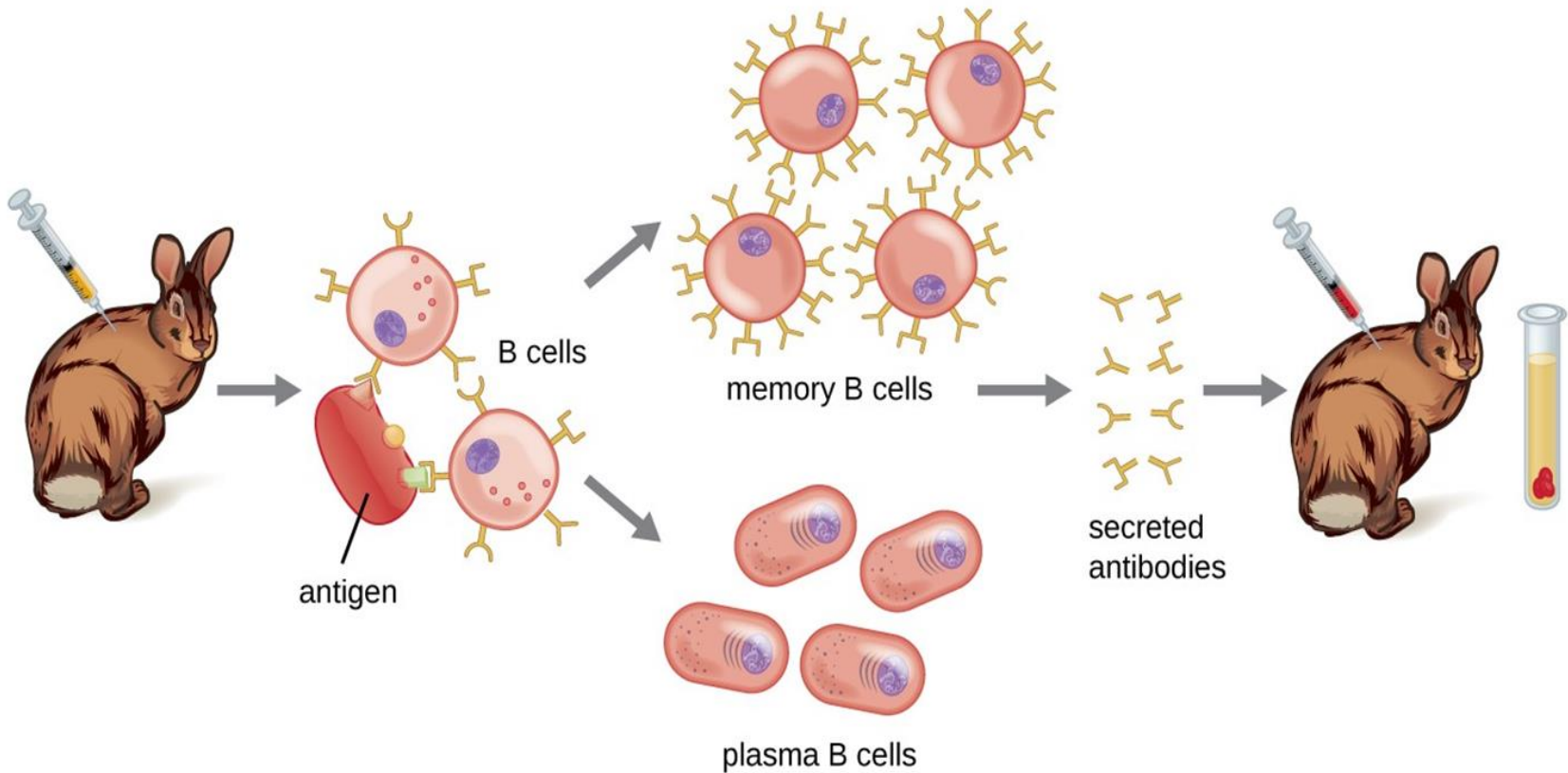
Polyclonal antibodies production

1 Inject antigen into rabbit.

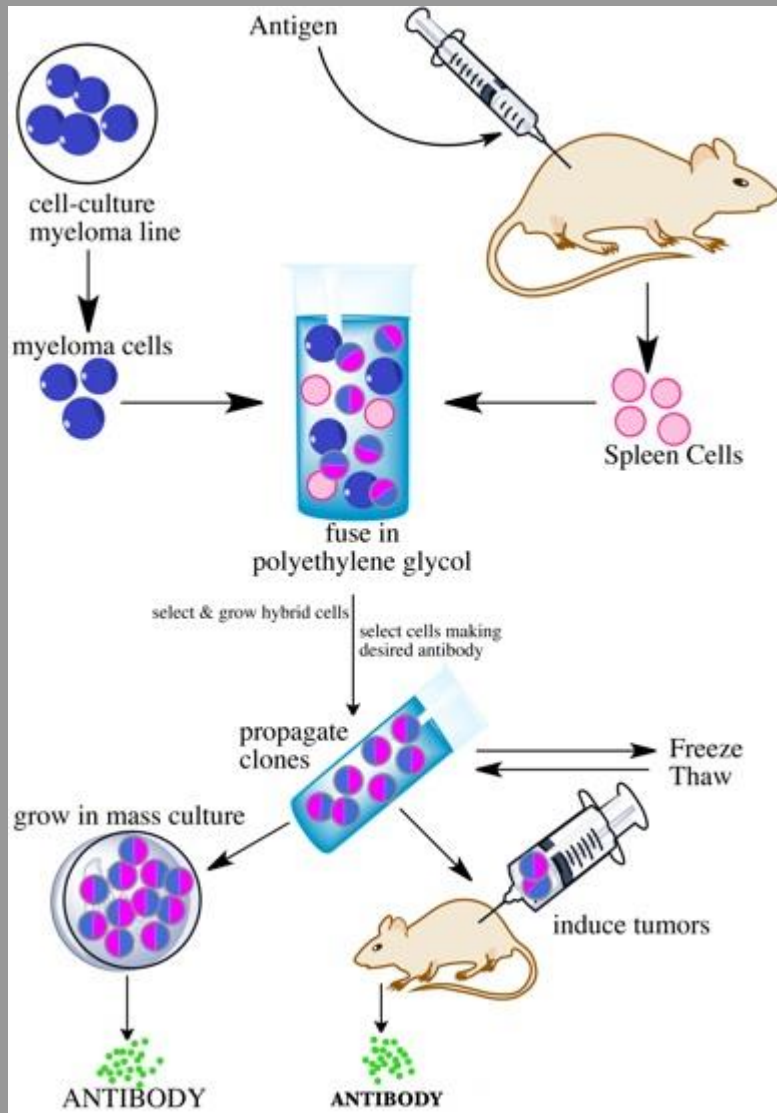
2 Antigen activates B cells.

3 Plasma B cells produce polyclonal antibodies.

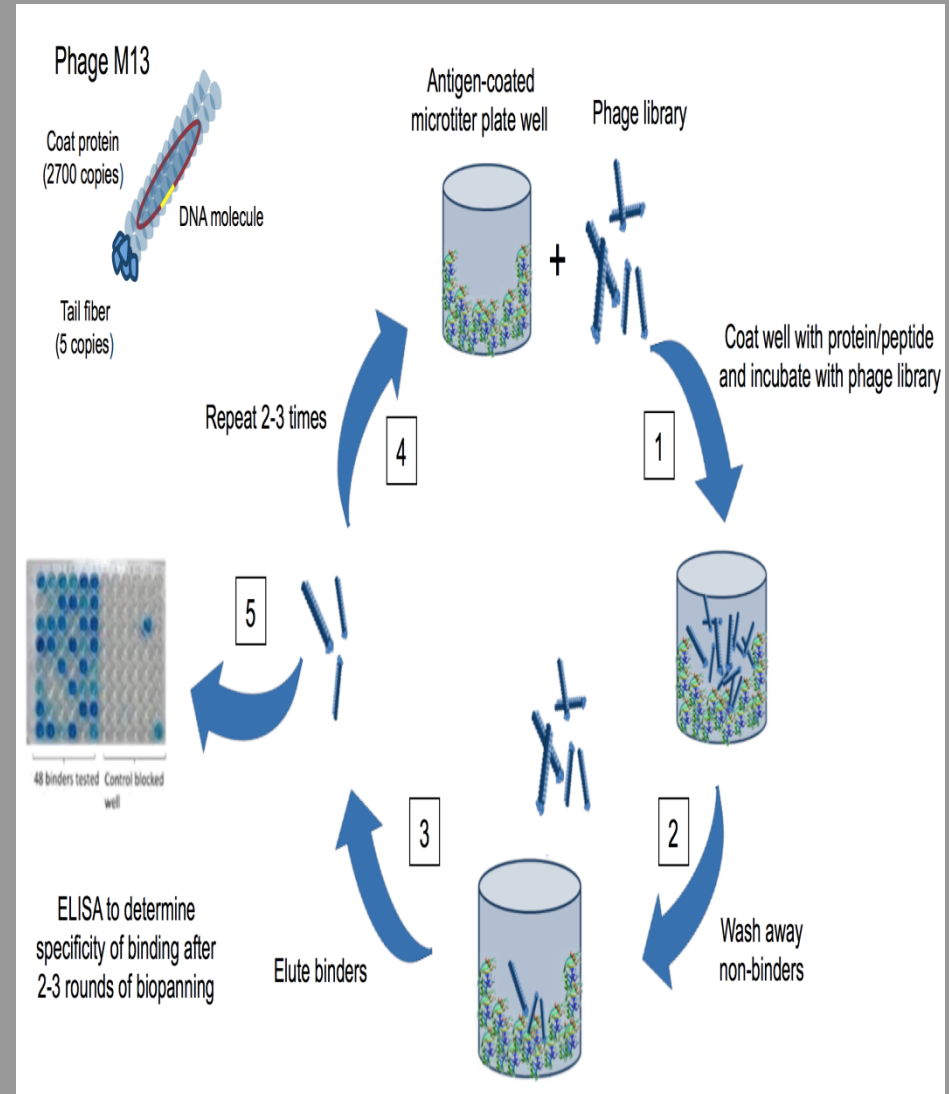
4 Obtain antiserum from rabbit containing polyclonal antibodies.



Monoclonal antibodies

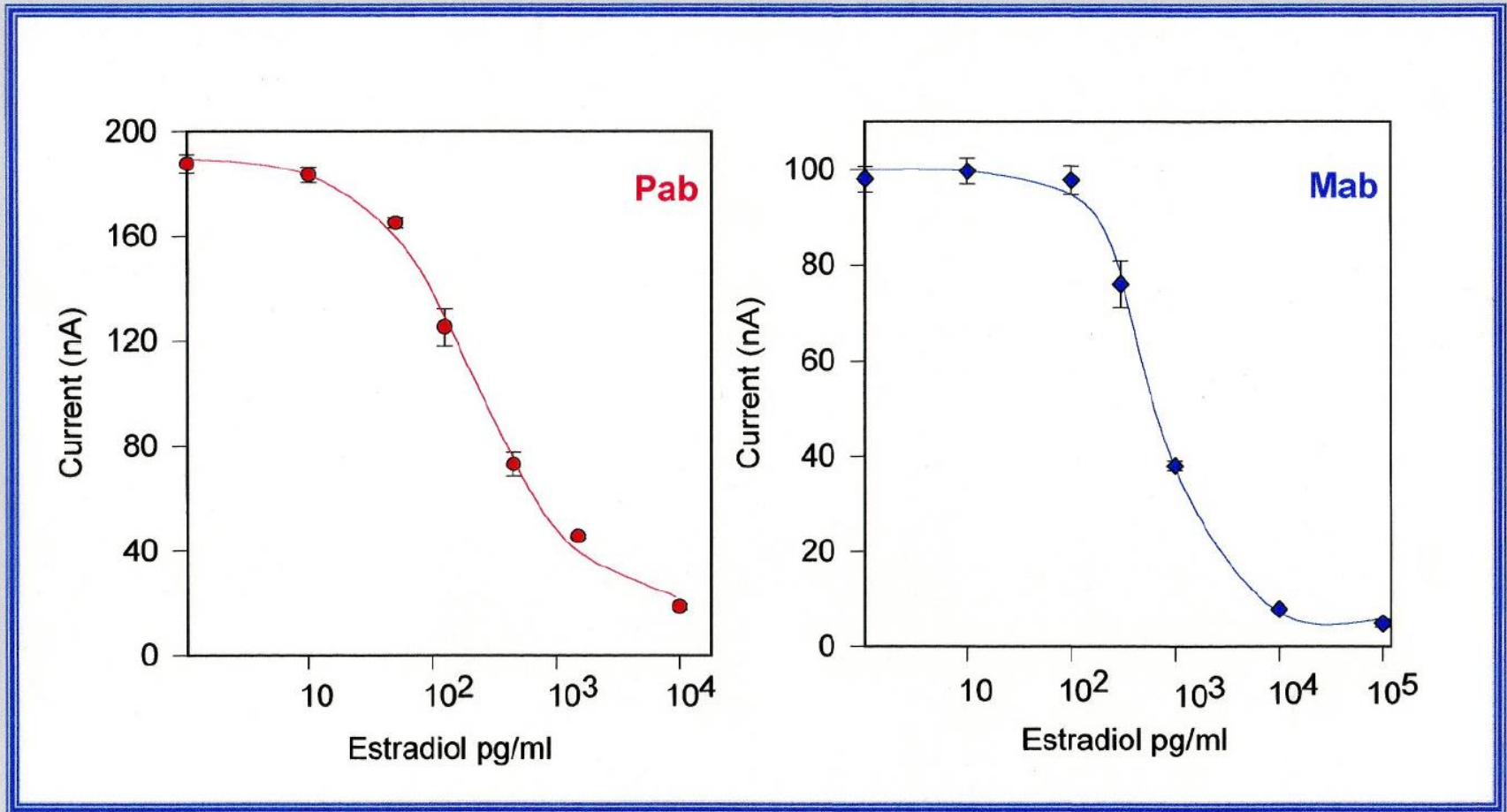


Recombinant antibodies



Enzyme Linked Immuno-Sorbent Assay

ELISA elettrochimico



Pab have wider analytical range sensitivity depends on K_{aff}

ELISA



- **Enzyme-linked immunosorbent assay (ELISA)** is a test that uses antibodies and color change to identify a substance.



ELISA STEPS

COATING

Polystyrene plate is treated with a solution of either antigen or antibody.



*remove liquid
and wash plate*

BLOCKING

An unrelated protein-based solution is used to cover all unbound sites on the plates



*remove liquid
and wash plate*

DETECTION

Enzyme-conjugated antibody or antigen binds specifically to the target antigen or antibody



*remove liquid
and wash plate*

READ RESULTS

Substrate is added and the signal produced by the enzyme-substrate reaction is measured

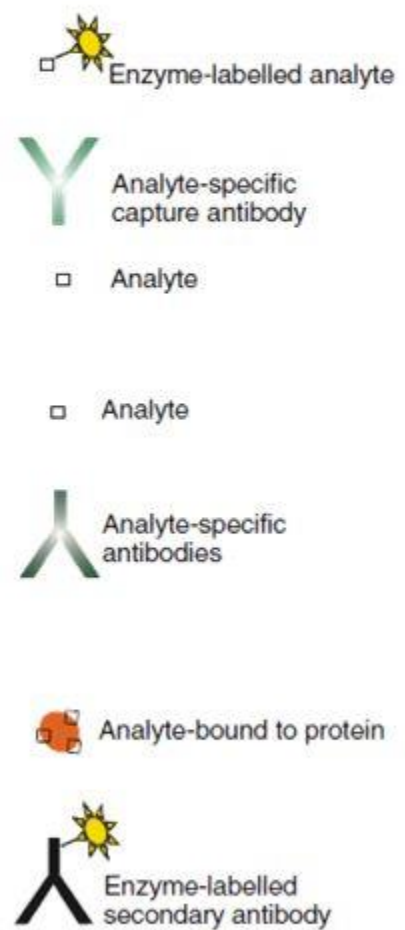
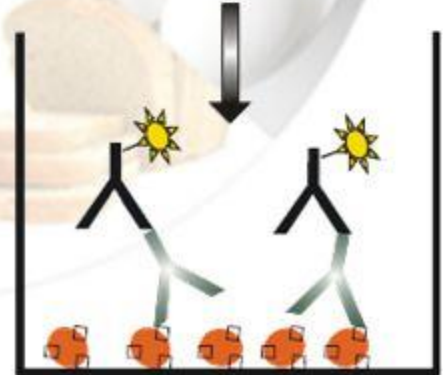
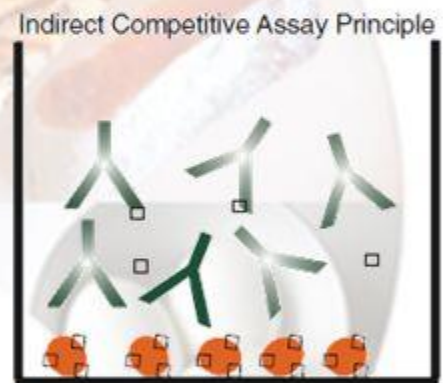
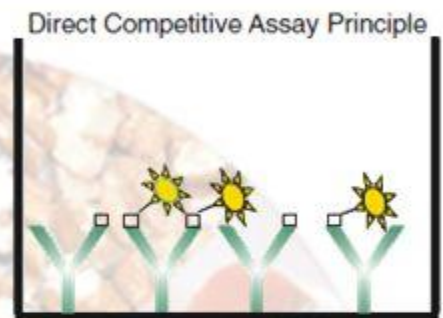
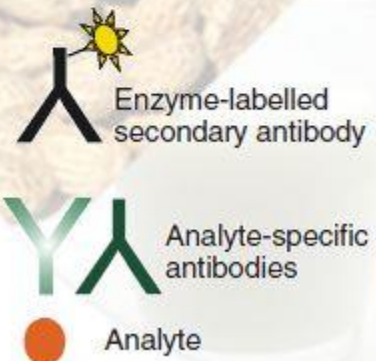
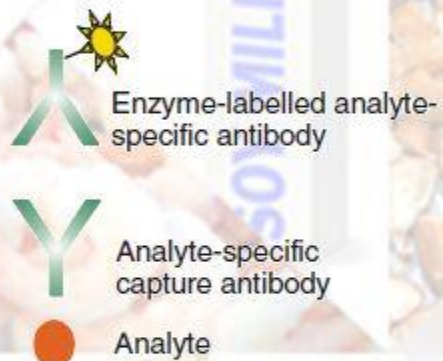
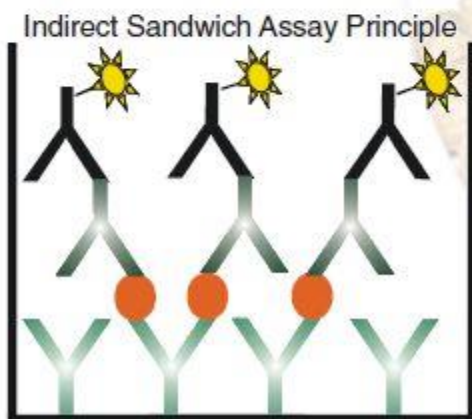
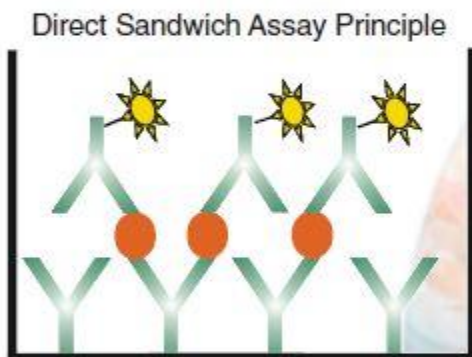






How to detect food allergens?

ELISA



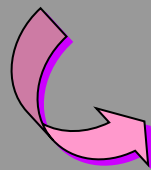


À la carte ELISA Systems

				
Almond	Beta-Lactoglobulin	Buckwheat	Casein	Crustacean
				
Egg	Gluten	Hazelnut	Lupin	Mustard
				
Peanut	Sesame	Soy		

❖ Rivelazione elettrochimica per immunosensori:

Cronoamperometria



Voltammetria
Differenziale a impulsi
(DPV)

❖ Enzimi e relativi substrati:

Fosfatasi alcalina

Perossidasi da rafano



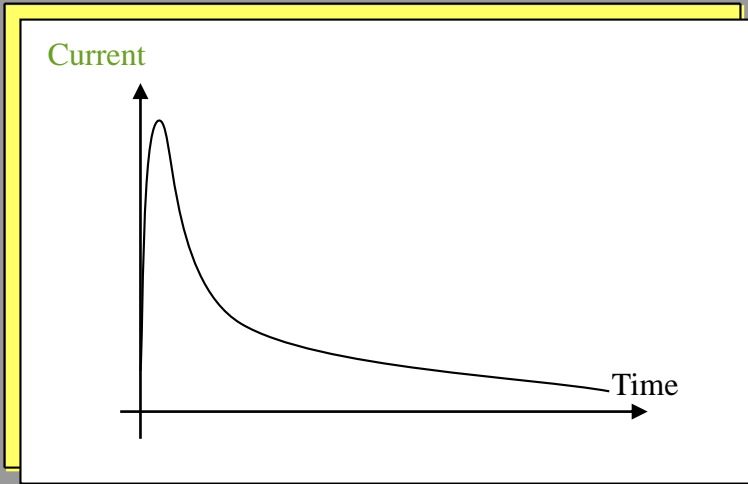
1-naftil fosfato



• TetrametilBenzidina + H_2O_2
• $[K_4Fe(CN)_6] + H_2O_2$

electrochemical detection:

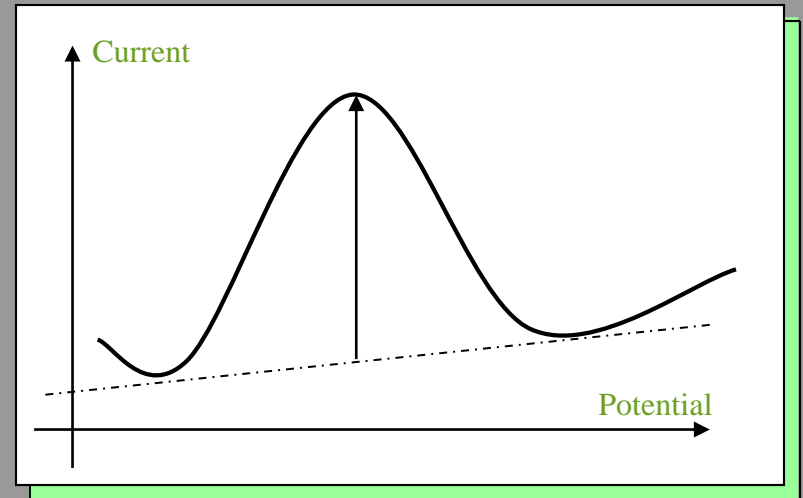
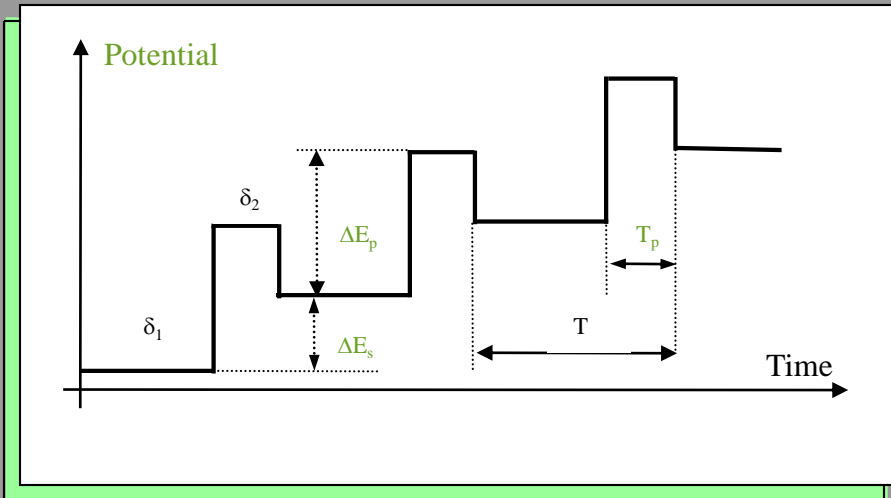
chronoamperometry and differential pulse voltammetry (DPV) :

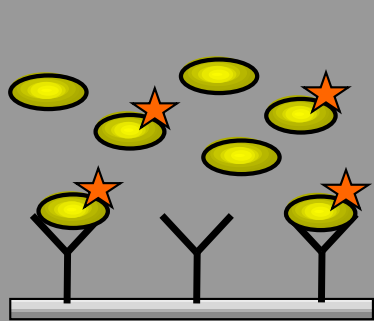


$$\Delta E = \text{const.}$$

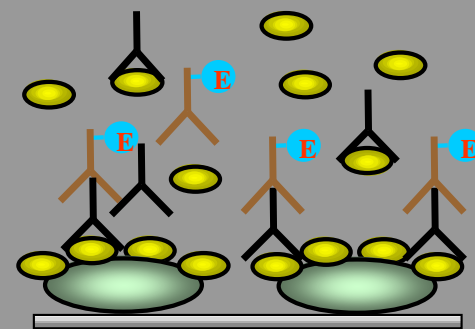
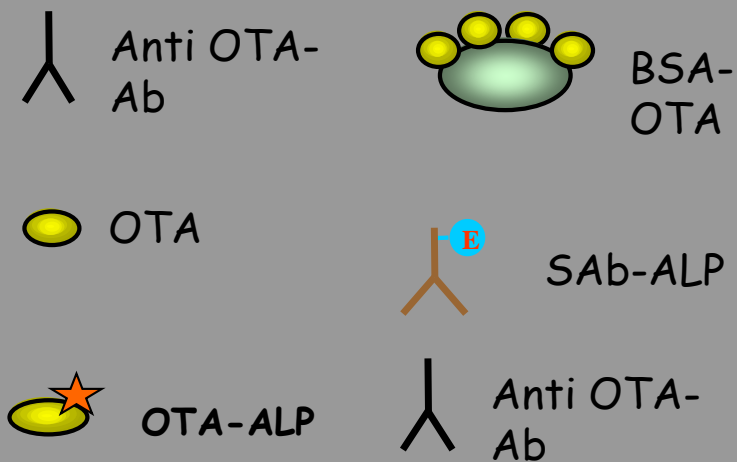
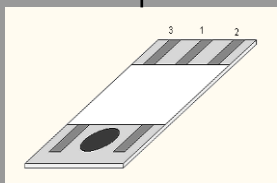
$$\delta_2 = 60 \text{ ms}$$

$$\Delta E_p = 5-100 \text{ mV}$$

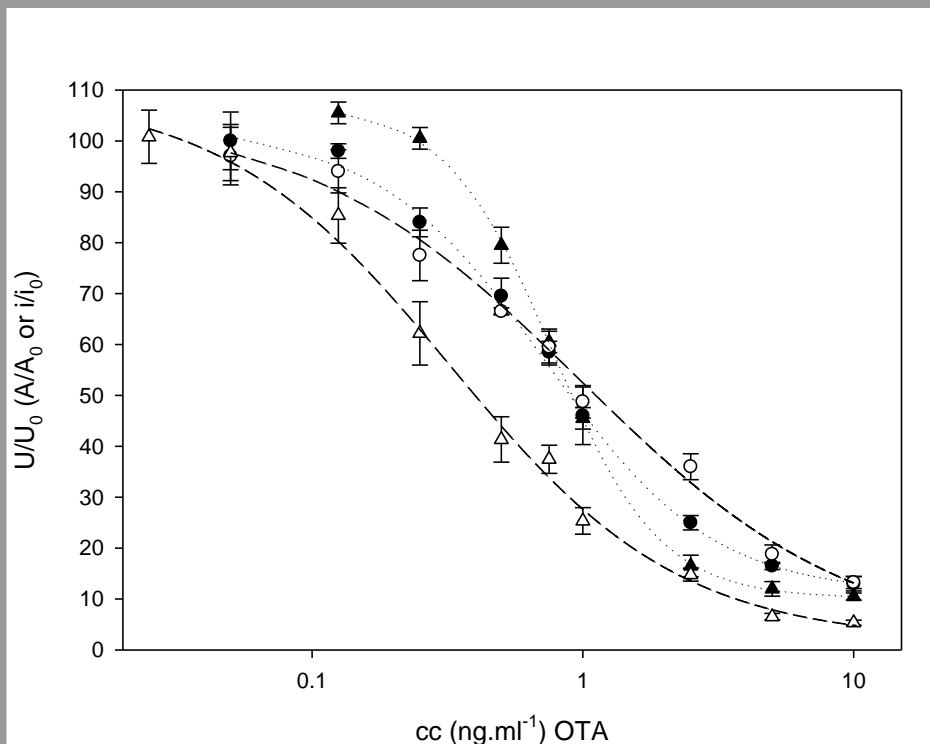
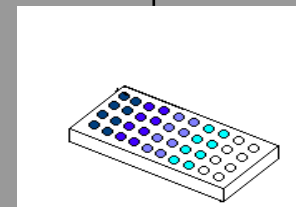




saggio diretto



saggio indiretto



OTA = ocratossina A

$$f(x) = \{(a - d)/[1 + (x/c)b]\} + d$$

	Competition curve parameters				Linear regression
	<i>a</i> (A or nA)	<i>b</i> (nA.ng.ml ⁻¹)	<i>c</i> (ng.ml ⁻¹)	<i>d</i> (A or nA)	
ic spettr	1.220 ± 0.053	1.40 ± 0.50	0.80 ± 0.22	0.129 ± 0.077	$f(x) = 49.3 (\pm 0.8) - 57.5 (\pm 0.1) x$ [$r = 0.991$]
ic amp.	6019 ± 118	0.90 ± 0.22	0.93 ± 0.10	176 ± 30	$f(x) = 52.5 (\pm 0.4) - 43.7 (\pm 0.5) x$ [$r = 0.994$]
dc spettr	1.392 ± 0.061	2.17 ± 0.15	0.80 ± 0.14	0.132 ± 0.071	$f(x) = 47.4 (\pm 0.7) - 86.0 (\pm 0.3) x$ [$r = 0.993$]
dc amp.	707 ± 56	1.10 ± 0.10	0.35 ± 0.04	16 ± 13	$f(x) = 34.9 (\pm 0.6) - 52.2 (\pm 0.9) x$ [$r = 0.992$]

Immunoassay	Working Range (ng/ml)	L.O.D. (Blank - 3 σ) (ng/ml)
ic spettr	0.20 – 2.5	0.150
ic amp.	0.10 – 7.5	0.120
dc spettr	0.10 – 10	0.080
dc amp.	0.05 – 2.5	0.060

Procedura immunosensore:

✓Pre-coating: 6 μ l di soluzione di anti IgG di coniglio (4° C overnight)

✓Bloccaggio: 6 μ l di soluzione 1 % di alcool polivinilico (30 min)

✓Coating: 6 μ l di anti-OTA (1 h)

✓Competizione: 6 μ l di OTA-AP + standard/campione (30 min)

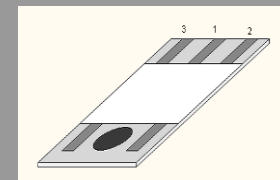
✓Rivelazione: 100 μ l di 5 mg/ml 1-Naftilfosfato (2 min) + DPV

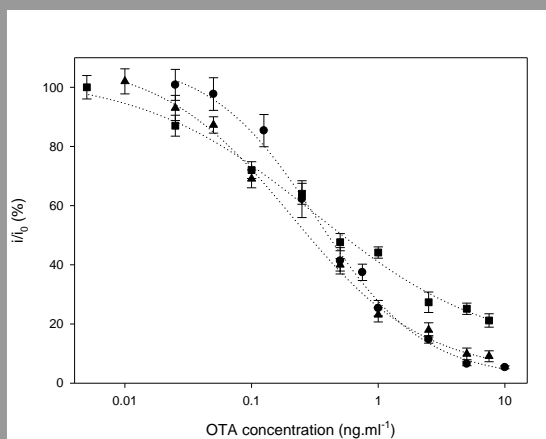
Lavaggi: 150 μ l tampone fosfato pH 7.4

Effetto del solvente di estrazione

Attività di un elettrodo modificato con IgG-ALP dopo incubazione per 30 min con soluzioni 1:9 - 9:1 (1:1 in DPBS) acetone:acqua \rightarrow 95-108%

Sensibilità della curva di calibrazione ~ 50%





25 g in 100 mL di
ACN:H₂O

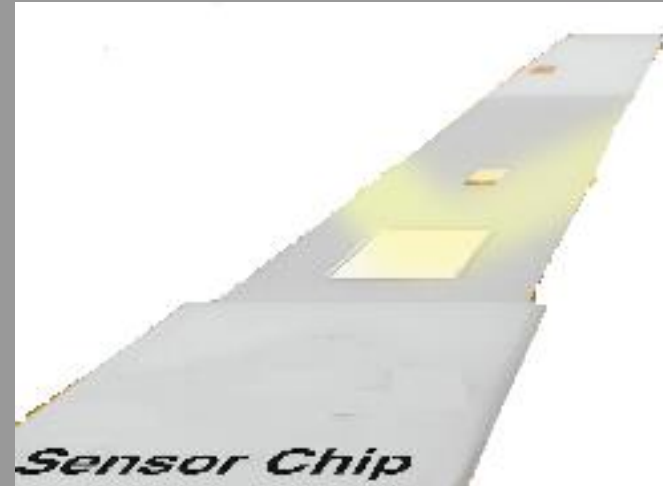
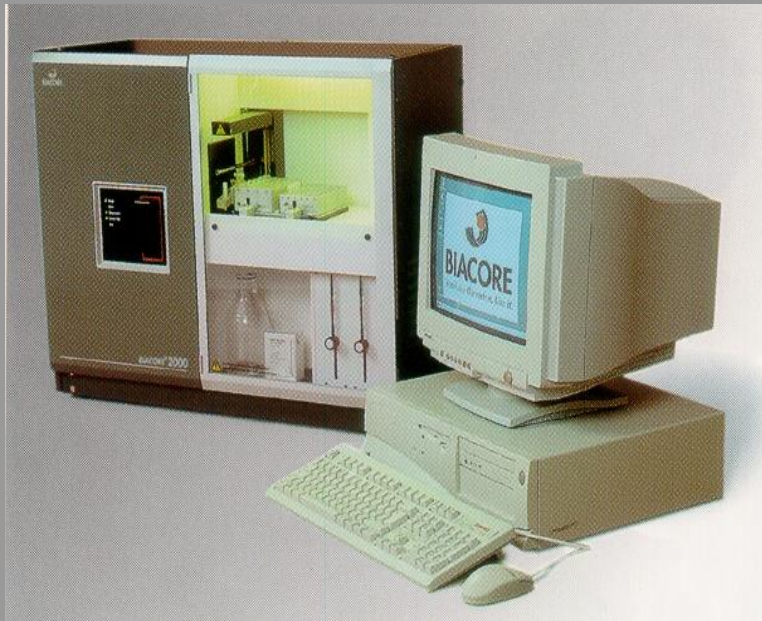
Final dilution 1:8

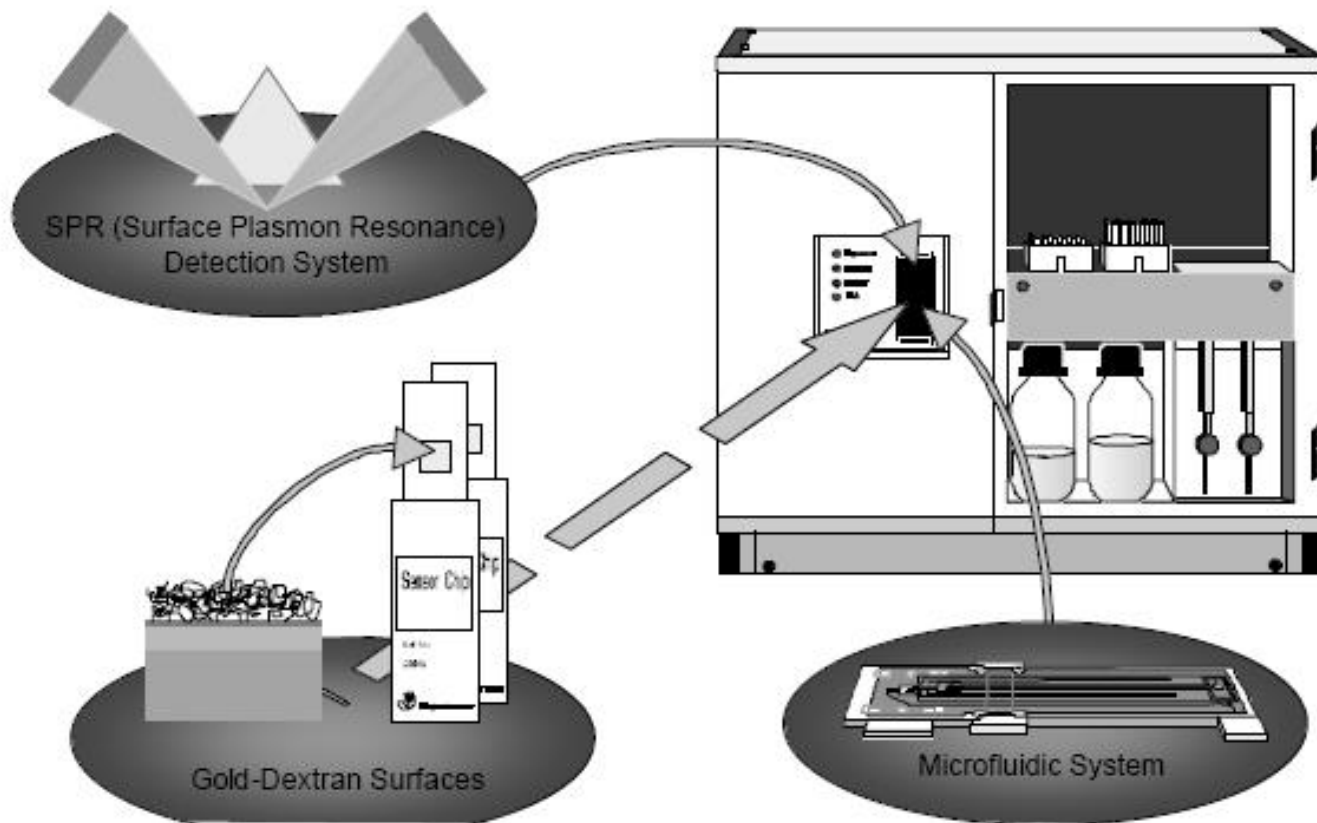
MRL = 3 ng/g

I₅₀ = 1.6 ng/g

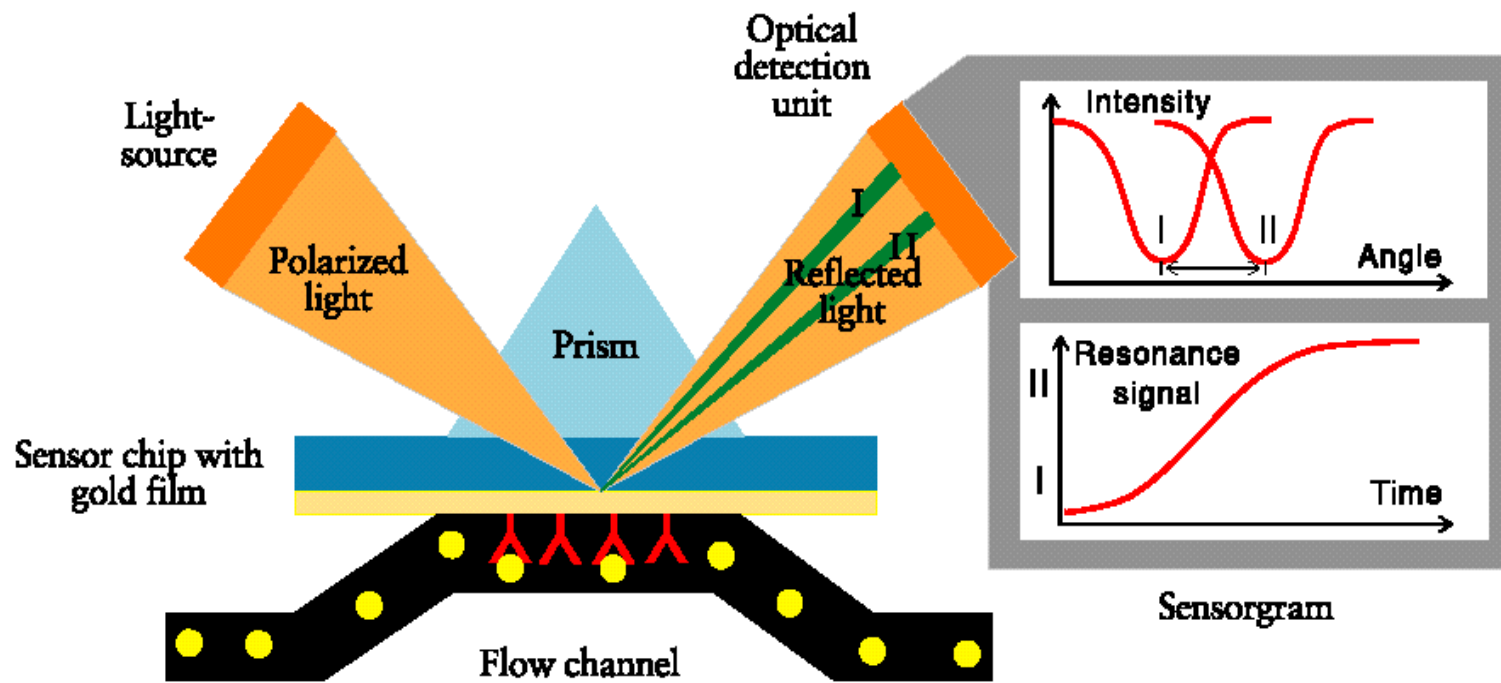
Parameters		0.1 PBS Buffer ●	ACN:H ₂ O (6:4) ▲	Wheat Extract (blank) ■
<i>a</i>	(nA)	707 (± 56)	260 (± 12)	408 (± 72)
<i>b</i>	(nA.ng.ml ⁻¹)	1.1 (± 0.1)	0.62 (± 0.03)	0.8 (± 0.1)
<i>c</i> (I ₅₀)	(ng.ml ⁻¹)	0.35 (± 0.04)	0.32 (± 0.02)	0.20 (± 0.03)
<i>d</i>	(nA)	16 (± 13)	24 (± 8)	13 (± 15)
w.r.	(ng.ml ⁻¹)	0.05 – 2.5	0.02 – 5.0	0.05 – 2.5
L.O.D.	(ng.ml ⁻¹)	0.06	0.015	0.05
Lin.	Reg.	30.9 (± 0.6) – 52.2 (± 0.9) x	42.3 (± 0.3) – 25.4 (± 0.6) x	23.5 (± 0.1) – 41.1 (± 0.5) x

Biacore

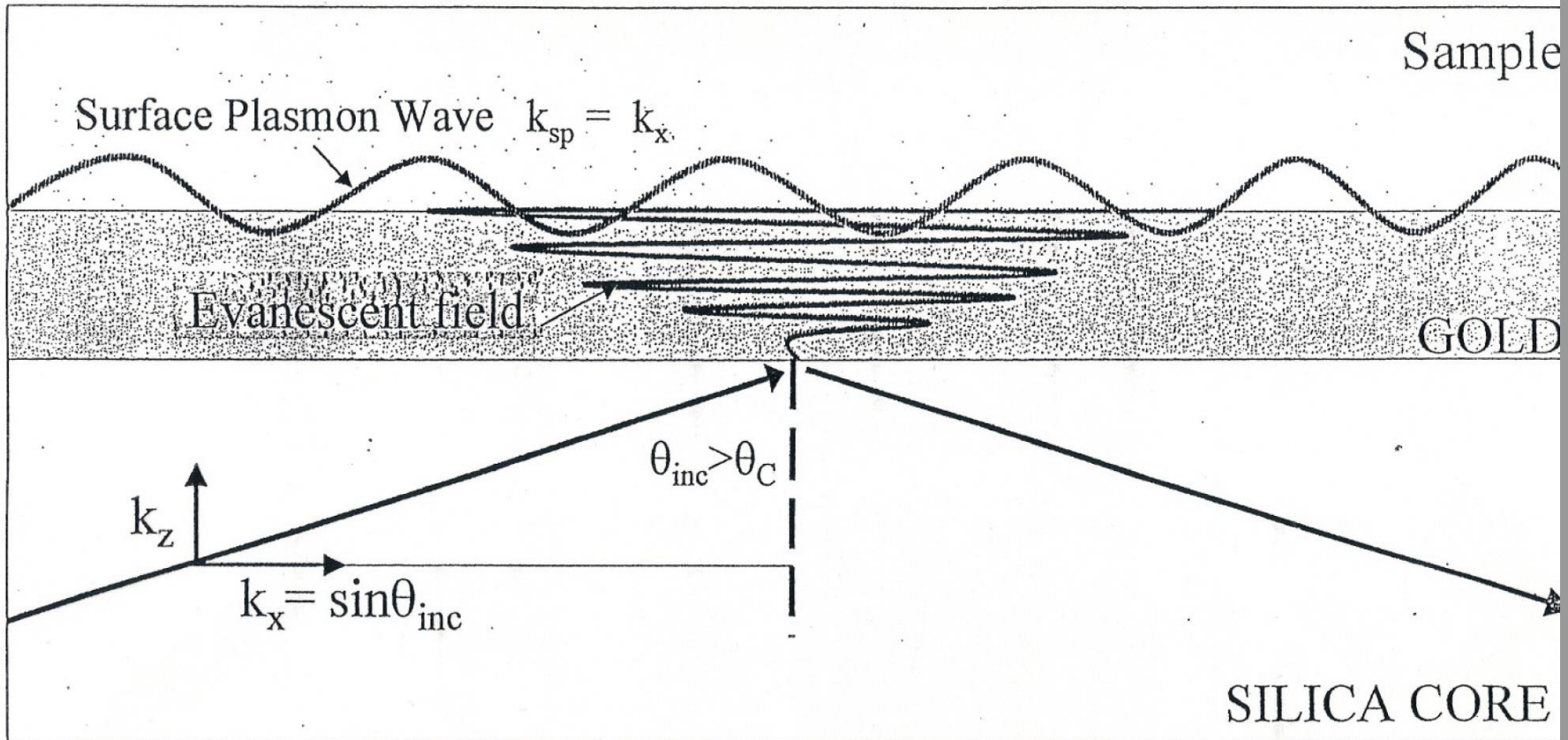




SPR Biosensors



Surface Plasmon Resonance



θ_{inc} - angle of incident light

λ_{inc} - wavelength of incident light

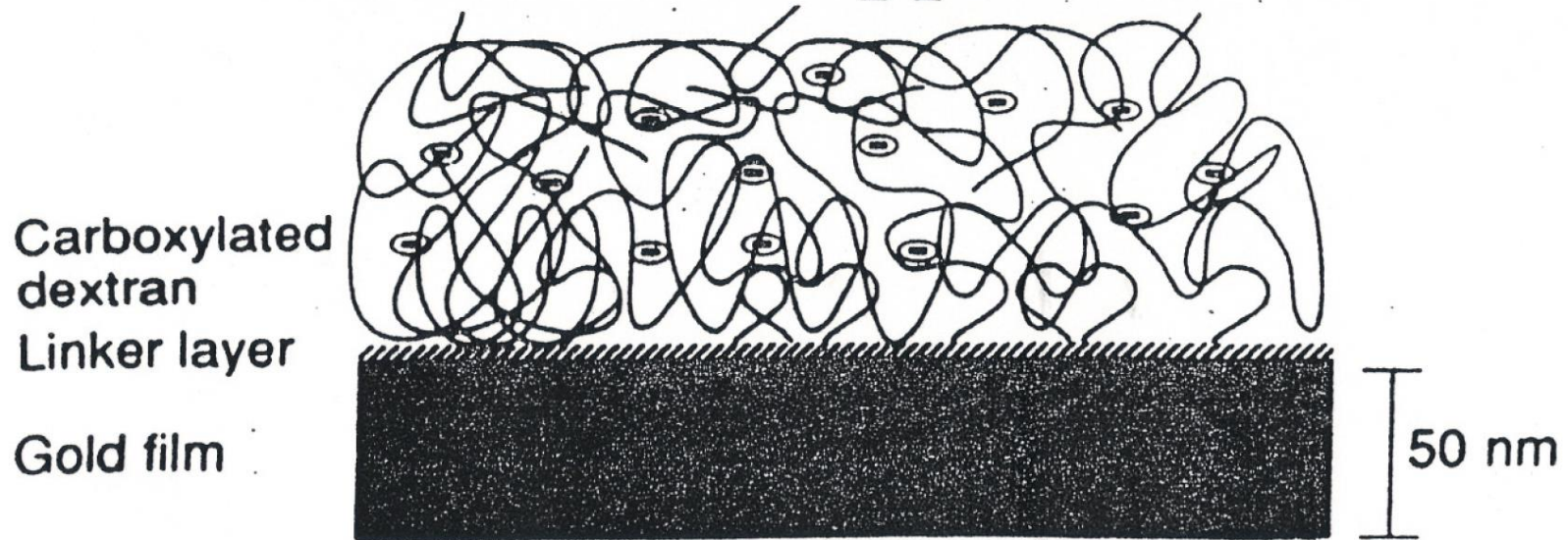
n_{glass} - Refractive Index of glass

n_{metal} - Refractive Index of metal

n_{sample} - Refractive index of sample

t_{metal} - Thickness of metal

BIACORE approach



dextran hydrogel

open structure (good accessibility)

no denaturation

- enhancement of the capacity of the interaction layer
- stagnant layer / mass transport flow needed ($\mu\text{l}/\text{min}$)
- negative charge
- regenerable (up to 100 x)

Principio della SPR

Surface plasmon resonance (SPR) arises when light is reflected under certain conditions from a conducting film at the interface between two media of different refractive index. The media are the sample and the glass of the sensor chip, and the conducting film is a thin layer of gold on the chip surface. SPR causes a reduction in the intensity of reflected light at a specific angle of reflection. This angle varies with the refractive index close to the surface on the side opposite from the reflected light.

When molecules in the sample bind to the sensor surface, the concentration and therefore the refractive index at the surface changes and an SPR response is detected. Plotting the response against time during the course of an interaction provides a quantitative measure of the progress of the interaction. This plot is called a sensorgram.

What Biacore actually measures is the angle of minimum reflected light intensity. The light is not absorbed by the sample: instead the light energy is dissipated through SPR in the gold film. Thus the light used to detect interaction processes never enters the sample.

SPR response values are expressed in resonance units (RU). One RU represents a change of 0.0001° in the angle of the intensity minimum. For most proteins, this is roughly equivalent to a change in concentration of about 1 pg/mm² on the sensor surface. The exact conversion factor between RU and surface concentration depends on properties of the sensor surface and the nature of the molecule responsible for the concentration change.

Immobilizzazione di biomolecole su oro

Adsorbimento



**Forze elettrostatiche;
Attraverso i disolfuri delle proteine**

Vantaggi:

semplicità, economicità, facilità di realizzazione;

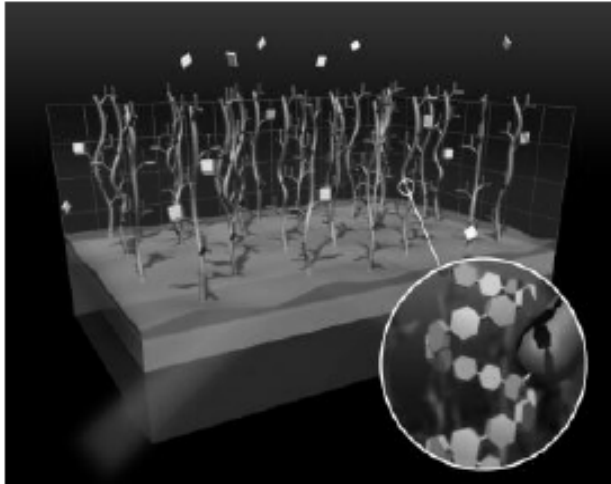
Svantaggi:

Perdita del recettore dal supporto;

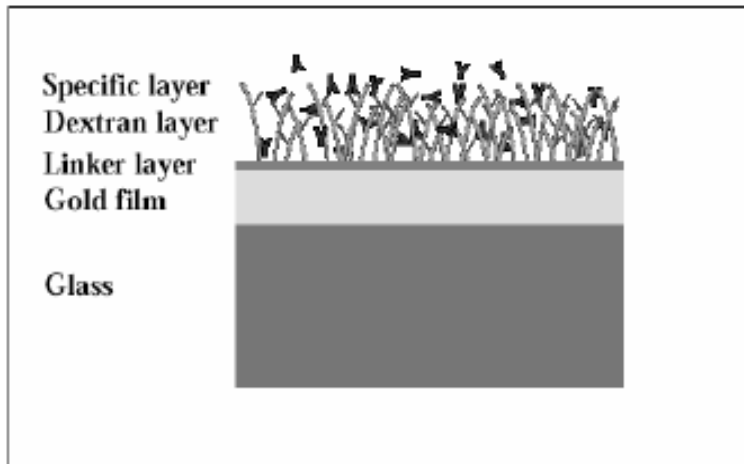
Legame non-specifico;

Immobilizzazione non orientata (random orientation).

Destrano

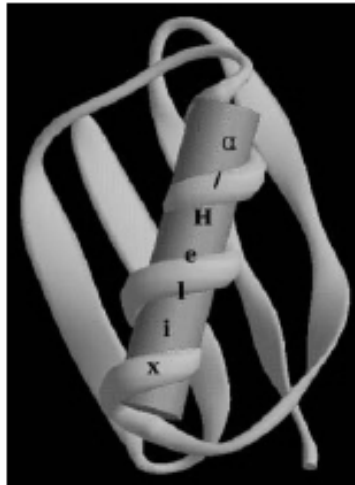


Carboidrato polimerico naturale



Stabilità
Basso legame aspecifico
Matrice tridimensionale

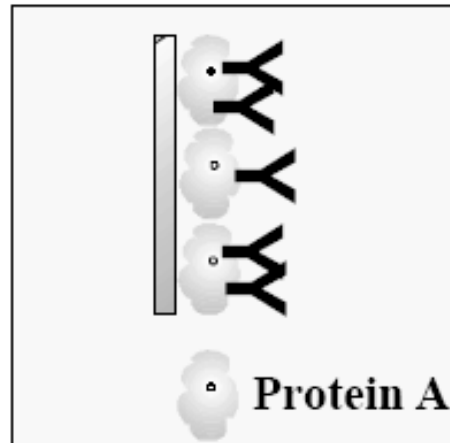
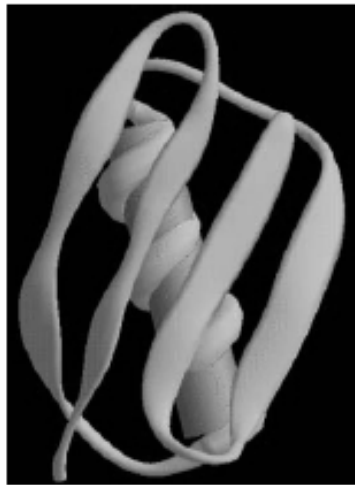
IgG binding proteins



PROTEINA A e PROTEINA G

Proteine batteriche

Contengono siti ad alta affinità di legame per la regione Fc degli anticorpi di varie specie



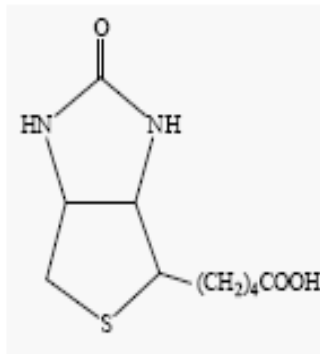
**Principali svantaggi:
breve vita del sensore;**

Avidina-Biotina



Alta costante d'affinità: $10^{-15} \text{ mol}^{-1}$

Legame molto stabile (pH, lavaggi)



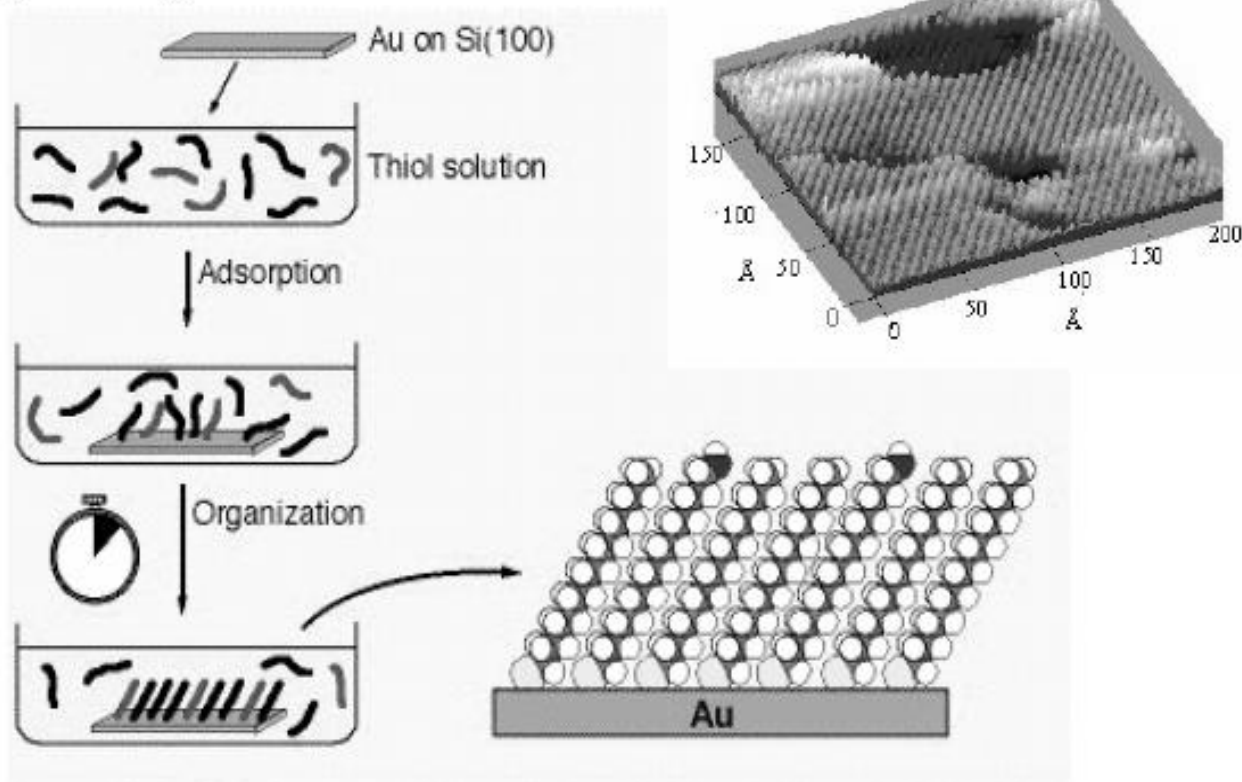
La biotinilazione non inficia l'attività biologica della biomolecola (recettore)

Self Assembled Monolayers (SAM)

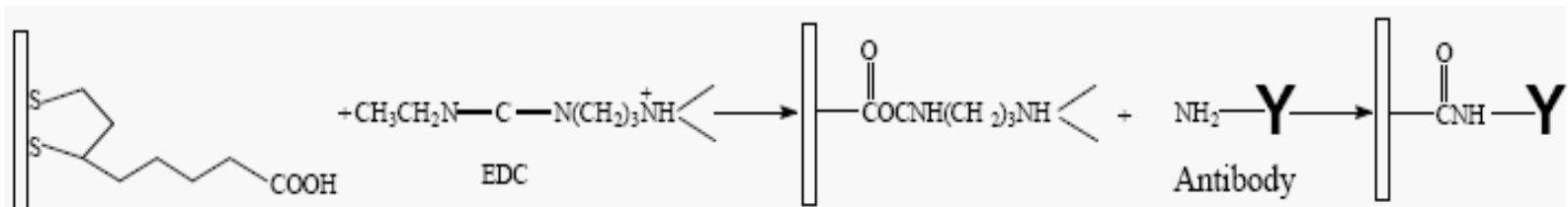
Disulphides (R-S-S-R)

Sulphides (R-S-R)

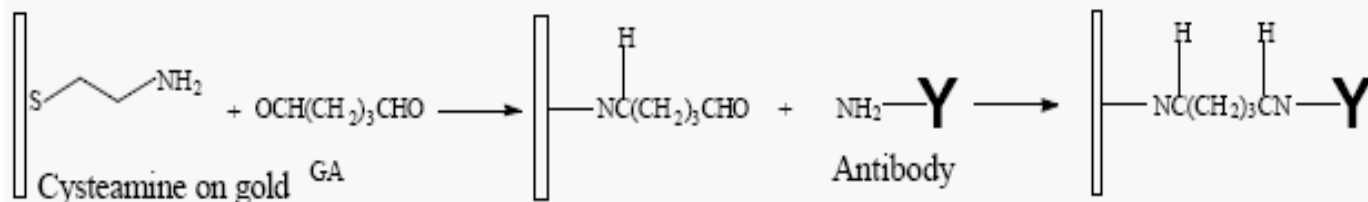
Thiols (R-SH)



SAM



Thioctic acid on gold



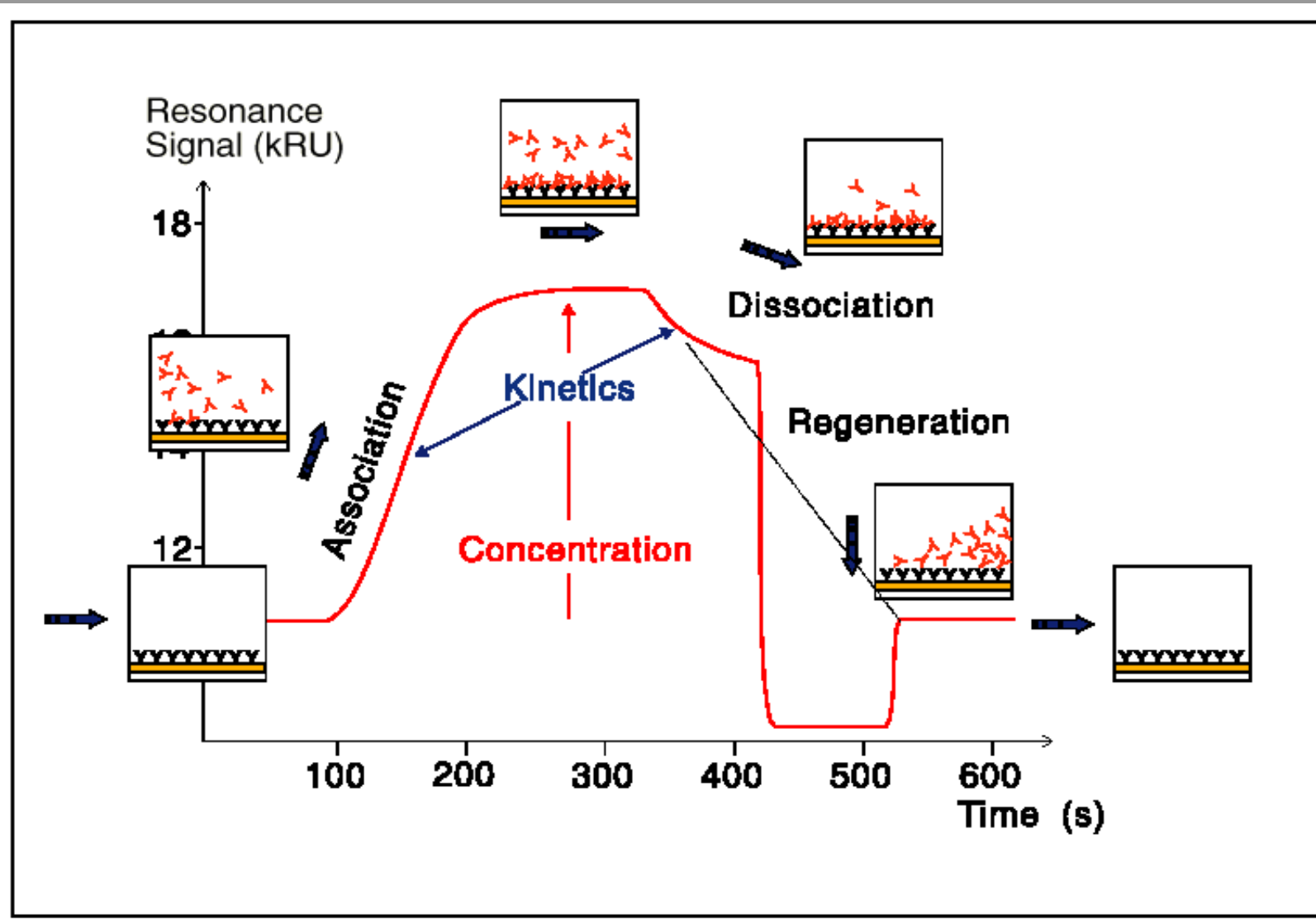
Cysteamine on gold GA

Stabilità

Alta densità di superficie

Rigenerazione

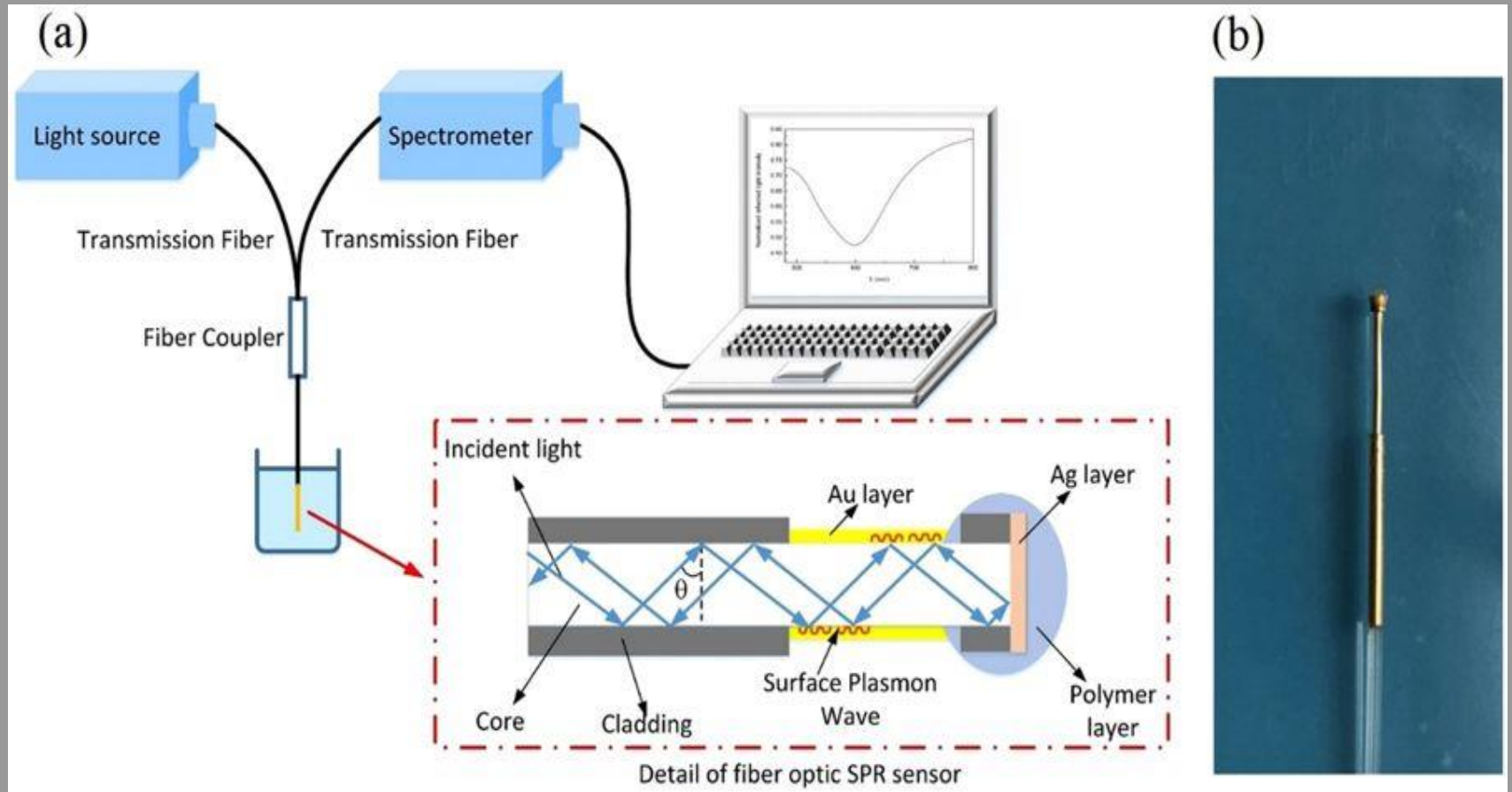
Sensorgram



A label-free fiber optic SPR biosensor for specific detection of C-reactive protein

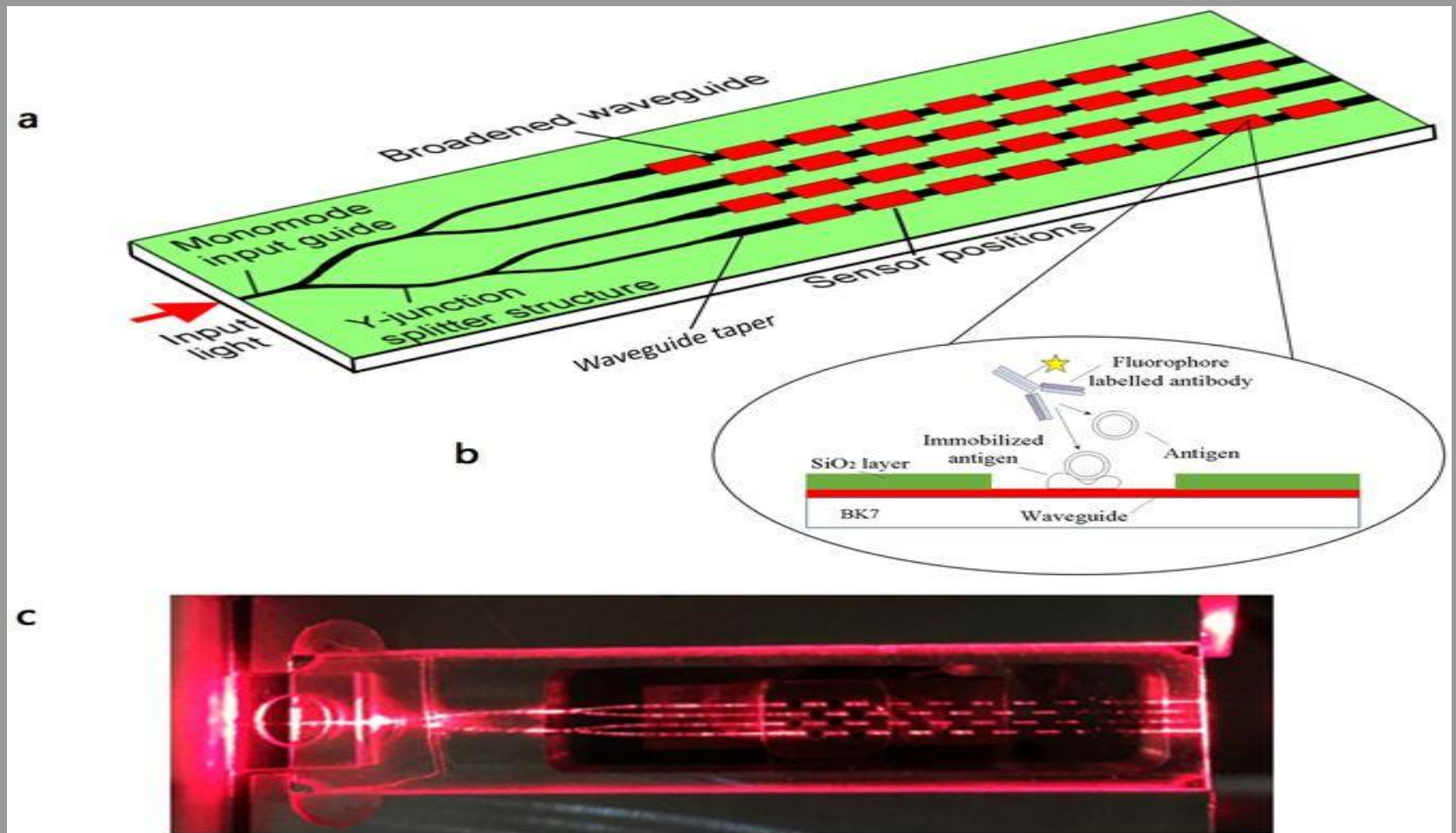
Wenjia Wang, Zhigang Mai, Yuzhi Chen, Jiaqi Wang, Liang Li, Qingning Su, Xuejin Li
Xueming Hong

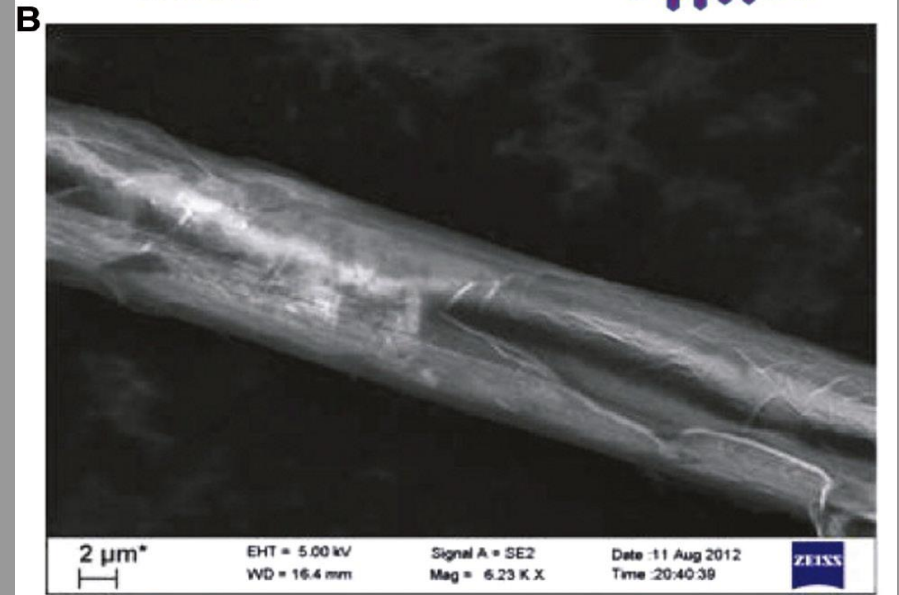
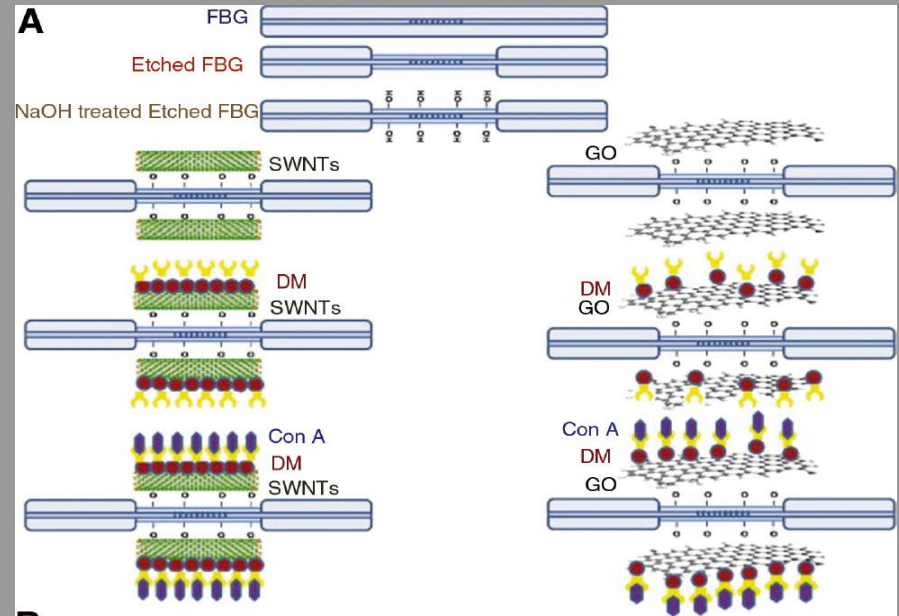
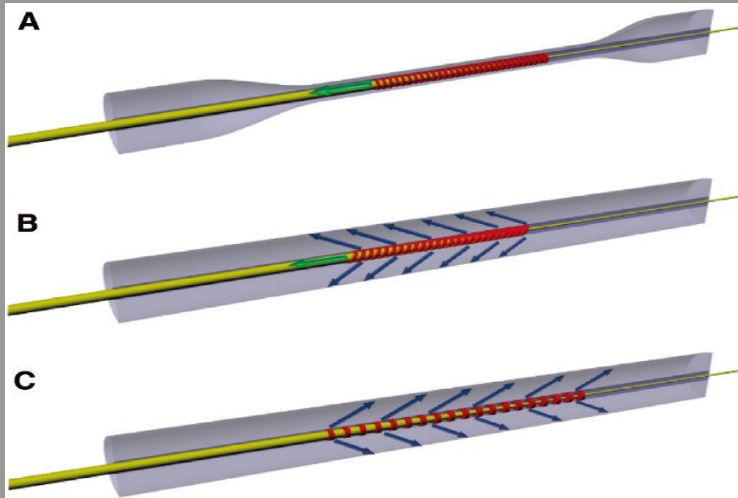
Scientific Reports **volume 7**, Article number: 16904 (2017)



Integrated optical waveguide-based fluorescent immunosensor for fast and sensitive detection of microcystin-LR in lakes: Optimization and Analysis [Lanhua Liu](#), [Xiaohong Zhou](#), [James S. Wilkinson](#), [Ping Hua](#), [Baodong Song](#), [Hanchang Shi](#)

Scientific Reports **volume 7**, Article number: 3655 (2017)





Biosensing with optical fiber gratings

Francesco Chiavaioli, Francesco Baldini, Sara Tombelli, Cosimo Trono, Ambra Giannetti

Published Online: 2017-06-07 | DOI: <https://doi.org/10.1515/nanoph-2016-0178>

DOI: 10.1002/elan.201500237

Lateral Flow Immunoassays – from Paper Strip to Smartphone Technology

Evgeni Eltzov,^[a, b, c] Sarah Guttel,^[d] Adarina Low Yuen Kei,^[b, c] Prima Dewi Sinawang,^[b, c] Rodica E. Ionescu,^[b, e] and Robert S. Marks*^[a, b, c, f, g]

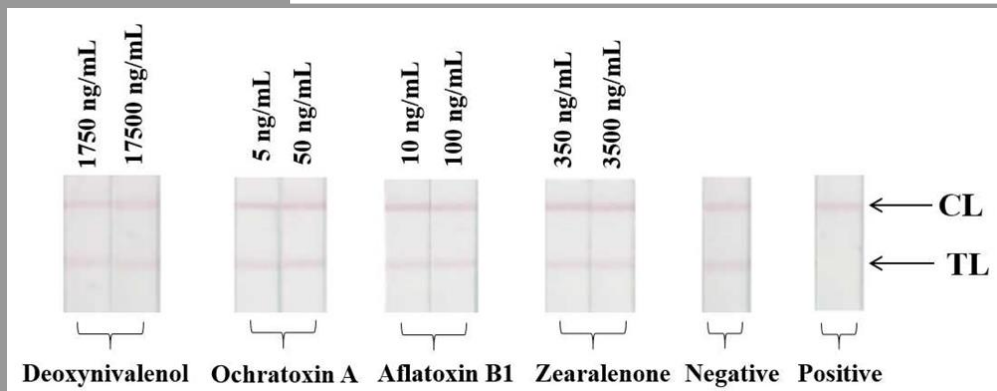
Lateral flow biosensors

Advantages

- Simple operation without pretreatment
- Low cost
- Stable
- Portable
- Fast
- Wide range of the formats
- Simple in construction, that will allow adaption to the target analyte

Disadvantages

- Only qualitative and not quantitative
- Very limited quantitative dynamic range
- Low multiplexity
- Lack of automation
- Possible error for color blind people



Lateral flow immunoassays

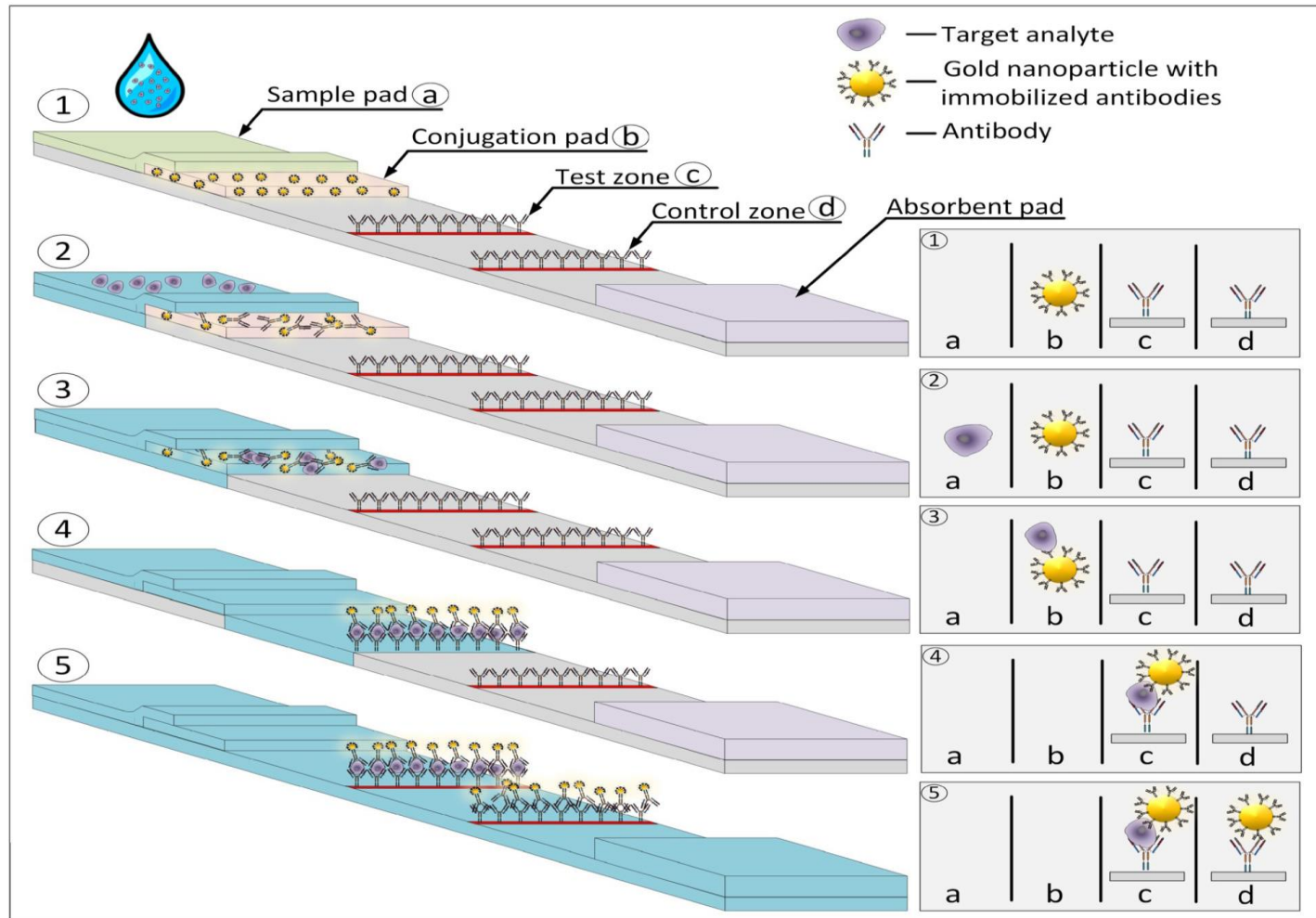


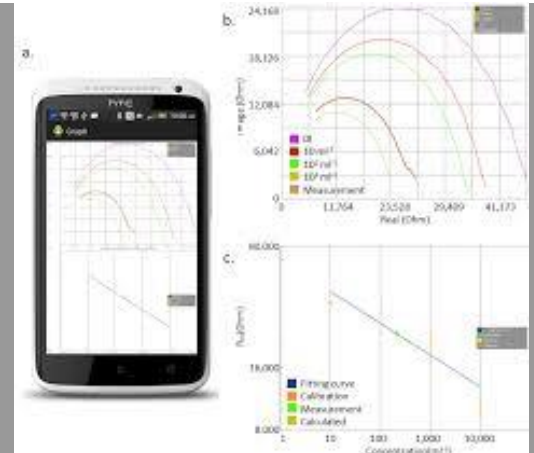
Fig. 1. Schematic presentation of lateral flow assay and measurement process. 1 and 2. Water sample placed above sampling pad. 3. Target analyte migrates through sample pad to conjugation. 3. It will bind to conjugated labeled antibodies. All these clusters are moved to the test zone (4) and control zone (5).

Labels used in lateral flow assays

Label type	Advantages	Disadvantages
Latex	<ul style="list-style-type: none"> • Low price • Appropriate for multiple components assays • Variety of colors • Variety of available surface chemistries • Good control of antibodies orientation and their activity 	<ul style="list-style-type: none"> • Large and not very intensely colored particles • Reduced parking density on test lines and less sensitivity than gold in many instances • Requirement for the use of high surfactant due to hydrophobic characteristics and size
Gold	<ul style="list-style-type: none"> • Price • Different sizes • Generate relatively high sensitivity results • User friendly format • Inert 	<ul style="list-style-type: none"> • Only qualitative and not quantitative • Very limited quantitative dynamic range • Low multiplexity • Lack of automation • Sensitive to changes in pH, salt and organics • Single color choice, thus can not be used in multiplexing environments
Colloidal carbon	<ul style="list-style-type: none"> • Increased surface area • Don't aggregate • Inexpensive • Easily may be scale up • High color contrast • Stable 	<ul style="list-style-type: none"> • Longer immobilization procedures • Only a few vendors for well-characterized carbon particles available and the use of colloidal carbon for lateral flow assays requires a licensing agreement from the vendors
Magnetic beads	<ul style="list-style-type: none"> • Measuring of particles throughout the membrane • High stability • Aggregation hardly changes the absorption properties • Not affected by the sample matrix • Labels stable thus may be reanalyzed if required 	<ul style="list-style-type: none"> • Identification of the population of multiple markers must be done in series, rather than concurrently, increasing the time of the testing
Fluorescent nanoparticles	<ul style="list-style-type: none"> • Sensitive • Broad absorption bands • Commercially available 	<ul style="list-style-type: none"> • Quenching • Photobleaching • Extensive modification of the protein frequently cause physicochemical changes that can lead to changes in hydrophobicity, conformational changes, and steric hindrance



Smartphone detection of *E. coli* in water



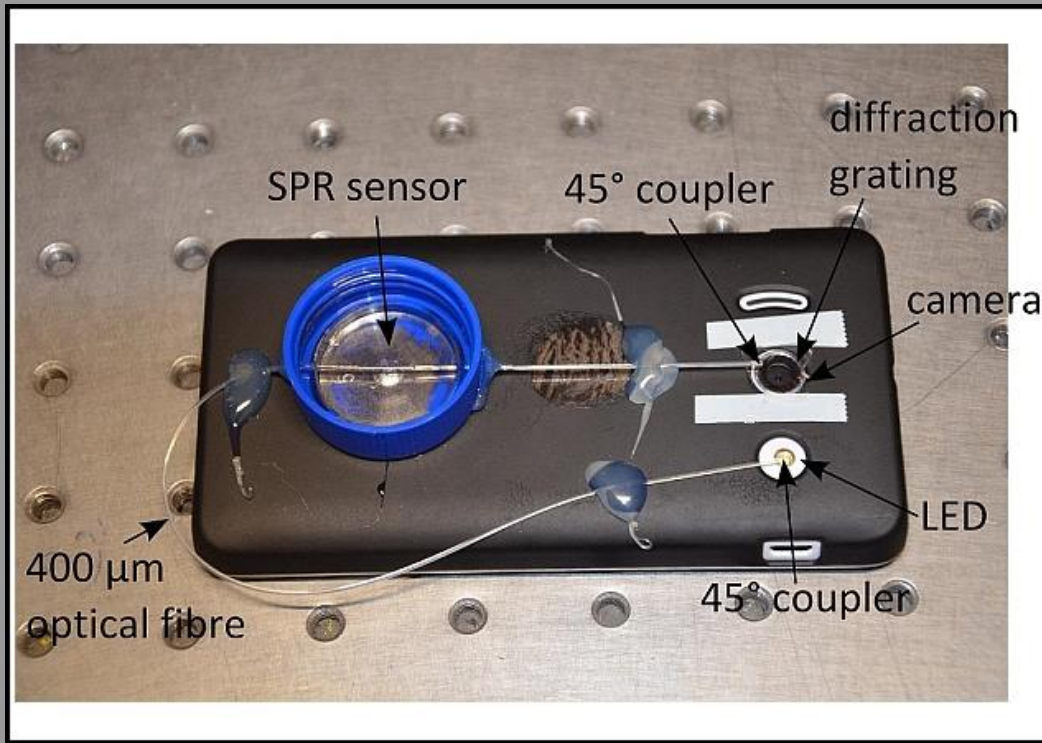
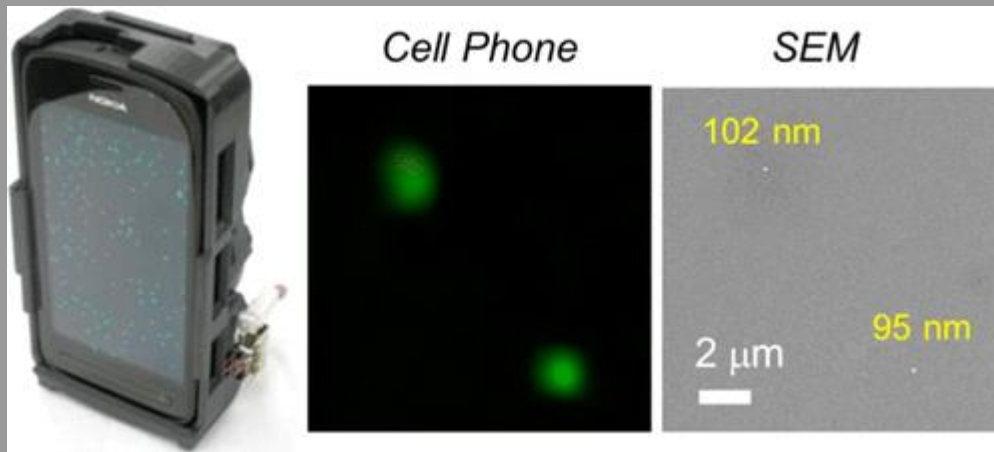


Image: Kort Bremer, Hanover Centre for Optical Technologies



Miscoscopio
basato su smart
detection di
virus

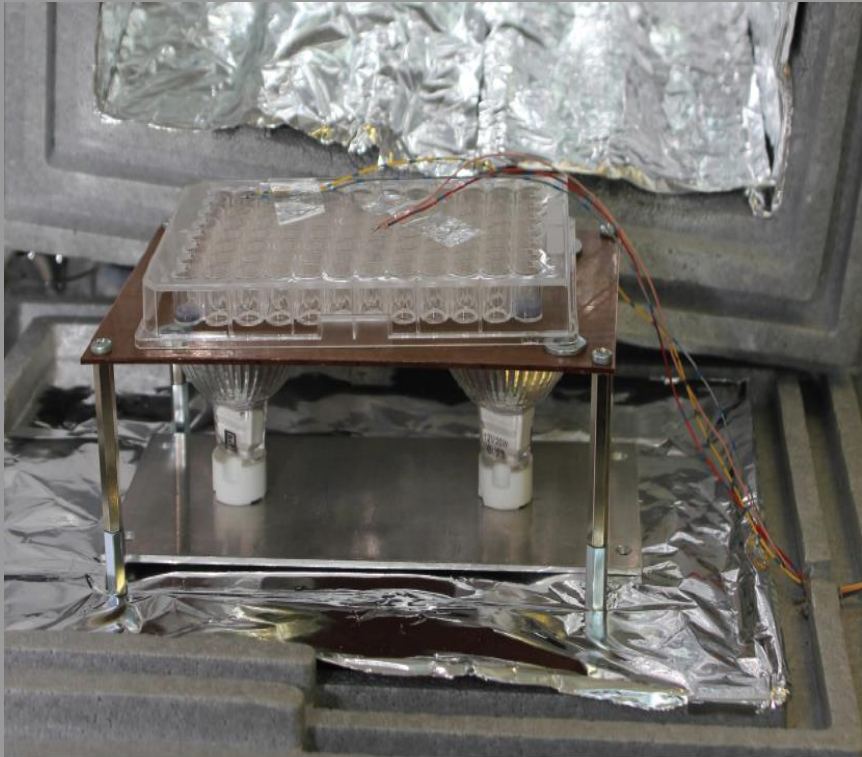


Fig. 1

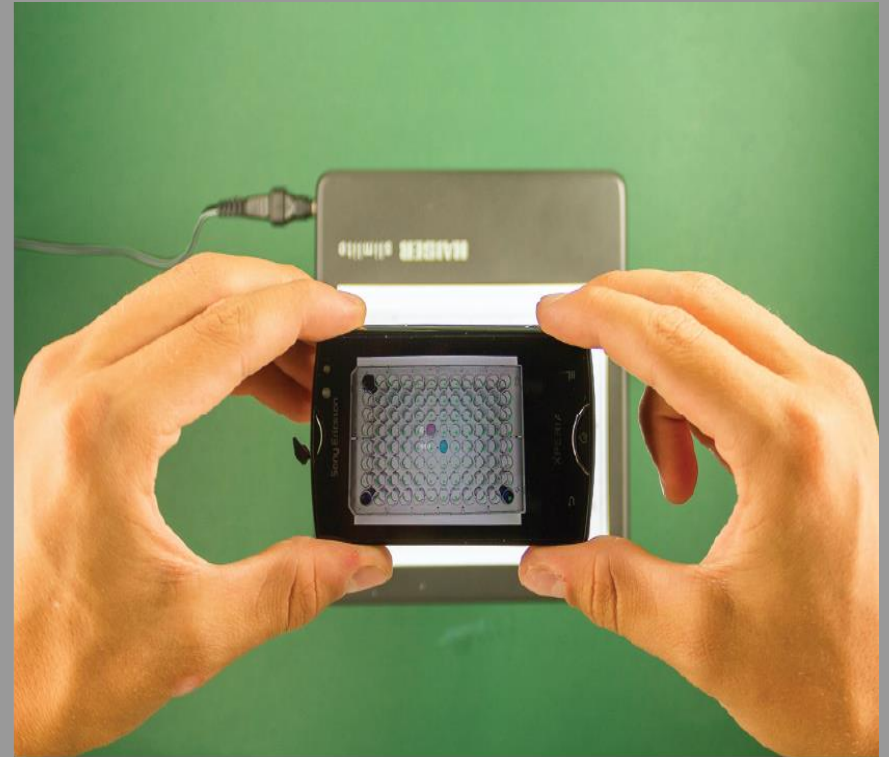
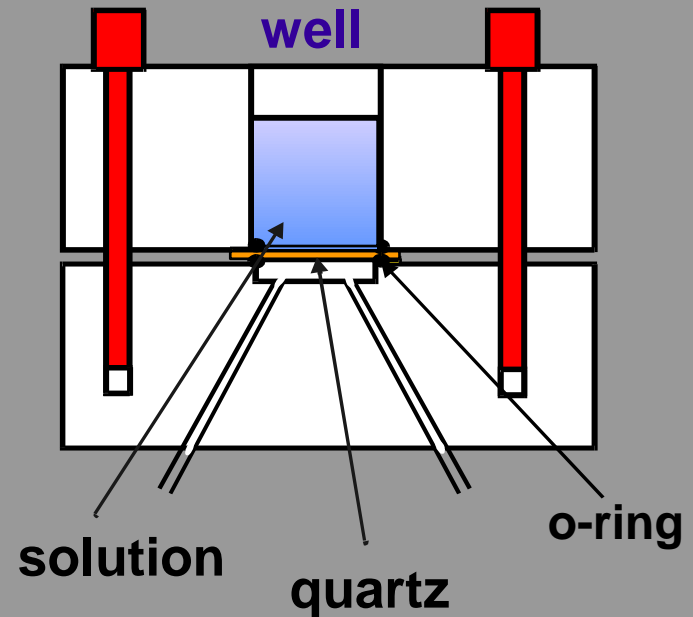
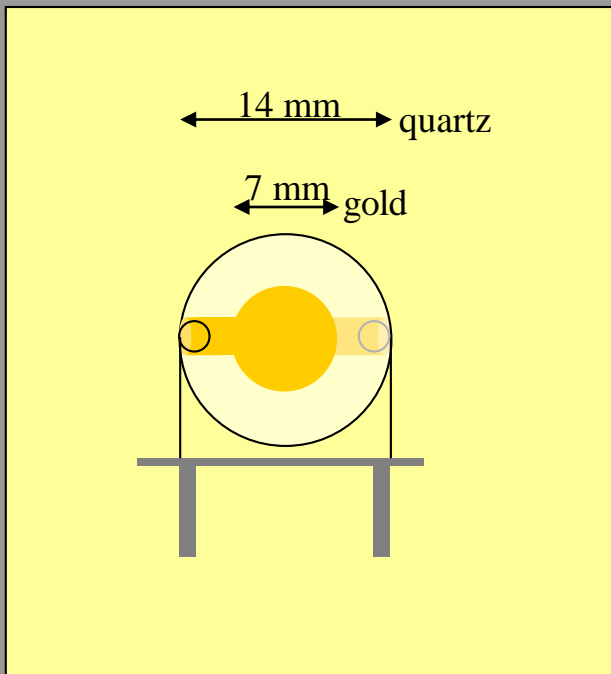
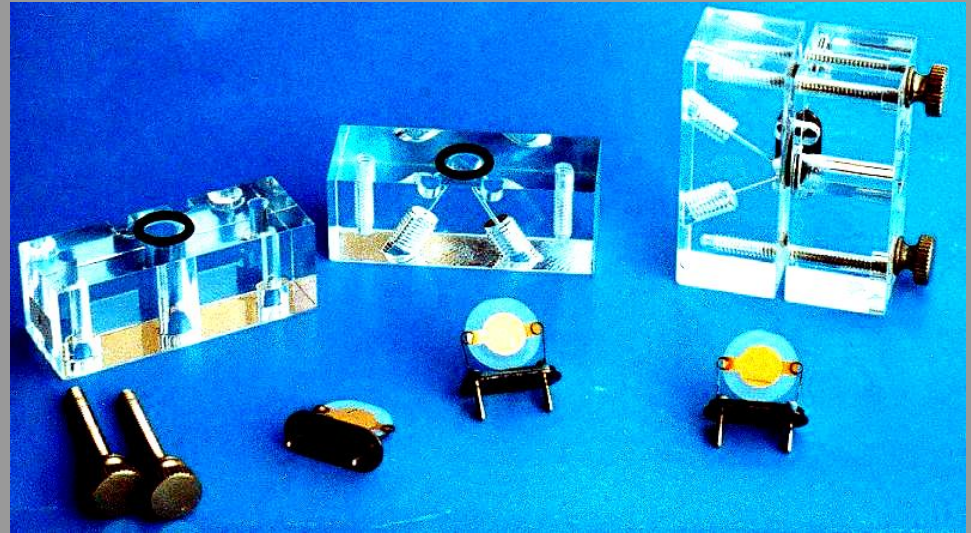
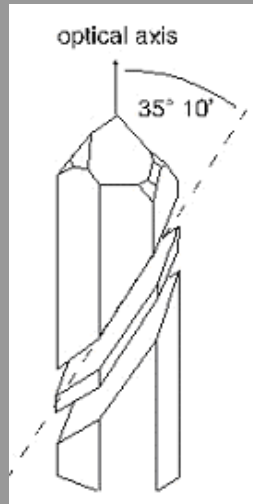
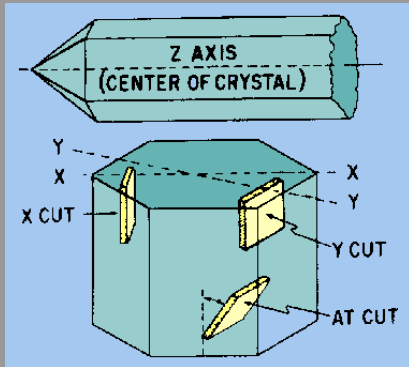


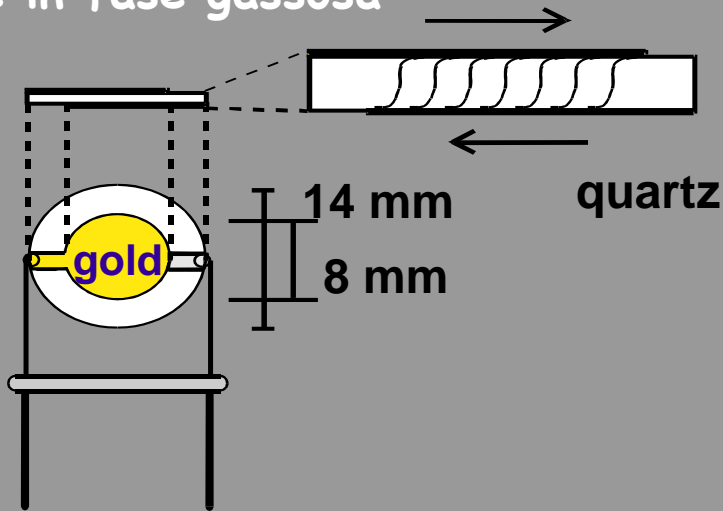
Fig. 2

Lettore ELISA adattabile a Smartphone

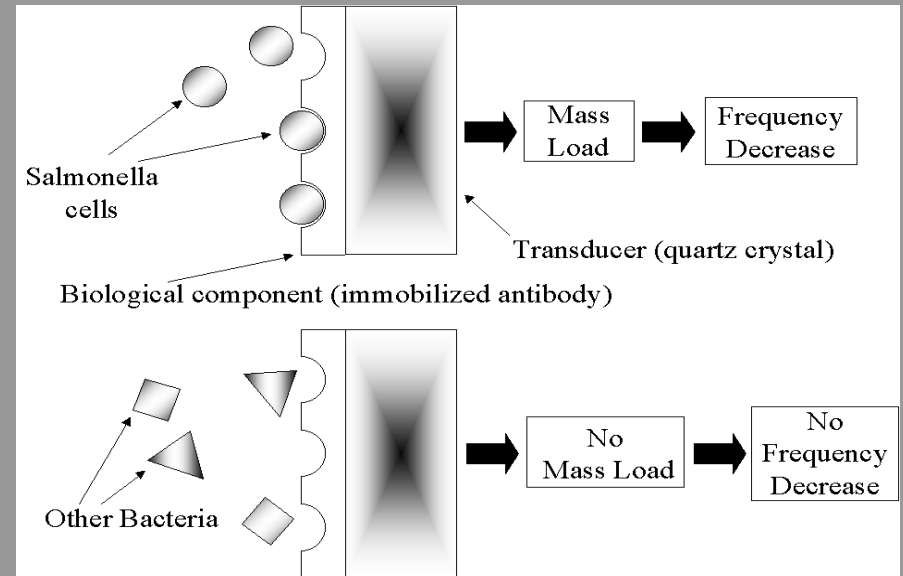
Piezoelectric Biosensors



Sensori piezoelettrici usati per tutti i biosensori di affinità e in fase gassosa



The mass-loading frequency effects of the transducer are based upon Sauerbrey's equation



The standard QCM measures the mass of a material deposited on a quartz crystal surface as a linear function of a change in the oscillating crystal resonant frequency

QCM-Mass

$$\Delta F = (-2.3 \times 10^{-6}) F^2 \Delta M / A$$

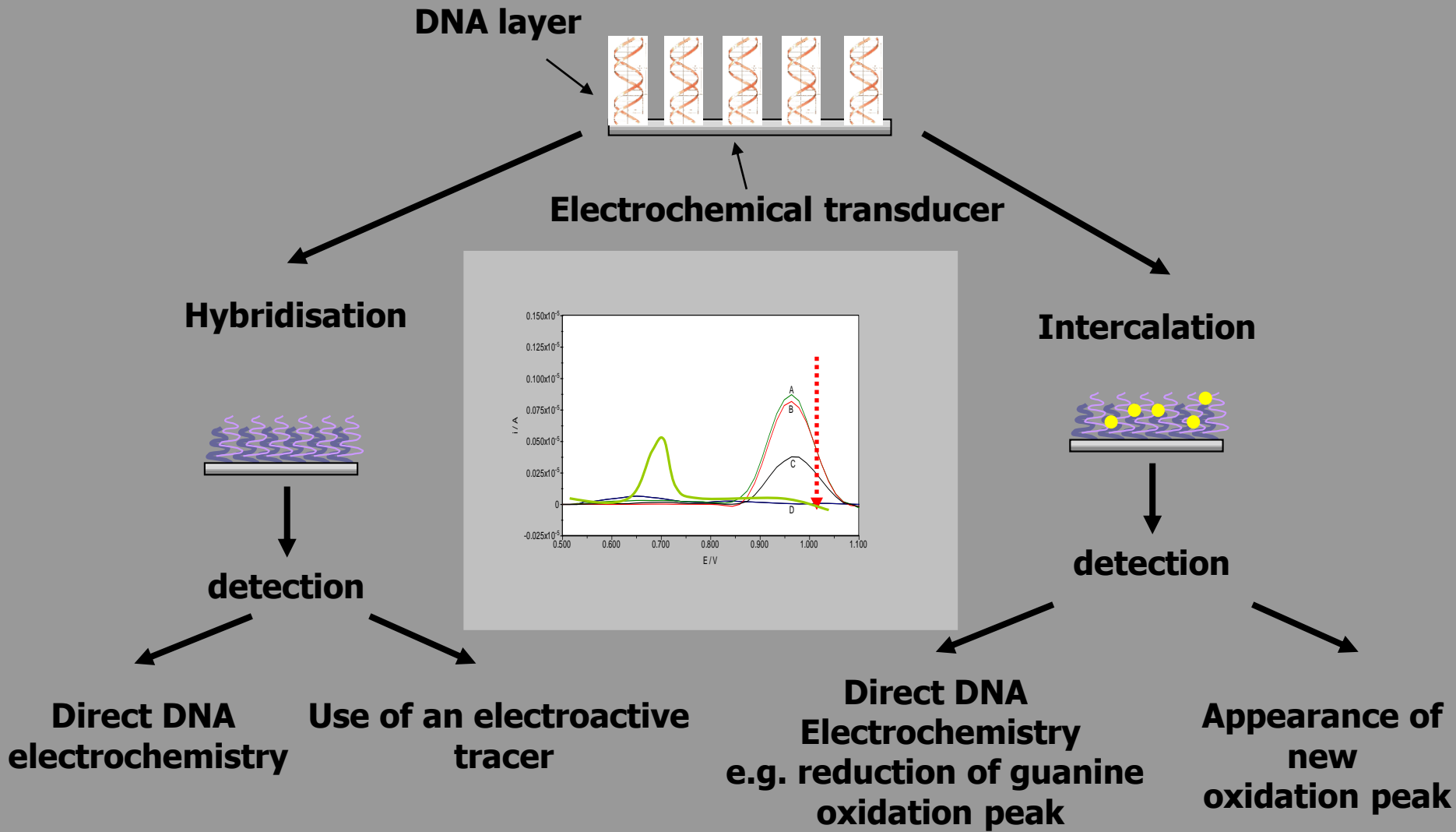
ΔF (Hz) = frequency shift of the coated crystal

F (Hz) = resonance frequency of the crystal

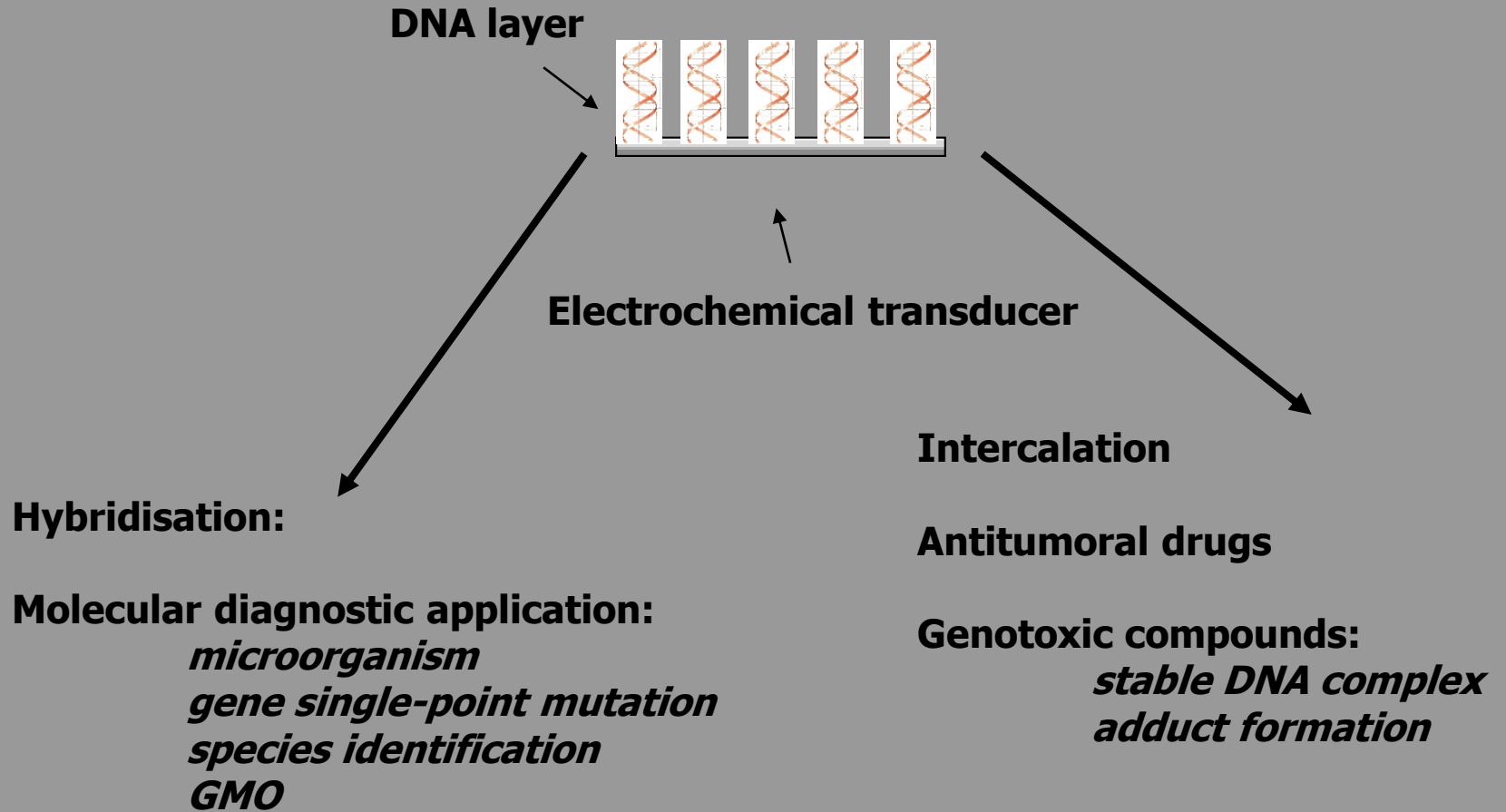
ΔM (g) = increase in mass loading

A (cm²) = area of the coated crystal

DNA electrochemical biosensors



DNA electrochemical biosensors application

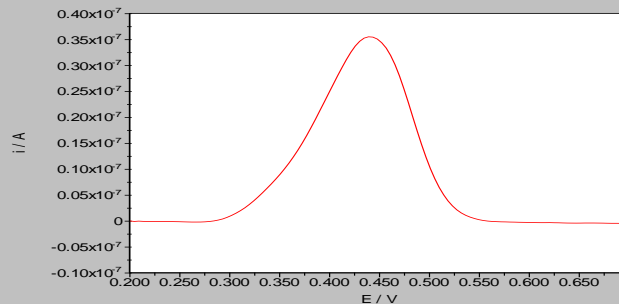
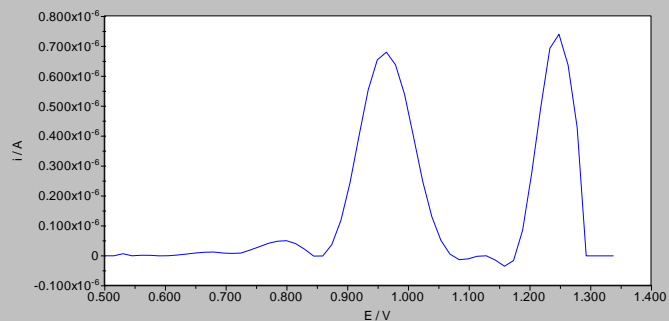


Obiettivo

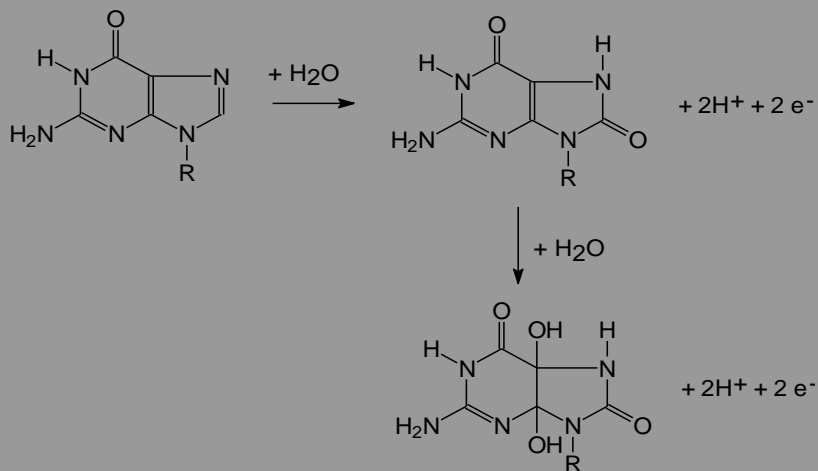


Ottimizzare una procedura di monitoraggio rapido basata sull' utilizzo di sensori elettrochimici a DNA per rivelare la presenza di ceppi potenzialmente tossinogenici di *Fusarium culmorum*

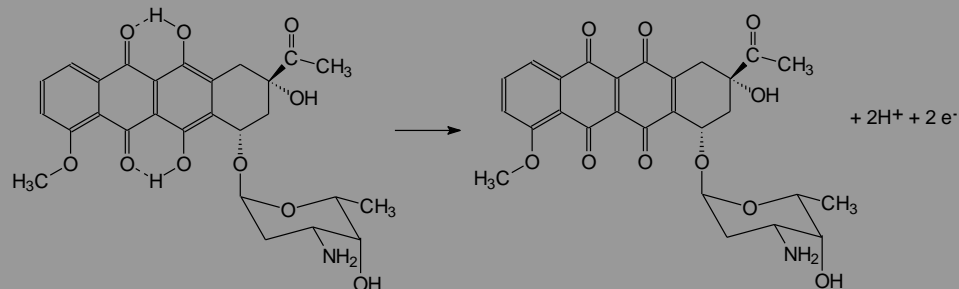
Voltammetria ad onda quadra



Guanine oxidation



Daunomycin oxidation



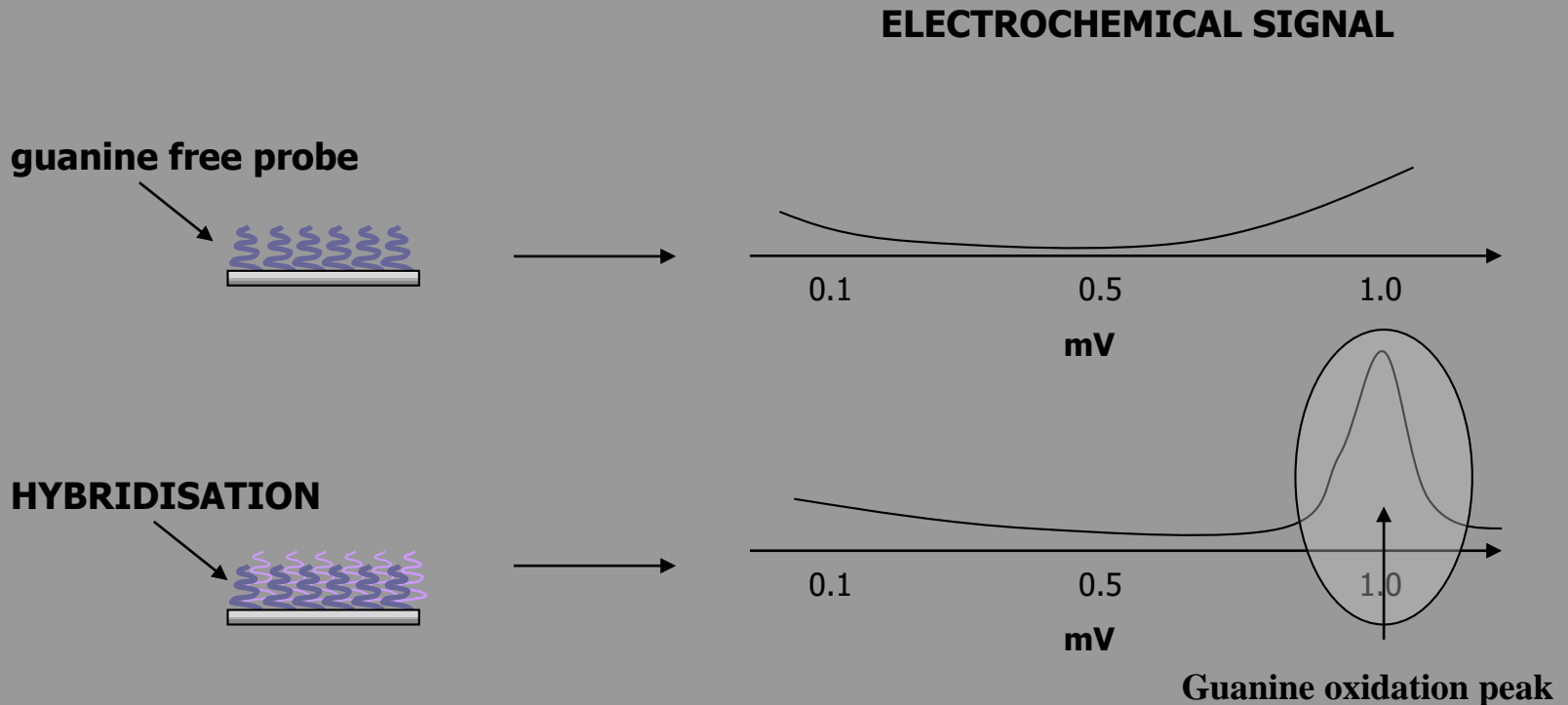
DNA from *Fusarium culmorum*

Aim:

- to develop a DNA electrochemical biosensor able to specifically detect specific sequences of *Fusarium Culmorum* in PCR amplified samples.

Sensing principle:

- direct electrochemical detection of guanine bases upon hybridisation of a *guanine free* probe.



GACATGAGTCTCTATGGAAAGAAGATTTATATTGAGACTCCTGTGCAGAGATGGGTTG
AAGTGACTGTTGTGGACTCAACC GATGGTGGTATTGATGAGA ACTATTTAGACTTGTCT
GTGGCTGCTTTCAAGGTTCTTGCTAGGGTTGAGGATGGCGTTTCGCAGATTACTTGGAA
CTACATGTAGGCTTGTCGTGTCTGAAGCTCTGTTAAGTTTCCAGAGTAA AGCTGATAGC
AGTATTAATCATA CATATGAAAAAAAAATGGGATGCAAGAAGCTCAAAGTCAAGGTCCA
TTCTTCAATGGACGCCATTTGCTTTACCCCTCTGTTACTAACTATCACCCAAGACGGG
AATGAATGAACGCTTGGATATCTTTCCAAGCTTGAGGGCAGCGCTCCCCGTGTTGGCG
AAAAAAGGAATCAACCCCGTCCAGAAGCGTCTCAACCTCCCGTGAGTCAAGGTTCTCG
TTTCTGAGTAGAACTGAATTGATCGCAAGCGGTCCC GGGTCTCTGATATGG

Probe *fusarium* 1: 5' TIA-CTI-TTI-TII-ACT-CAA-CC 3' (20 basi; 5 citosine)

Comp *Fusarium* 1: 5' GG-TTG-AGT-CCA-CAA-CAG-TCA 3'

Probe *fusarium* 2: 5' CTC-TIT-TAA-ITT-TCC-AIA-ITA-A 3' (22 basi; 4 citosine)

Comp *Fusarium* 2: 5' T-TAC-TCT-GGA-AAC-TTA-ACA-GAG 3'

Probe *fusarium* 3: 5' CTT-TAC-CCC-TCT-ITT-ACT-AAA-CTA-T 3' (25 basi; 8 citosine)

Comp *Fusarium* 3: 5' A-TAG-TTT-AGT-AAC-AGA-GGG-GTA-AAG 3'

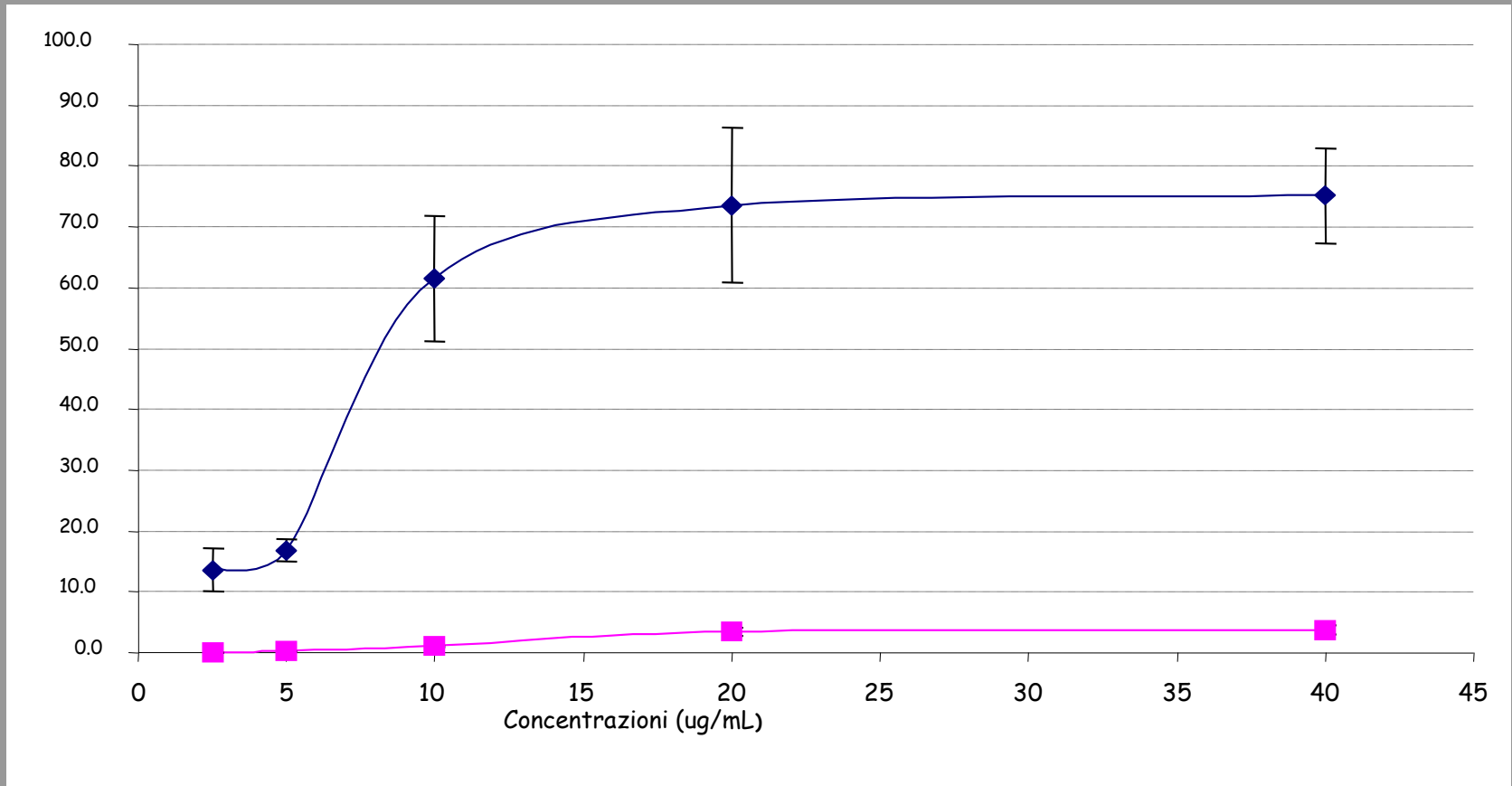
Probe *Fusarium* 4: 5' CII-TCC-CII-ITC-TCT-IAT-ATI-I 3' (22 basi; 6 citosine)

Comp *Fusarium* 4: 5' C-CAT-ATC-AGA-GAC-CCG-GGA-CCG 3'

1. PRETRATTAMENTO (+1.6Vx120s - +1.8Vx60s)
2. IMMOBILIZZAZIONE (+0.5Vx300s)
3. IBRIDAZIONE (10min)

FASI DELLA PROCEDURA ANALITICA

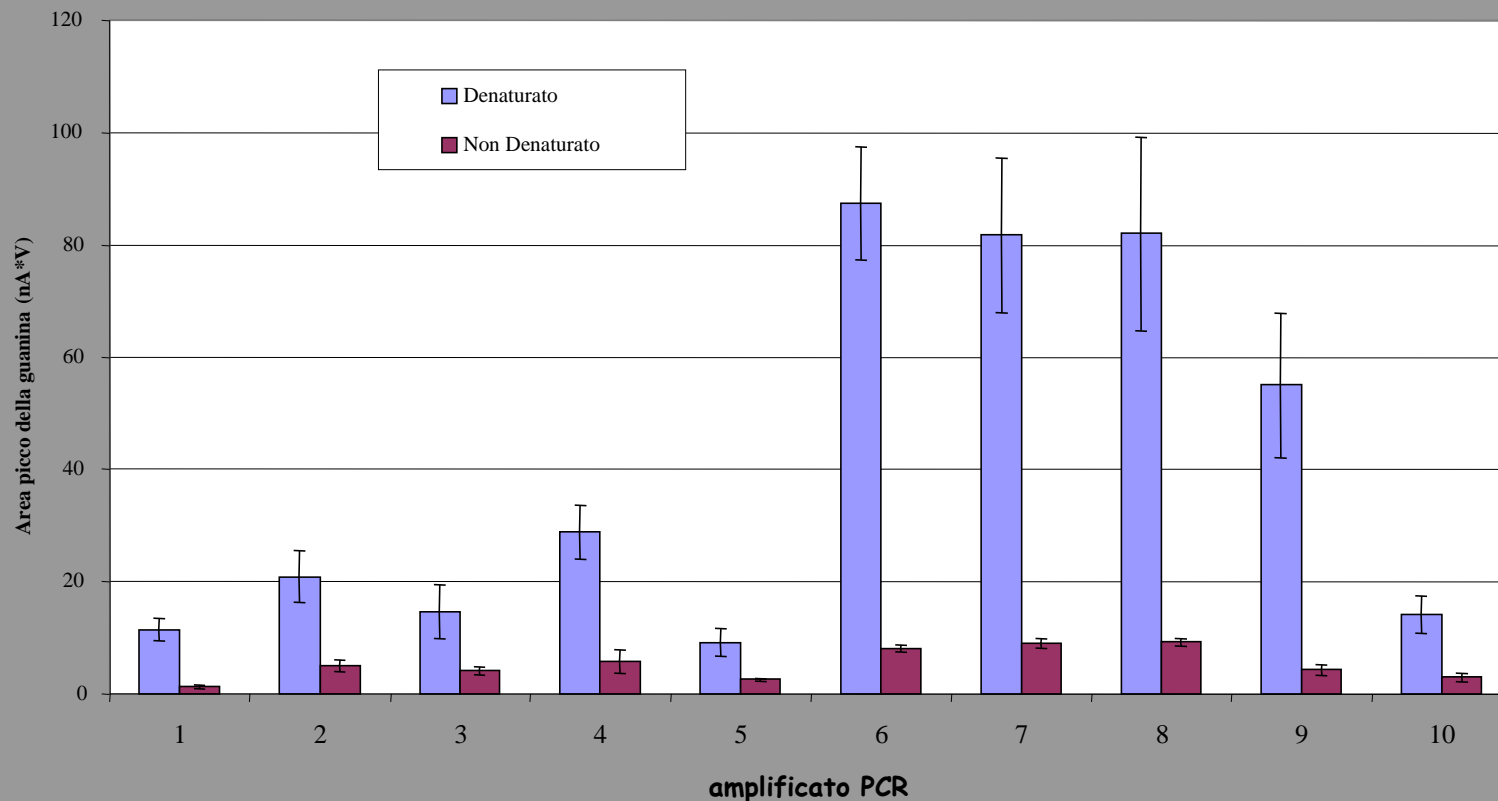
3. IBRIDAZIONE



Risposta del sensore a varie concentrazioni del complementare e del non complementare del probe 3

risposta denaturato/non denaturato per 10 ceppi europei di *F.Culmorum*

Probe 3-40ug/mL
Amplificato PCR 10 ug/mL



Risposta del probe 3 agli amplificati denaturati e non denaturati

Genetically modified organisms (GMO)

- Determination of specific DNA sequences obtained by a genetic modification in plant materials (the matrix for food production)
- Screening methods are based on the detection of the two regulatory sequences by Polymerase Chain Reaction:

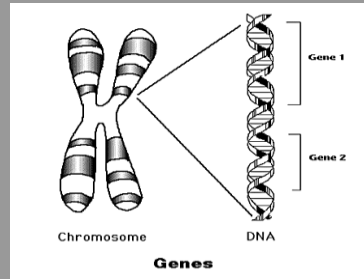
35S promoter

NOS terminator

These sequences are introduced in most of GMO
(Except China)

for the expression of transgenes.

- **Development of an *Hybridisation sensor***



Synthesis of a DNA fragment (probe, bioreceptor) containing the sequence of interest (**analytical problem**)

Immobilisation of the probe onto the solid support of the sensor (**surface**)
(*thiol/dextran/streptavidin/biotinylated probe*)

Extraction of the DNA from the real sample (blood, water, food) and amplification of the sequence of interest (**sample pretreatment**)

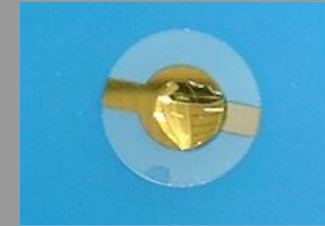
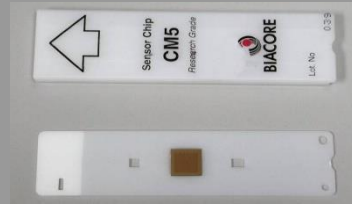
Denaturation of the dsDNA (amplified fragment or genomic) to obtain a single-stranded DNA (**sample pretreatment**)

Hybridisation of the obtained ssDNA with the immobilised probe

Changes in the physicochemical parameters of the layer formed on the transducer (quartz crystal or gold –glass chip)

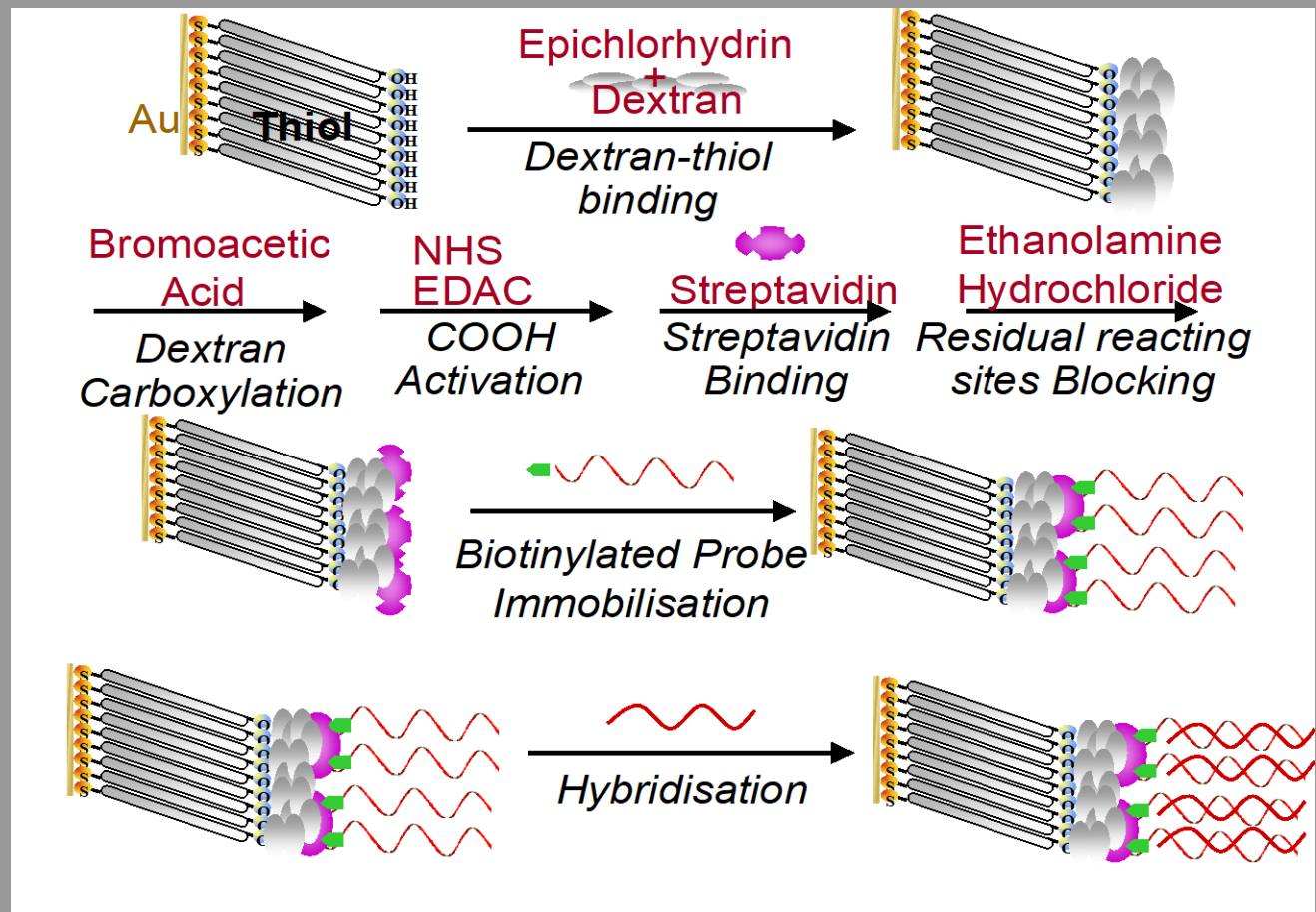
Probe immobilisation on gold film

optical



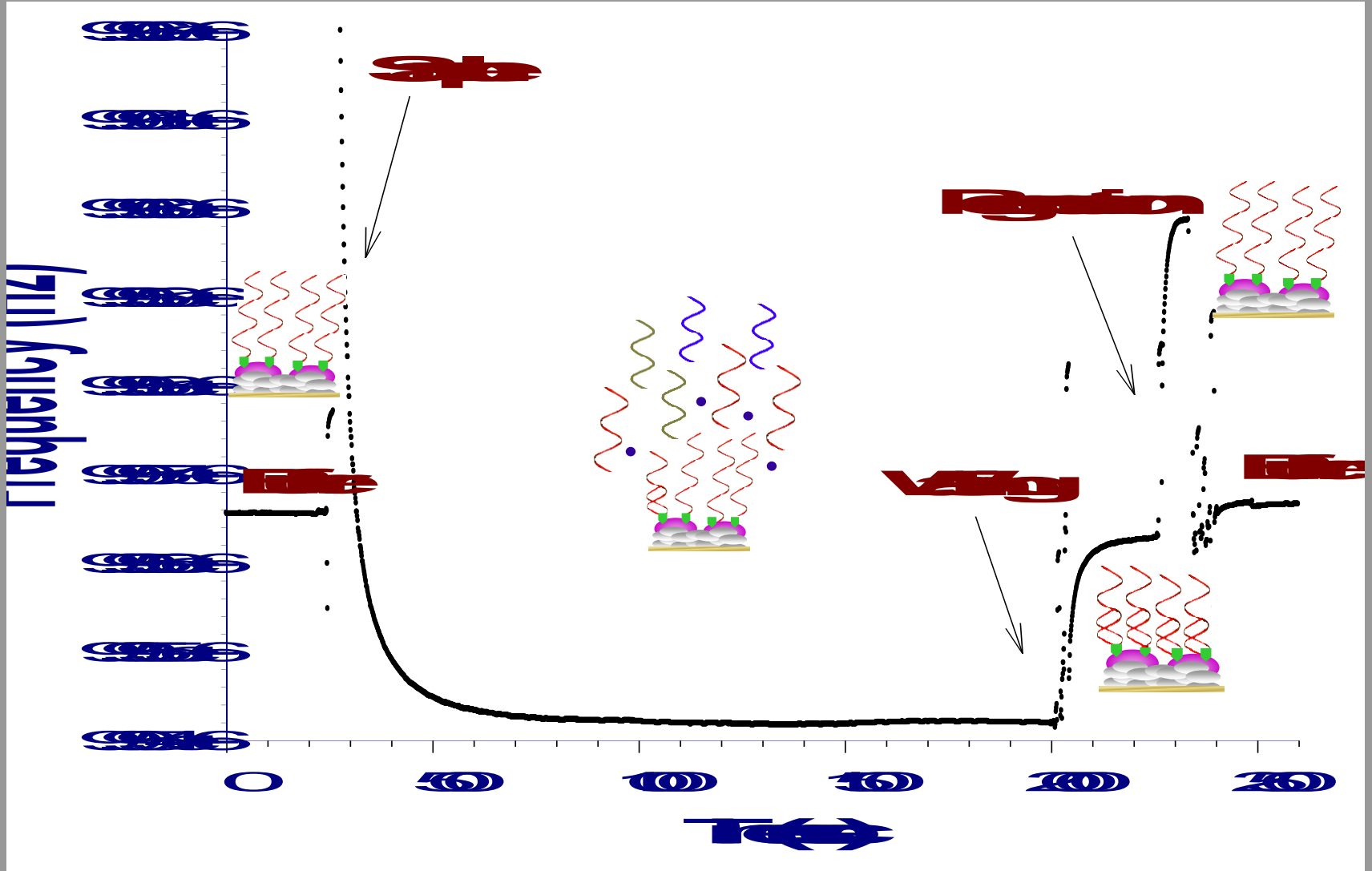
piezoelectric

thiol/dextran/streptavidin/biotinylated probe



Specificity,
no aspecific
adsorption,
stability,
multi-use

Hybridation-Regeneration Cycle



Detection of DNA target sequence in real matrices

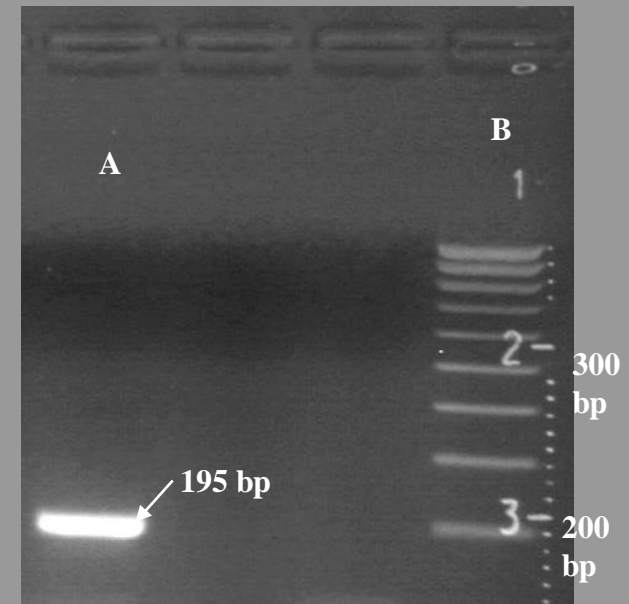
- Certified Reference Materials (CRM) -Fluka
- Processed food (dietetic snaks, soy crackers, soft drinks)

1. PCR amplified DNA

Processing the sample

- **Extraction** of DNA from samples (CTAB method)
- **Amplification** of DNA by PCR (Pietsh K. et al. 1997)
- **Dilution** with *Hybridisation buffer*. NaCl 150 mM, Na₂HPO₄ 20 mM, EDTA 0.1 mM, pH 7.4
- **Denaturation** to obtain ssDNA from amplified dsDNA

Control: Post PCR
Electrophoresis

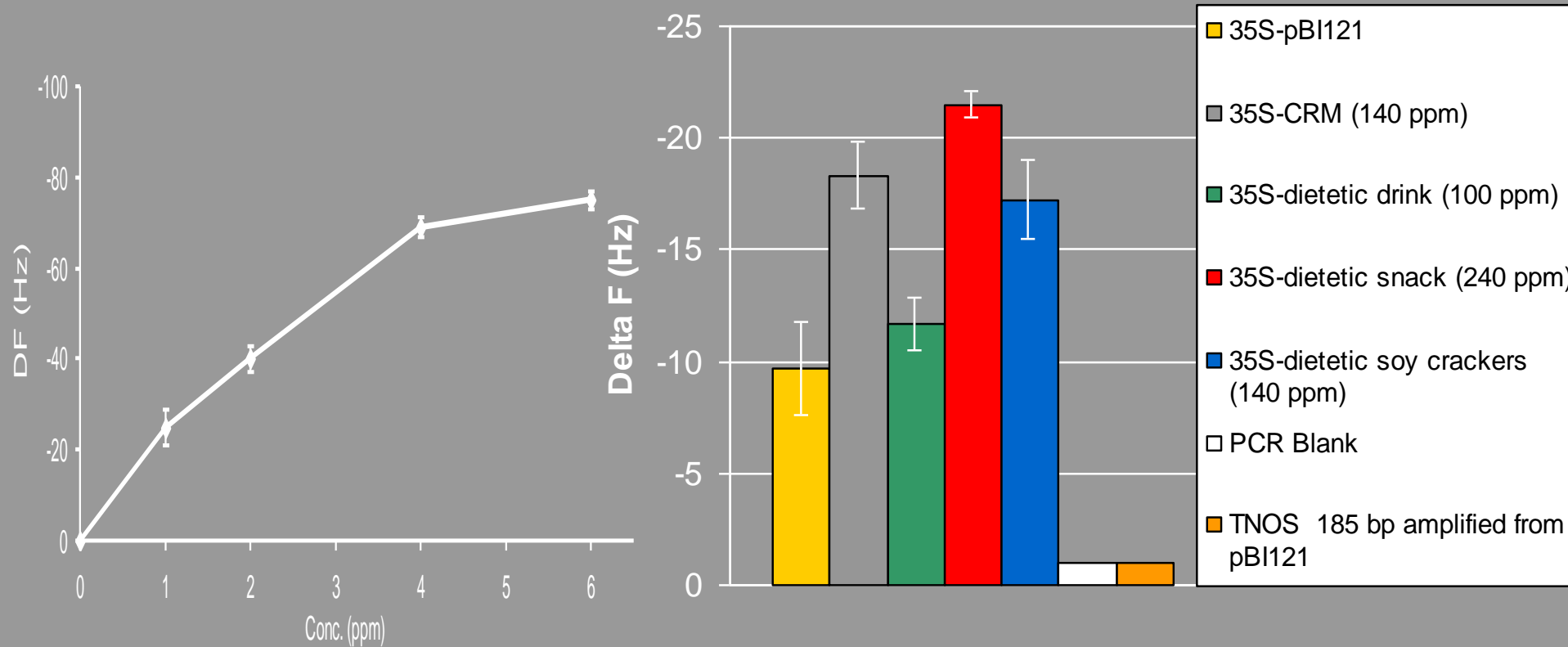


A: amplified fragment
(**Promoter 35S** 195 bp)

B: Standard length fragments

Piezoelectric sensor, CRM 2% samples and processed food samples

Sample pre-treatment: PCR amplified DNA, thermal denaturation



DL: 0,3 ppm

CV% 6 (n=3)

5'-BIOT-ggc cat cgt tga aga tgc ctc tgc c-3' probe 35S
3'- ccg gat gca act tct acg gag acg g-5 target 35S